



M/EEG Preprocessing

MfD 10th May 2023

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EEG and MEG signal is usually acquired at a high temporal sampling frequency

• e.g., 250Hz to several kHz

>Not all frequencies in data reflect underlying neural sources

- e.g., motion can generate low frequencies, muscular activity generates high frequencies
- Useful to filter out these frequencies during preprocessing

➢ Relevant frequencies would depend on study design/question

Evoked/event-related potentials

Spontaneous activity / Oscillations

➤Time-frequency

Steady-state evoked potentials

Evoked/event-related potentials

➤Large number of trials

- ➤Time-locked average
- ➢Typically seen in 1—10Hz range
- Components: P100, N140, P300, LPP



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Katyal, S., et al (2020). Event-related potential and behavioural differences in affective self-referential processing in long-term meditators versus controls. *Cognitive, Affective & Behavioral Neuroscience, 20*(2), 326–339.

Oscillations / spontaneous activity

- ➤Continuous activity
- Extract different frequency bands corresponding to mental functions
 - Delta: 1–3 Hz
 - Theta: 4–7 Hz
 - Alpha: 7–13 Hz
 - Beta: 15–25 Hz
 - Gamma: >30 Hz

- Beta vellerliste detaistanteen liebelleren al steratettationersaliseen alter data partette etaiteer.



- e.g., modulation alpha and theta

oscillations with depth of meditation

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Katyal, S., & Goldin, P. (2021). Alpha and theta oscillations are inversely related to progressive levels of meditation depth. *Neuroscience of Consciousness*, 2021(1), niab042.

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Time-frequency



- Combination of time-locked and spectral analysis



Steady-state evoked potentials

- Continuous stimulus contains repeated frequencies
- obtain response by filtering signal at those frequencies and linear combinations of those frequencies
- Katyal, S., Engel, S. A., He, B., & He, S. (2016). Neurons that detect interocular conflict during binocular rivalry revealed with EEG. *Journal of Vision*, *16*(3), 18–18.

Katyal, S., Vergeer, M., He, S., He, B., & Engel, S. A. (2018). Conflict-sensitive neurons gate interocular suppression in human visual cortex. *Scientific Reports*, 8(1), 1239.

Left eye Right eye $\int_{\frac{1}{4}} \int_{\frac{1}{4}} \int_{\frac{1}{8}} \int_{\frac{1}{12}} \int_{\frac{1}{12}}$

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f₂



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e.g., ocular opponency neurons in visual perception

- mixed rivalry perception related to *f2-f1* signal
- *f2-f1* signal specifically adapt in exposure to rivalry/interocular conflict



Unexpected features of M/EEG data

- Eye movements
- Heartbeat
- Participant head movement
- Muscle Artefact
- Poorly attached EEG electrode
- SQUID Jump
- 50/60Hz Line Noise

Non-physiological

Physiological



Filtering

Removing frequencies not expected in the study

- **Low-pass** remove high-frequency noise.
- High-pass remove the DC offset and slow trends in the data.
- Notch (band-stop) remove artefacts limited in frequency, most commonly line noise and its harmonics.
- Band-pass focus on the frequency of interest and remove the rest.
 More suitable for relatively narrow frequency ranges.





Filtering examples



11/05/2023

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- Sampling rate: speed at which your data is recorded/sampled

- PROS:
 - Speeds up analysis
- -CONS:
 - Aliasing: an effect that causes different signals to become indistinguishable (or aliases of one another) when sampled
 - Nyquist Frequency: Highest frequency that can be resolved without alisasing=
 ½ of sampling rate

Epoching



Extracting segments around events

- What: event type, coded event value
- When: onset/offset time of events

Need to define:

- Segment borders
- Trial type (can be different triggers => single trial type)
- Shift of time zero of the trial with respect to the trigger (no shift by default)

Note for SPM:

- only supports fixed length trials
- Performs baseline correction during epoching using negative times



- In EEG, voltages recorded at each electrode are relative to voltages recorded at other electrodes.
- Best practice to use a common electrode to reference all electrodes
 E.g. (average of) mastoids or Cz
- Can also use average of all channels, but harder to detect subtler voltage changes
- Montage function can apply any linear weighting to the channels & has a wider range of applications.



- Decompose data into different components
- Option not available in SPM





- Identify components to reject
- e.g., eye blinks are observed at frontal electrodes





After eye blink
 component removal





An Introduction to the SPM Interface



SPM interfaces

GUI

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spm eeg

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51 - 52 - 53 -	S.circularise = false; D = som eeg average TF(S):	

Batch



run within MATLAB

script

- SPMpath = 'D:\spm12';
- -addpath(SPMpath);
- -spm ('defaults', 'eeg')
- -spm eeg

– IMPORTANT → Make sure your path has just been cleared and do not put different imaging toolboxes in the same folder as they might interfere – causing crashes!

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Open SPM



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Steps to cover

- 1. Conversion
- 2. Filtering
- 3. Downsampling
- 4. Epoching
- 5. Re-referencing for EEG
- 6. Artefacts correction
- 7. Averaging

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– The *.dat file contains the raw binary data, is memory- mapped and linked to the object in order to save memory.
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Properties of M/EEG dataset

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	圭 fiducials	1x1 struct
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	🗐 other	1x1 struct

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- -The *.mat file contains a struct, named D, which is converted to an meeg object by spm_eeg_load.
 - Contains header information sampling rate, channel information, trial information, etc.

