

# Dynamic Causal Modelling for EEG/MEG: principles

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# Overview

- 1 DCM: introduction
- 2 Dynamical systems theory
- 3 Neural states dynamics
- 4 Bayesian inference
- 5 Conclusion

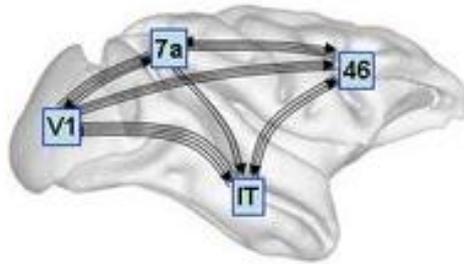
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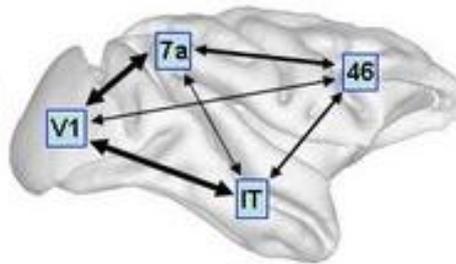
# Introduction

*structural, functional and effective connectivity*

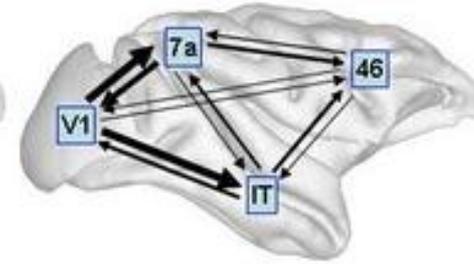
structural connectivity



functional connectivity



effective connectivity



O. Sporns 2007, *Scholarpedia*

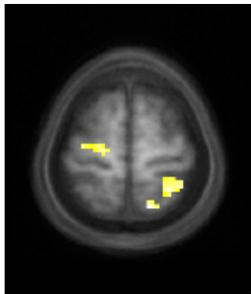
- ***structural* connectivity**  
= presence of axonal connections
- ***functional* connectivity**  
= statistical dependencies between regional time series
- ***effective* connectivity**  
= causal (directed) influences between neuronal populations

**! connections are recruited in a *context-dependent* fashion**

# Introduction

*from functional segregation to functional integration*

localizing brain activity:  
***functional segregation***

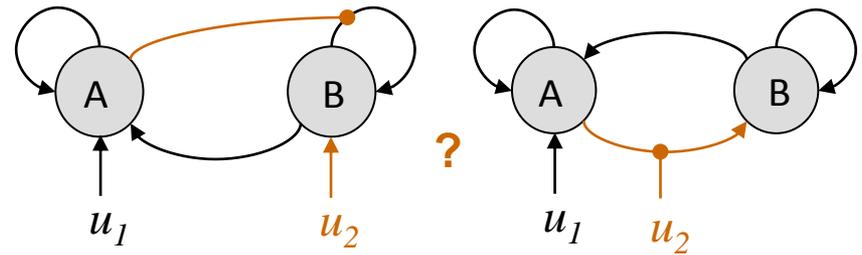


$u_1$



$u_1 \times u_2$

effective connectivity analysis:  
***functional integration***



« *Where, in the brain, did my experimental manipulation have an effect?* »

« *How did my experimental manipulation propagate through the network?* »

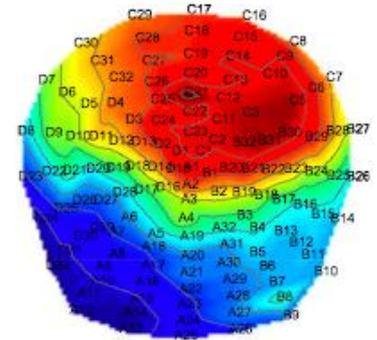
# Introduction

## DCM: evolution and observation mappings



Hemodynamic  
observation model:  
temporal convolution

Electromagnetic  
observation model:  
spatial convolution



neural states dynamics

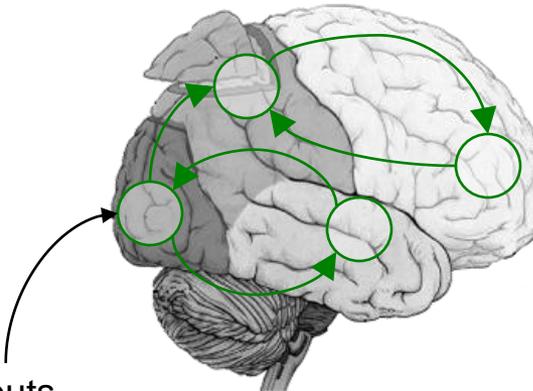
$$\dot{x} = f(x, u, \theta)$$

fMRI

EEG/MEG

- simple neuronal model
- complicated observation model

inputs



- complicated neuronal model
- simple observation model

# Introduction

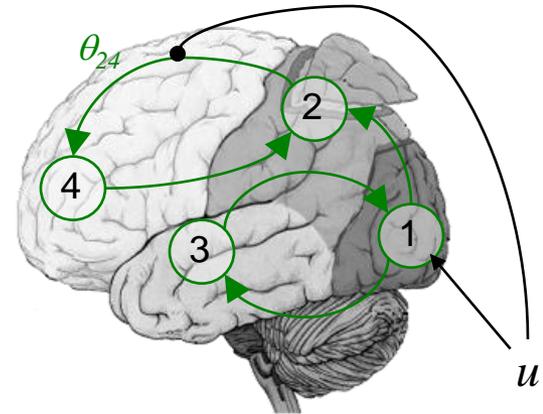
*DCM: a parametric statistical approach*

- DCM: model structure

$$\begin{cases} y = g(x, \varphi) + \varepsilon \\ \dot{x} = f(x, u, \theta) \end{cases}$$

likelihood

$$\Rightarrow p(y|\theta, \varphi, m)$$



- DCM: Bayesian inference

parameter estimate:  $\hat{\theta} = E[\theta|y, m]$

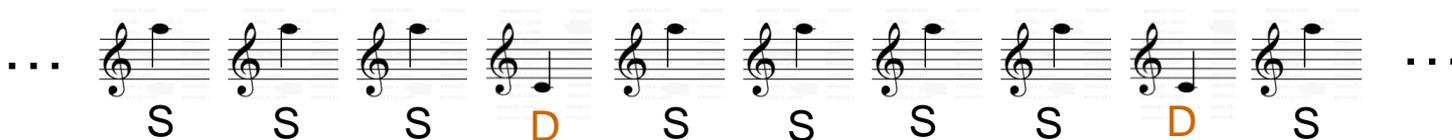
model evidence:

$$p(y|m) = \int p(y|\theta, \varphi, m) \overset{\text{priors on parameters}}{p(\theta|m) p(\varphi|m)} d\varphi d\theta$$

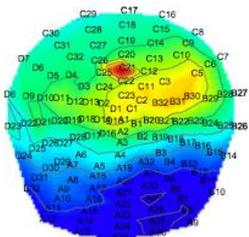
# Introduction

## DCM for EEG-MEG: auditory mismatch negativity

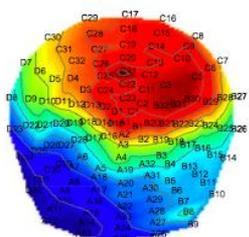
sequence of auditory stimuli



standard condition (S)

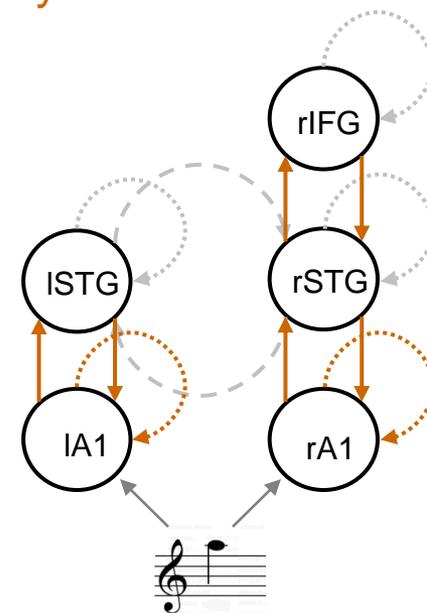
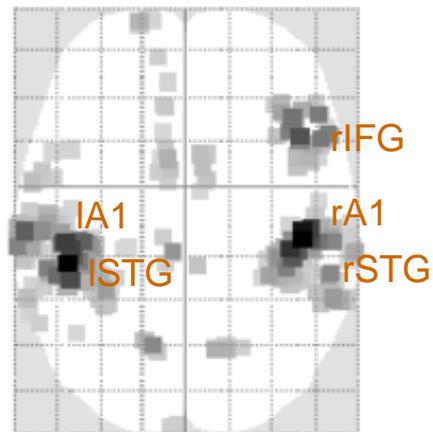


deviant condition (D)



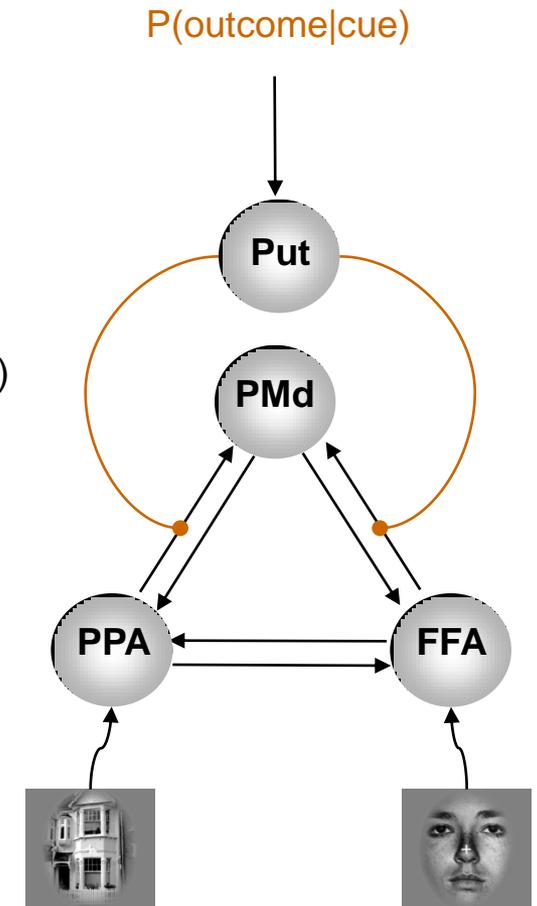
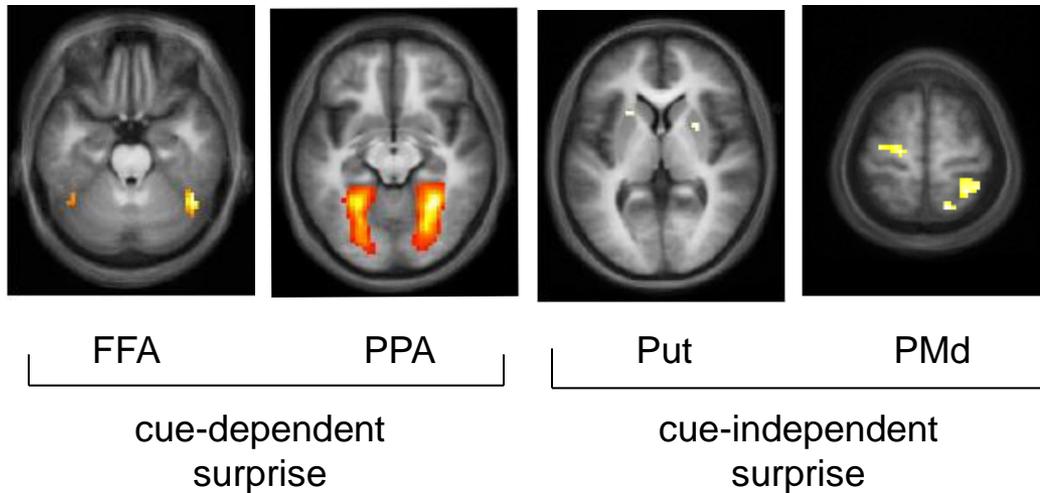
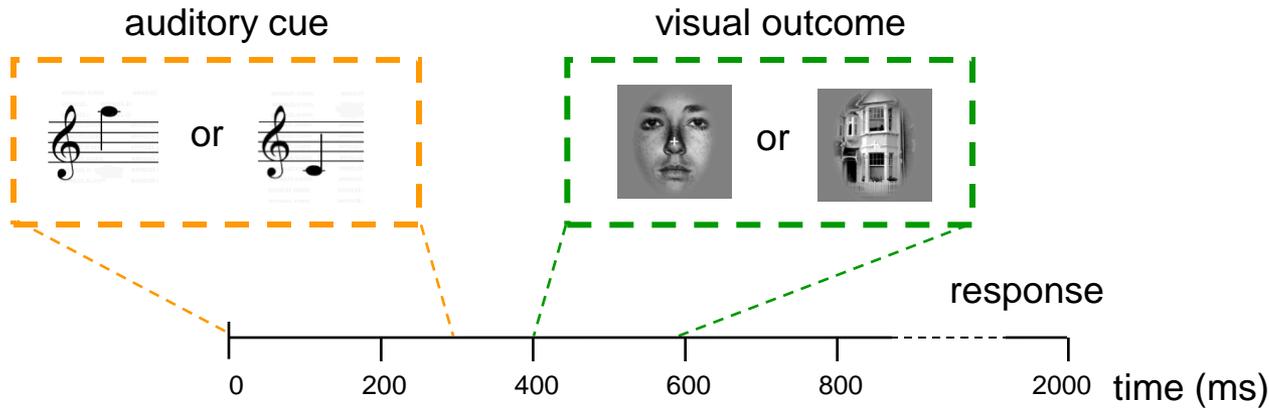
$t \sim 200$  ms

S-D: reorganisation  
of the connectivity structure



# Introduction

## DCM for fMRI: audio-visual associative learning



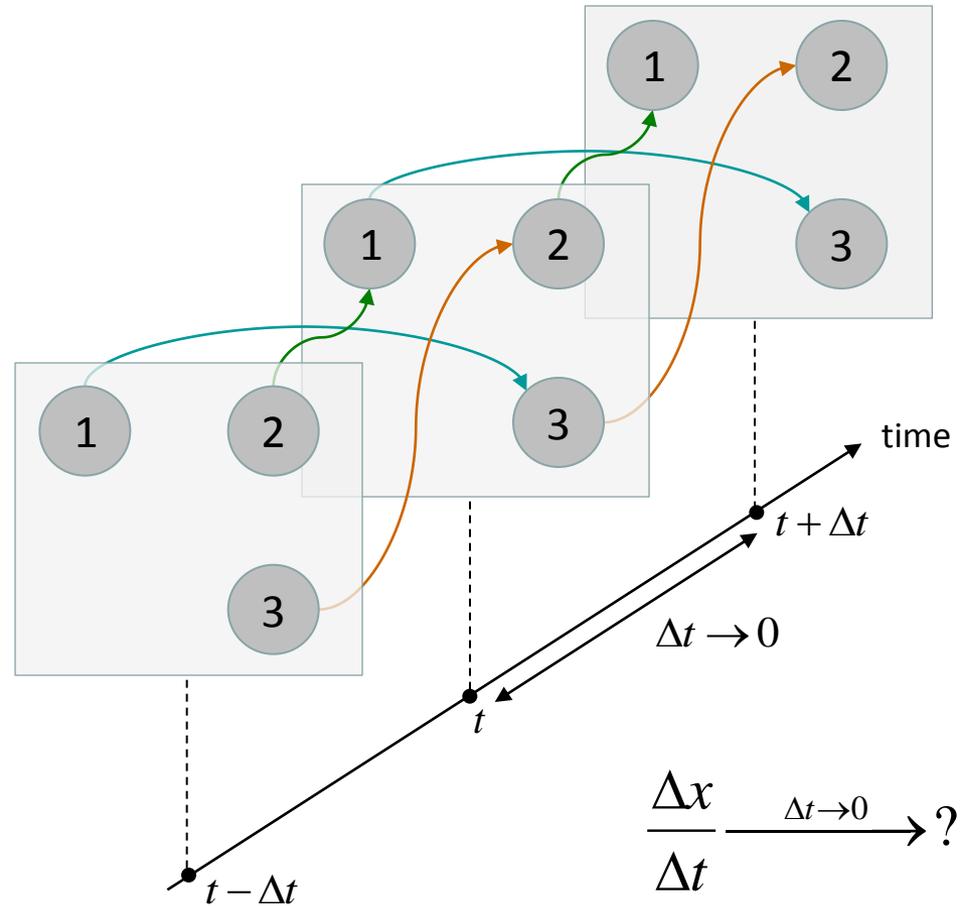
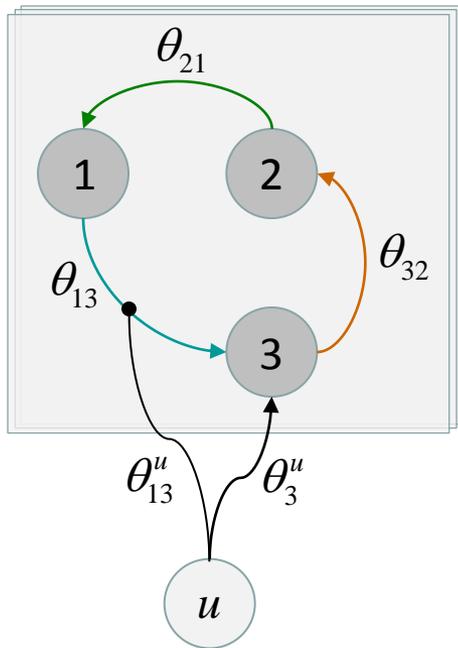
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# Dynamical systems theory