Conversion

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Filtering

- 1. Conversion
- 2. Filtering
- 3. Downsampling
- 4. Epoching
- 5. Re-referencing for EEG
- 6. Artefacts correction
- 7. Averaging

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Filtering

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<u>Downsampling</u>

- 1. Converting
- 2. Filtering
- 3. Downsampling
- 4. Epoching
- 5. Re-referencing for EEG
- 6. Artefacts correction
- 7. Averaging

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Downsampling

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Epoching

- 1. Converting
- 2. Filtering
- 3. Downsampling

4. Epoching

- 5. Re-referencing for EEG
- 6. Artefacts correction
- 7. Averaging

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Epoching



Offset - difference between the trigger value and the actual start of the trial

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 \rightarrow window is the baseline value (so -96 means 96 samples in each trial are considered baseline)

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Artefacts correction

- 1. Converting
- 2. Filtering
- 3. Downsampling
- 4. Epoching
- 5. Re-referencing for EEG
- 6. Artefacts correction
- 7. Averaging

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Searching for artefacts



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MEGGRAD

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Removing artefacts

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Averaging

- 1. Converting
- 2. Filtering
- 3. Downsampling
- 4. Epoching
- 5. Re-referencing for EEG
- 6. Artefacts correction
- 7. Averaging

spm_eeg_average

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Averaging

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Data visualisation





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Average of faces condition at 1010ms



Average of scrambled images condition at 1010ms

Data visualisation

承 SPM12 (7771): Graphics





Steps to cover

- 1. Converting
- 2. Filtering
- 3. Downsampling
- 4. Epoching
- 5. Re-referencing for EEG
- 6. Artefacts correction
- 7. Averaging

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Run preprocessing on several runs

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Averaging		9	spm_jobman('run', jobs, inputs{:});
Averaging		10	
		+3	MfD_preprocessingMEG_job.m 🗶 MfD_preprocessingMEG.m 🗶
		1 -	
		2	% JOD Saved on 09-May-2023 14:38:17 by ctg_utl1 (rev \$Rev: 7345 \$) % spm SDM - SDM12 (7771)
		4	% spin srn - srniz (///i) % cfg basicio BasicIO - Unknown
		5	%
		6	matlabbatch{1}.spm.meeg.convert.dataset = {'D:\MfD\MEG_templateSPMData\MEG\SPM_CTF_MEG_example_faces1_3D.ds\SPM_CTF_MEG_example_faces1_3D.meg4'};
		7	matlabbatch{1}.spm.meeg.convert.mode.continuous.readall = 1;
		8	<pre>matlabbatch{1}.spm.meeg.convert.channels{1}.all = 'all';</pre>
		9	<pre>matlabbatch{1}.spm.meeg.convert.outfile = '';</pre>
		10	<pre>matlabbatch{1}.spm.meeg.convert.eventpadding = 0; matlabbatch{1}.spm_meeg.convert.blocksize = 2276900;</pre>
		12	matlabbatch{1}.spm.meeg.convert.cbocksize = 5270000, matlabbatch{1}.spm.meeg.convert.cbockboundary - 1:
		13	<pre>matlabbatch{1}.spm.meeg.convert.saveorigheader = 0;</pre>
	~	14	<pre>matlabbatch{1}.spm.meeg.convert.inputformat = 'autodetect';</pre>
		15	<pre>matlabbatch{2}.spm.meeg.preproc.filter.D(1) = cfg_dep('Conversion: Converted Datafile', substruct('.','val', '{}',{1}, '.','val', '{}',{1}, '.','v</pre>
File Name		16	<pre>matlabbatch{2}.spm.meeg.preproc.filter.type = 'butterworth';</pre>
Select data set file.		17	<pre>matlabbatch{2}.spm.meeg.preproc.filter.band = 'high';</pre>
		18	<pre>matlabbatch{2}.spm.meeg.preproc.tilter.treq = 0.1; matlabbatch{2}.spm.meeg.preproc.tilter.treq = 0.1;</pre>
		20	matlabbatch{2}.spm.meeg.preproc.tilter.our = twopass ; matlabbatch{2} spm meeg.preproc.filter.order = 5:
		21	<pre>matlabbatch{2}.spm.meeg.preproc.filter.prefix = 'f';</pre>
		22	<pre>matlabbatch{3}.spm.meeg.preproc.downsample.D(1) = cfg_dep('Filter: Filtered Datafile', substruct('.', 'val', '{}', {2}, '.', 'val', '{}', {1}, '.', 'va</pre>
		23	<pre>matlabbatch{3}.spm.meeg.preproc.downsample.fsample_new = 200;</pre>
		24	<pre>matlabbatch{3}.spm.meeg.preproc.downsample.method = 'resample';</pre>
		25 ∢	

- There is no single correct order of steps, but here are some considerations for order choices
 - It is better to filter continuous data prior to epoching to avoid filter ringing artefacts in every trial. It is better to do high-pass filtering or baseline correction before other filtering steps to reduce filter ringing.
- Downsample early in the pipeline to make the subsequent steps faster.
- SPM only filters channels with physiological data. So the channel types should be set correctly before filtering.
- Some artefacts (e.g. discontinuous jumps, muscle) are more difficult to detect after filtering.

ШШ





Thank you so much for listening!

Thank you to our expert Mansoureh,

- SPM MEG course 2022 materials,

- to previous MfD course slides.

Questions?