*motivation*

$$u \xrightarrow{\theta} x \xrightarrow{\varphi} y$$



# Dynamical systems theory

## exponentials

We use the following shorthand for a time derivative

$$\dot{x} = \frac{dx}{dt}$$

The exponential function  $x = \exp(t)$  is invariant to differentiation. Hence

$$\dot{x} = \exp(t)$$

and

$$\dot{x} = x$$

Hence  $\exp(t)$  is the solution of the above differential equation.

# Dynamical systems theory

## initial values and fixed points

An exponential increase ( $a > 0$ ) or decrease ( $a < 0$ ) from initial condition  $x_0$

$$x = x_0 \exp(at)$$

has derivative

$$\dot{x} = ax_0 \exp(at)$$

The top equation is therefore the solution of the differential equation

$$\dot{x} = ax$$

with initial condition  $x_0$ .

The values of  $x$  for which  $\dot{x} = 0$  are referred to as Fixed Points (FPs). For the above the only fixed point is at  $x = 0$ .

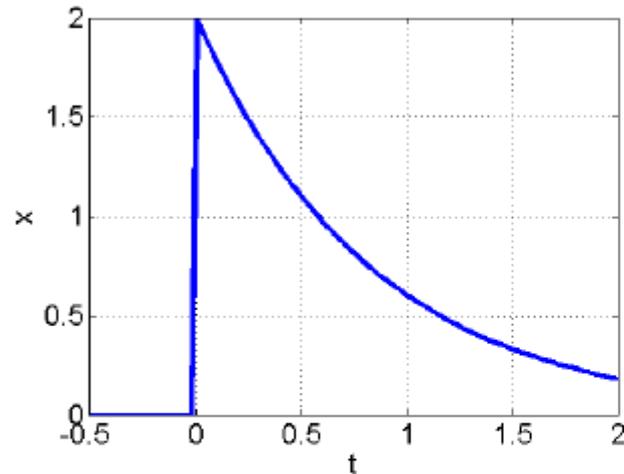
# Dynamical systems theory

## time constants

The figure shows

$$\dot{x} = ax$$

with  $a = -1.2$  and initial value  $x_0 = 2$ .



The time constant is  $\tau = -1/a$ .

The time at which  $x$  decays to half its initial value is

$$\tau_h = \frac{1}{a} \log(1/2)$$

which equals  $\tau_h = 0.58$ .

# Dynamical systems theory

## matrix exponential

If  $x$  is a vector whose evolution is governed by a system of linear differential equations we can write

$$\dot{x} = Ax$$

where  $A$  describes the linear dependencies.

The only fixed point is at  $x = 0$ .

For initial conditions  $x_0$  the above system has solution

$$x_t = \exp(At)x_0$$

where  $\exp(At)$  is the matrix exponential (written `expm` in matlab) (Moler and Van Loan, 2003).

# Dynamical systems theory

## eigendecomposition of the Jacobian

The equation

$$\dot{x} = Ax$$

can be understood by representing  $A$  with an eigendecomposition, with eigenvalues  $\lambda_k$  and eigenvectors  $q_k$  that satisfy (Strang, p. 255)

$$A = Q\Lambda Q^{-1}$$

We can then use the identity

$$\exp(A) = Q \exp(\Lambda) Q^{-1}$$

Because  $\Lambda$  is diagonal, the matrix exponential simplifies to a simple exponential function over each diagonal element.

# Dynamical systems theory

## dynamical modes

This tells us that the original dynamics

$$\dot{x} = Ax$$

has a solution

$$x_t = \exp(At)$$

that can be represented as a linear sum of  $k$  independent dynamical modes

$$x_t = \sum_k q_k \exp(\lambda_k t)$$

where  $q_k$  and  $\lambda_k$  are the  $k$ th eigenvector and eigenvalue of  $A$ . For  $\lambda_k > 0$  we have an unstable mode.

For  $\lambda_k < 0$  we have a stable mode, and the magnitude of  $\lambda_k$  determines the time constant of decay to the fixed point.

The eigenvalues can also be complex. This gives rise to oscillations.

# Dynamical systems theory

## spirals

A spiral occurs in a two-dimensional system when both eigenvalues are a complex conjugate pair. For example (Wilson, 1999)

$$\begin{bmatrix} \dot{x}_1 \\ \dot{x}_2 \end{bmatrix} = \begin{bmatrix} -2 & -16 \\ 4 & -2 \end{bmatrix} \begin{bmatrix} x_1 \\ x_2 \end{bmatrix}$$

has

$$\lambda_1 = -2 + 8i$$

$$\lambda_2 = -2 - 8i$$

giving solutions (for initial conditions  $x = [1, 1]^T$ )

$$x_1(t) = \exp(-2t) [\cos(8t) - 2 \sin(8t)]$$

$$x_2(t) = \exp(-2t) [\cos(8t) + 0.5 \sin(8t)]$$

# Dynamical systems theory

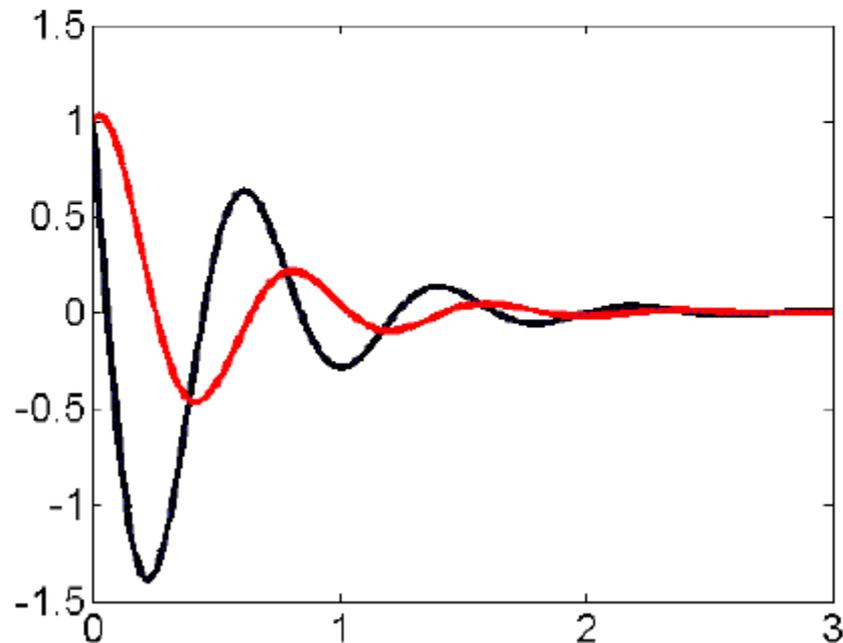
## spirals

We plot time series solutions

$$x_1(t) = \exp(-2t) (\cos(8t) - 2 \sin(8t))$$

$$x_2(t) = \exp(-2t) (\cos(8t) + 0.5 \sin(8t))$$

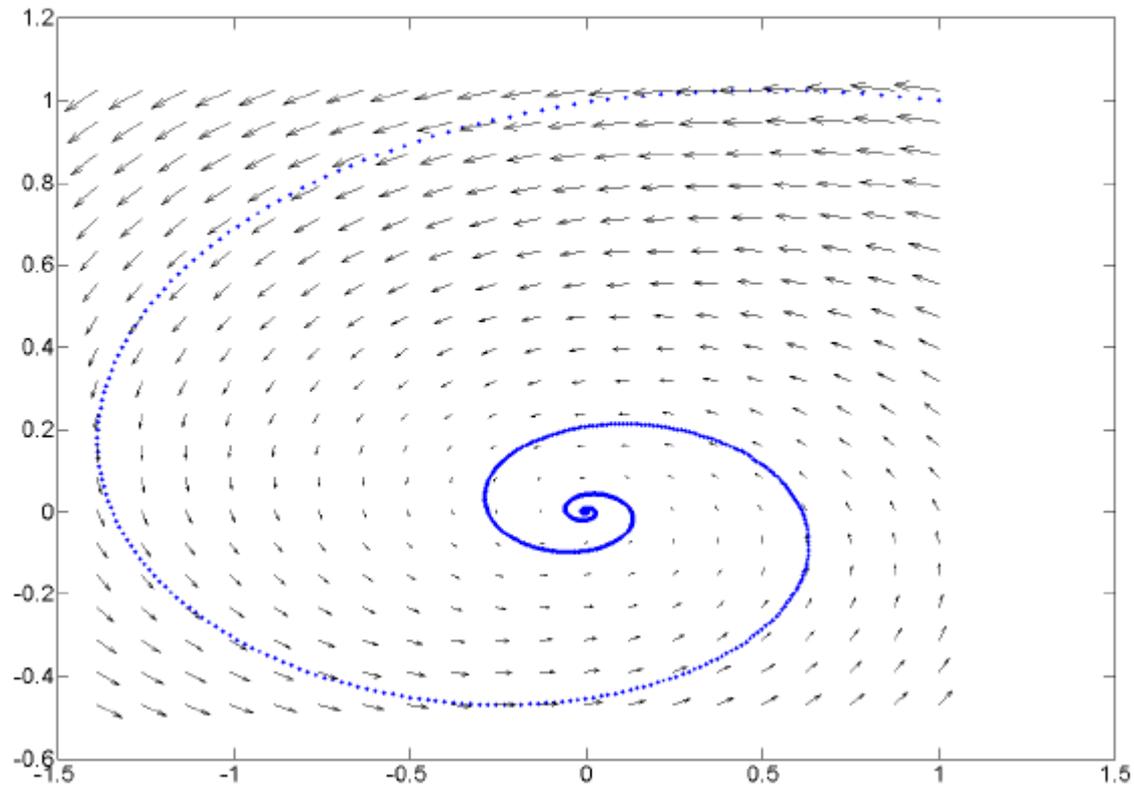
for  $x_1$  (black) and  $x_2$  (red).



# Dynamical systems theory

## spiral state-space

Plotting  $x_2$  against  $x_1$  gives the state-space representation.



# Dynamical systems theory

## embedding

Univariate higher order differential equations can be represented as multivariate first order DEs.

For example

$$\ddot{v} = \frac{H}{\tau} u_t - \frac{2}{\tau} \dot{v} - \frac{1}{\tau^2} v$$

can be written as

$$\begin{aligned} \dot{v} &= c \\ \dot{c} &= \frac{H}{\tau} u_t - \frac{2}{\tau} c - \frac{1}{\tau^2} v \end{aligned}$$

# Dynamical systems theory

## kernels and convolution

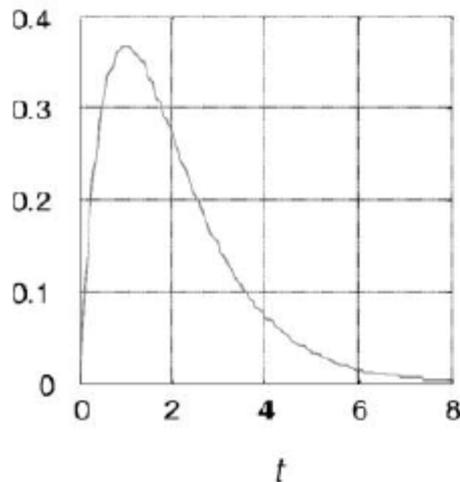
The previous differential equation has a solution given by the integral

$$v(t) = \int u(t)h(t - t')dt'$$

where

$$h(t) = \frac{H}{\tau}t \exp(-t/\tau)$$

is a kernel. In this case it is an alpha function synapse with magnitude  $H$  and time constant  $\tau$



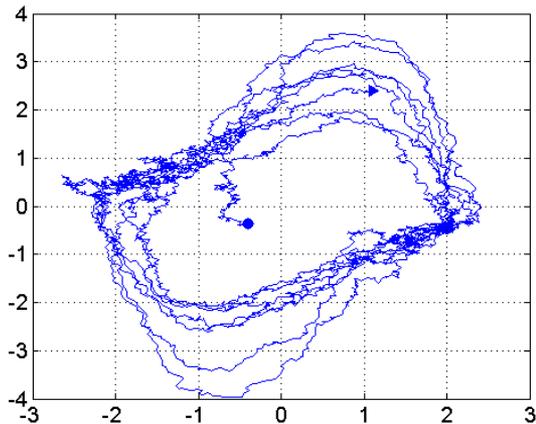
The previous integral can be written as

$$v = u \otimes h$$

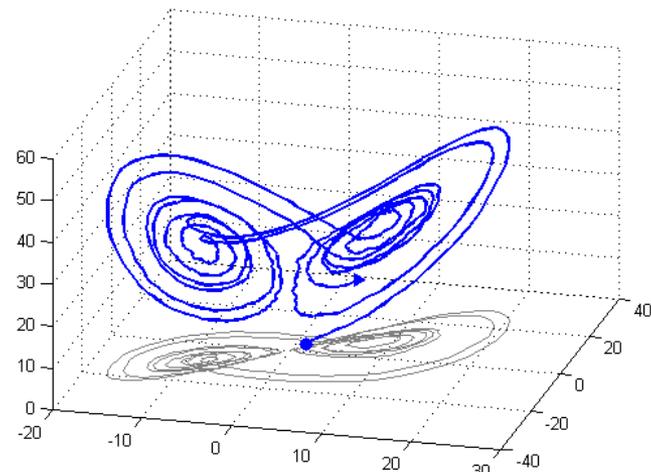
# Dynamical systems theory

## summary

- Motivation: modelling reciprocal influences
- Link between the integral (convolution) and differential (ODE) forms
- System stability and dynamical modes can be derived from the system's Jacobian:
  - $D > 0$ : fixed points
  - $D > 1$ : spirals
  - $D > 1$ : limit cycles (e.g., action potentials)
  - $D > 2$ : metastability (e.g., winnerless competition)



limit cycle (Vand Der Pol)



strange attractor (Lorenz)

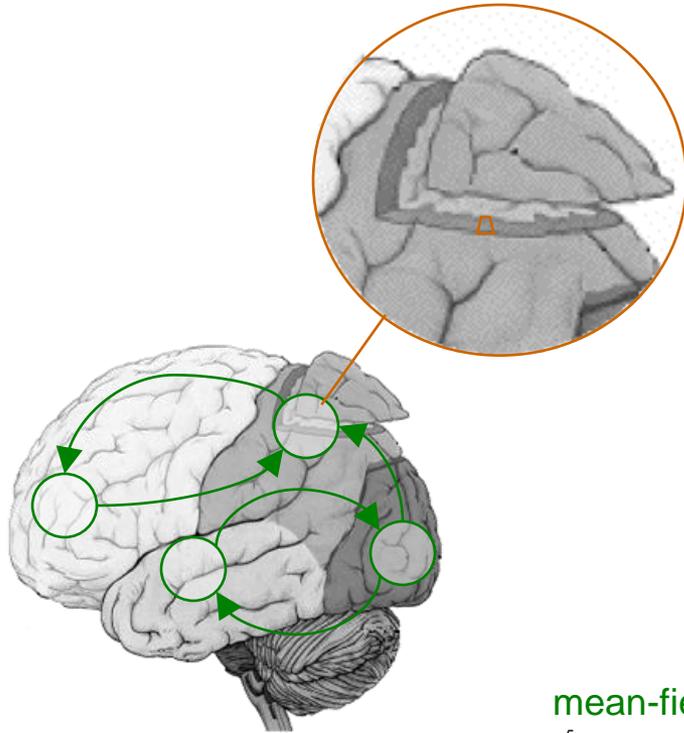
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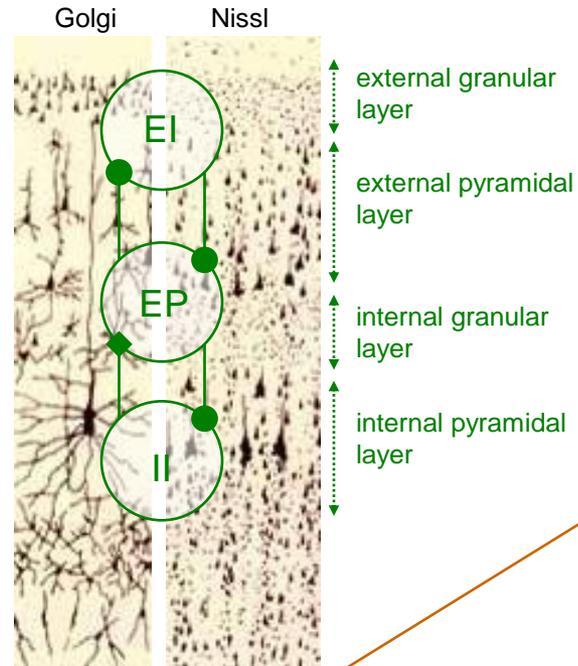
# Neural ensembles dynamics

## DCM for M/EEG: *systems of neural populations*

macro-scale



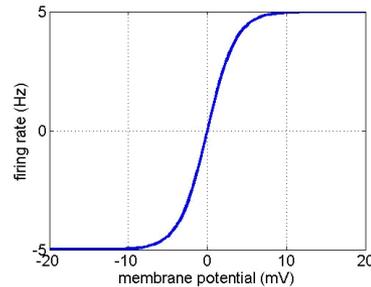
meso-scale



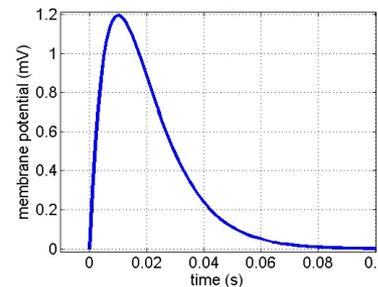
micro-scale



mean-field firing rate

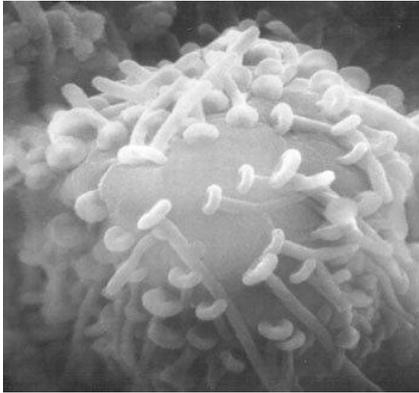


synaptic dynamics



# Neural ensembles dynamics

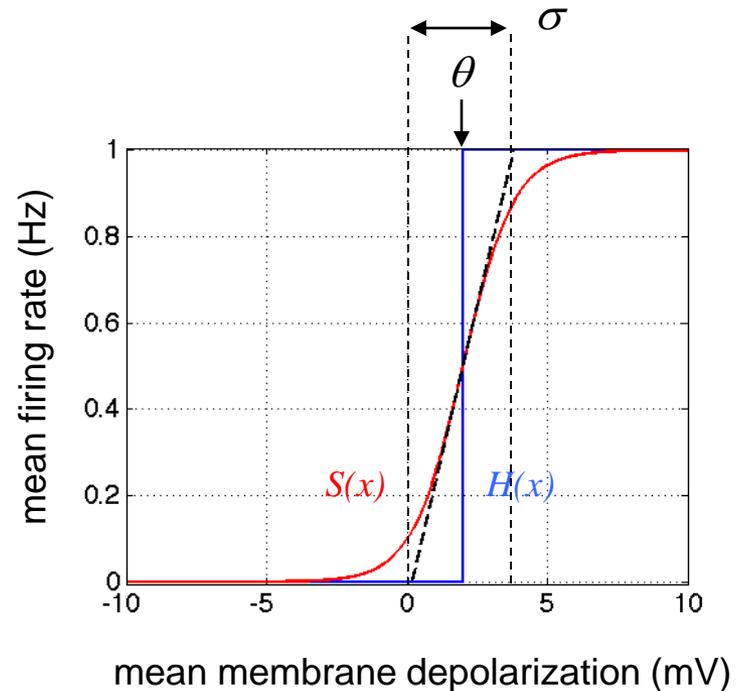
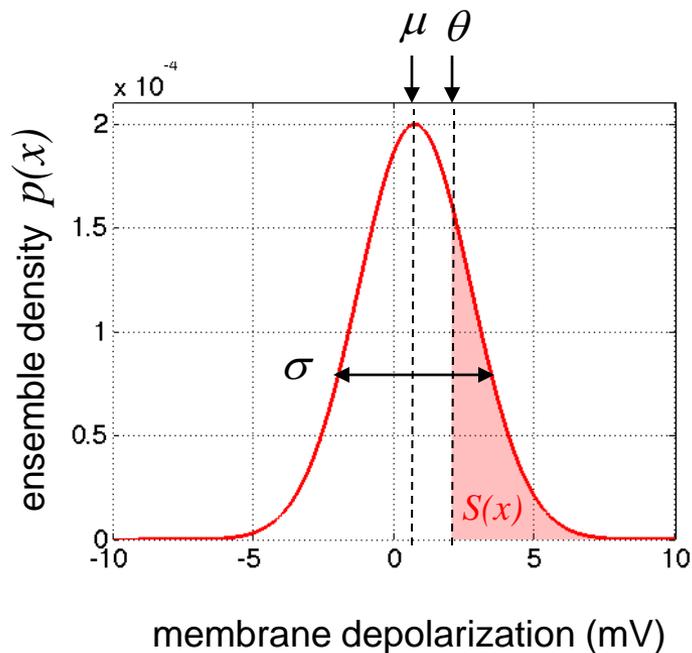
DCM for M/EEG: *from micro- to meso-scale*



$x_j(t)$ : post-synaptic potential of  $j^{\text{th}}$  neuron within its ensemble

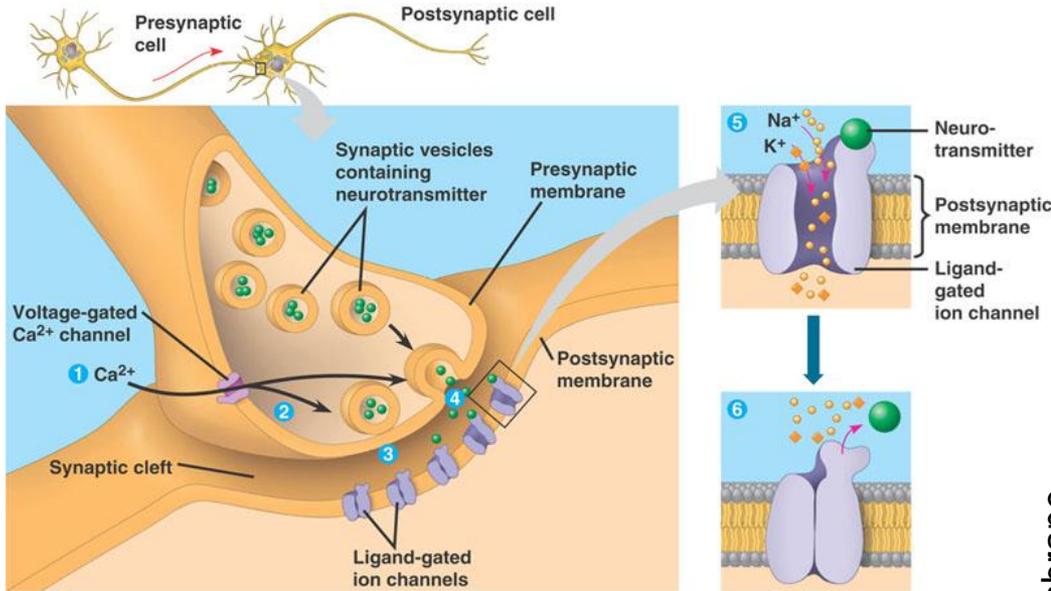
$$\frac{1}{N-1} \sum_{j \neq i} H(x_j(t) - \theta) \xrightarrow{N \rightarrow \infty} \int H(x(t) - \theta) p(x(t)) dx$$

$\approx S(\mu)$  **mean-field firing rate**

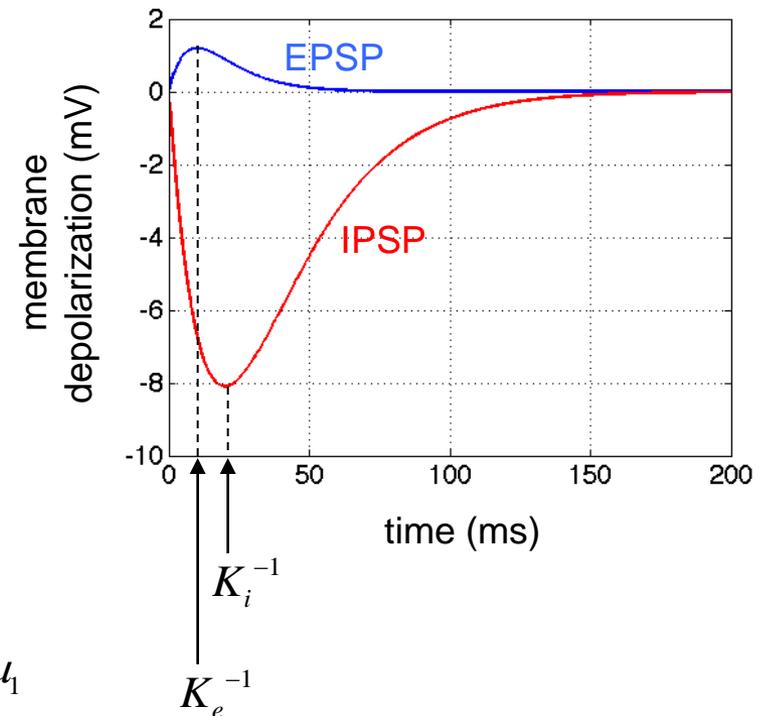


# Neural ensembles dynamics

## DCM for M/EEG: synaptic dynamics



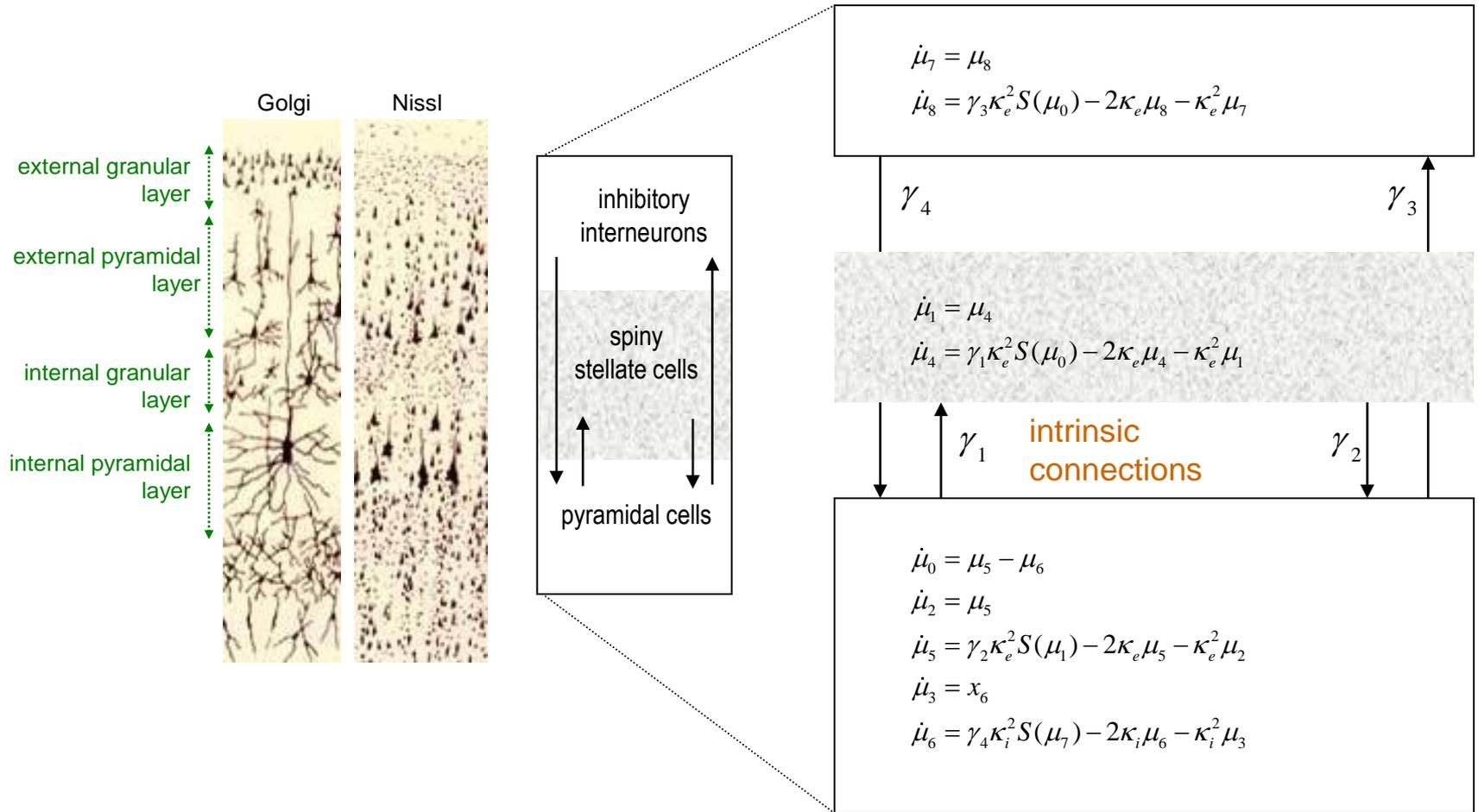
post-synaptic potential



$$\begin{cases} \dot{\mu}_1 = \mu_2 \\ \dot{\mu}_2 = \kappa_{i/e}^2 S(\square) - 2\kappa_{i/e} \mu_2 - \kappa_{i/e}^2 \mu_1 \end{cases}$$

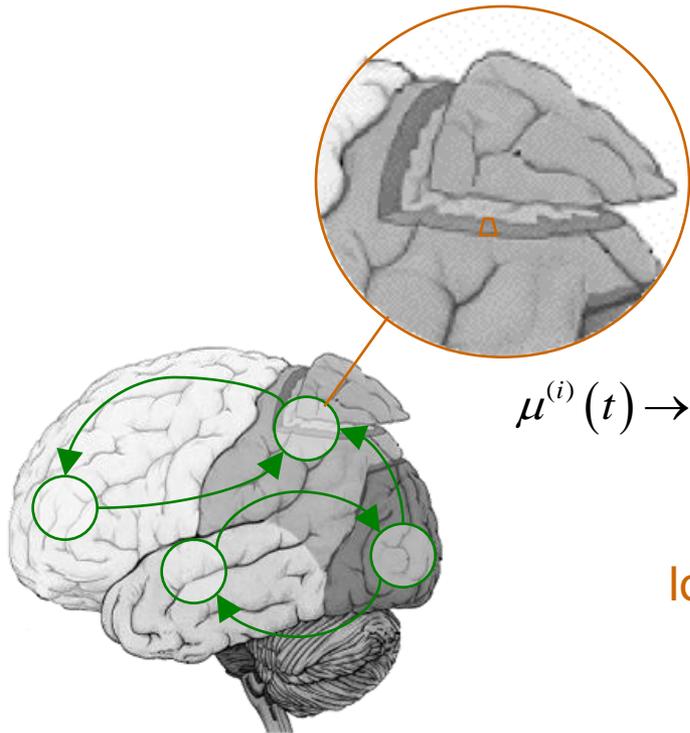
# Neural ensembles dynamics

DCM for M/EEG: *intrinsic connections within the cortical column*

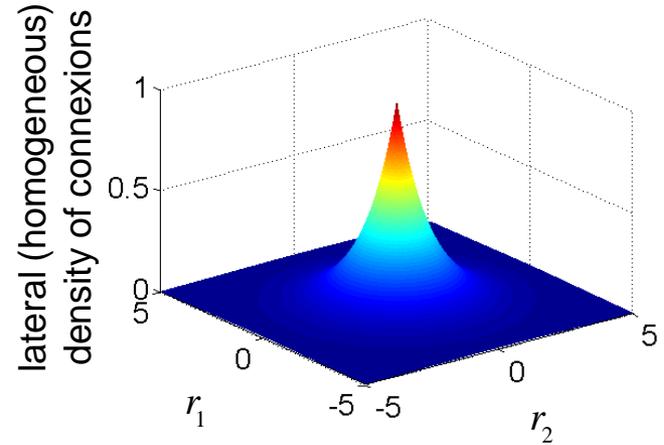


# Neural ensembles dynamics

DCM for M/EEG: *from meso- to macro-scale*



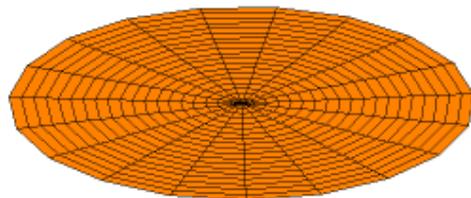
$$\mu^{(i)}(t) \rightarrow \mu^{(i)}(\mathbf{r}, t)$$



local wave propagation equation (neural field):

$$\left( \frac{\partial^2}{\partial t^2} + 2\kappa \frac{\partial}{\partial t} + \kappa^2 - \frac{3}{2} c^2 \nabla^2 \right) \mu^{(i)}(\mathbf{r}, t) \approx c\kappa \zeta^{(i)}(\mathbf{r}, t)$$

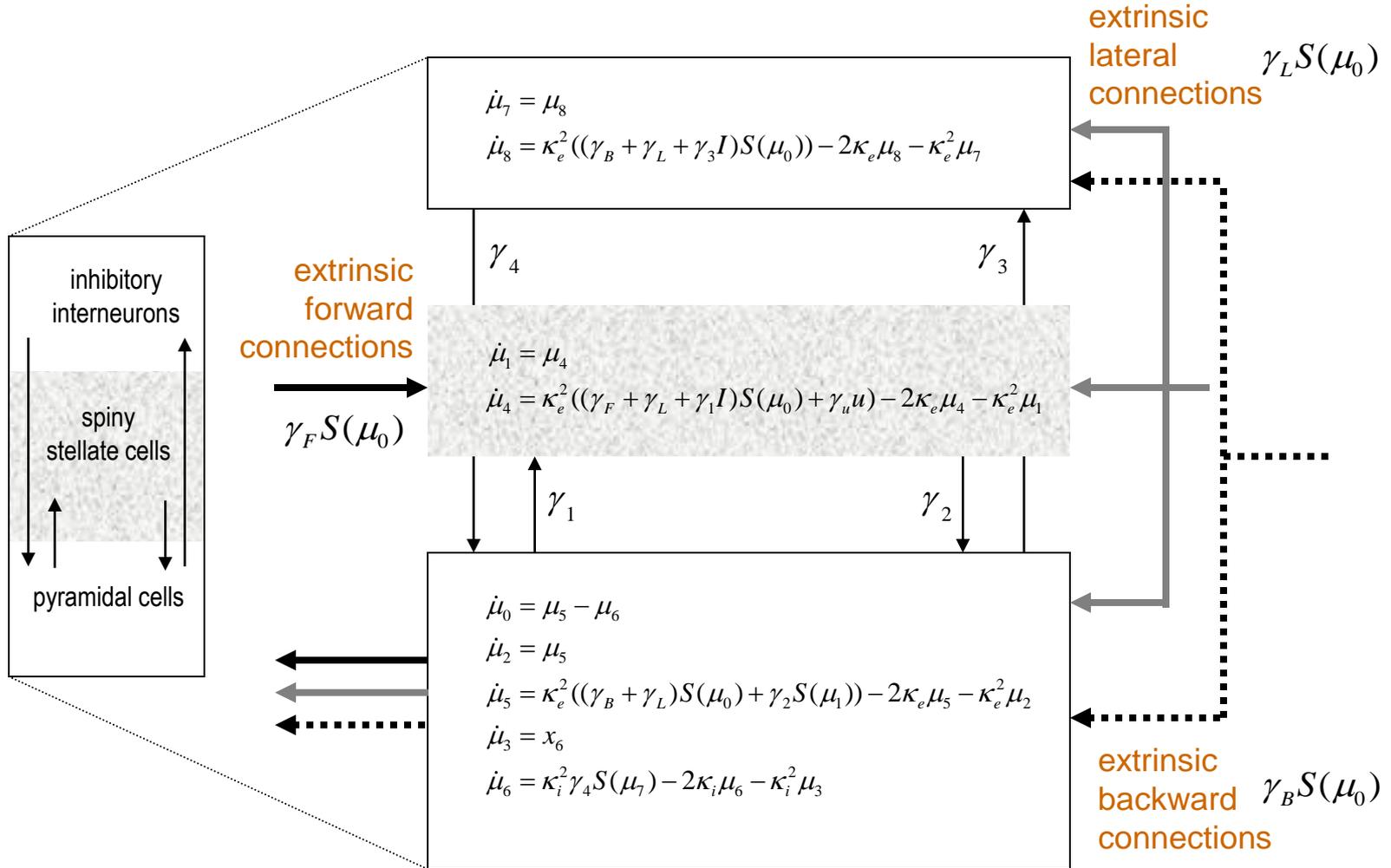
$$\zeta^{(i)} = \sum_{i'} \gamma_{ii'} S(\mu^{(i')})$$



0<sup>th</sup>-order approximation: standing wave

# Neural ensembles dynamics

DCM for M/EEG: *extrinsic connections between brain regions*

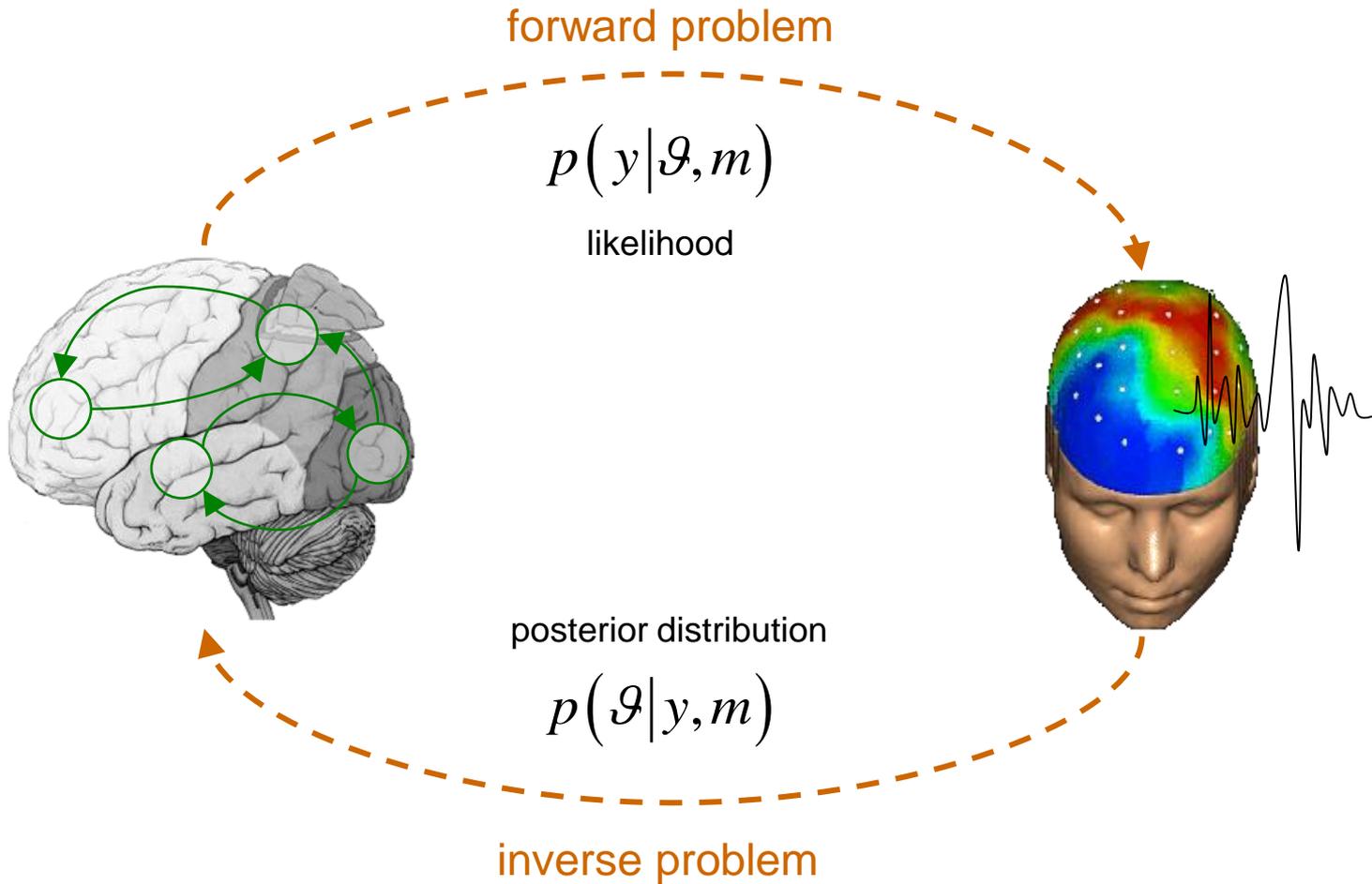


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# Bayesian inference

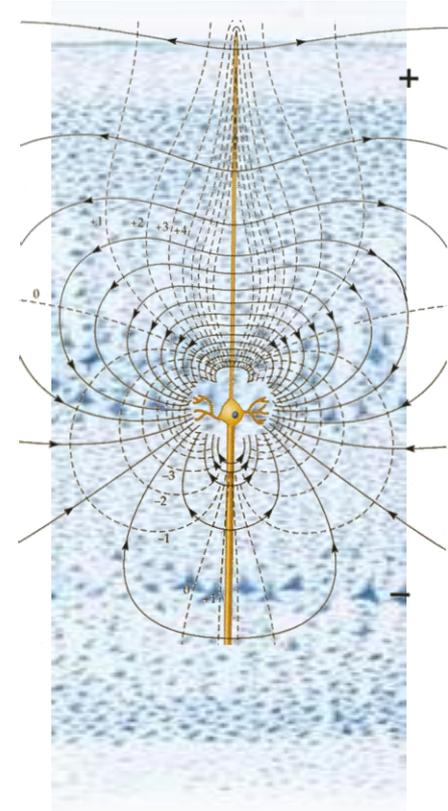
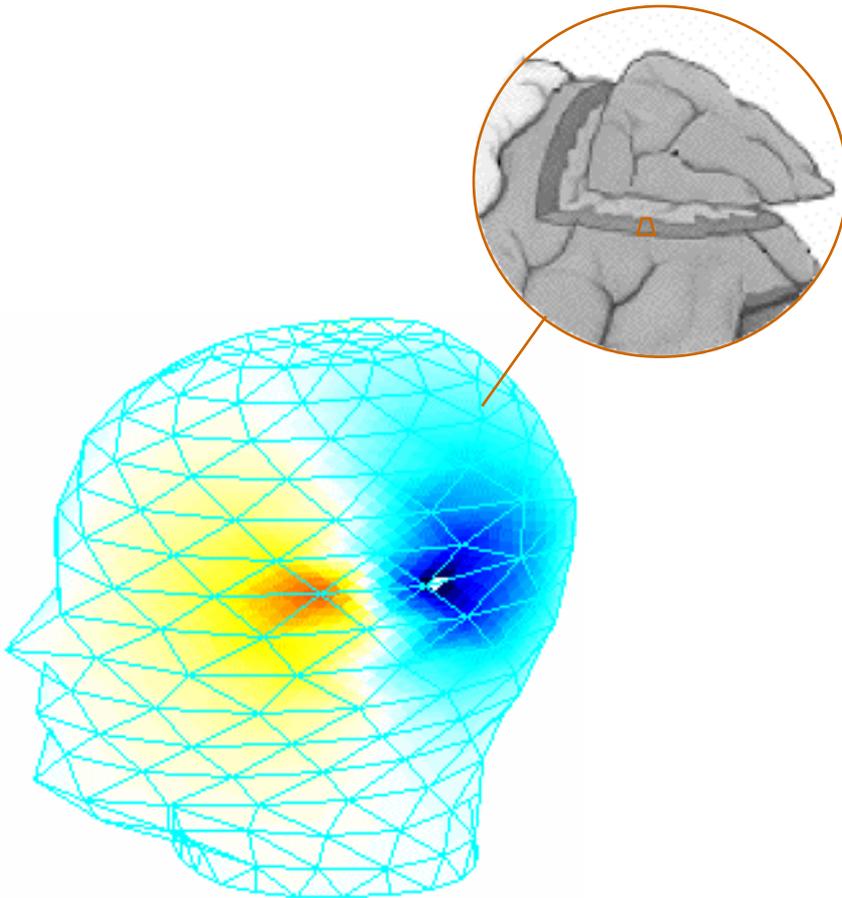
*forward and inverse problems*



# Bayesian inference

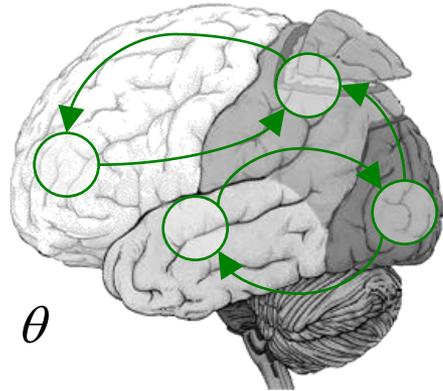
*the electromagnetic forward problem*

$$\mathbf{y}(t) = \sum_i \mathbf{L}^{(i)} \mathbf{w}_0^{(i)} \sum_j \beta_j \mu^{(ij)}(t) + \varepsilon(t)$$

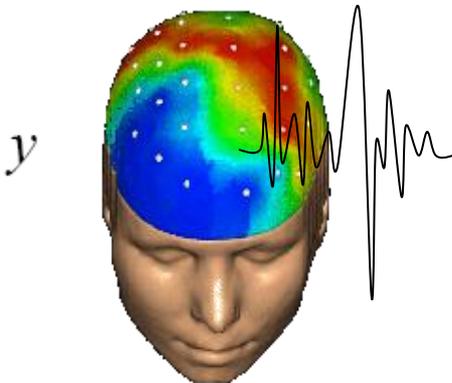


# Bayesian paradigm

*deriving the likelihood function*

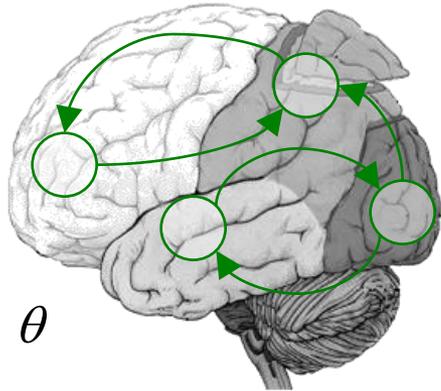


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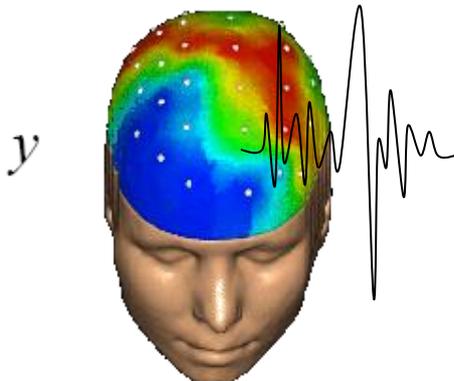


# Bayesian paradigm

*likelihood, priors and the model evidence*



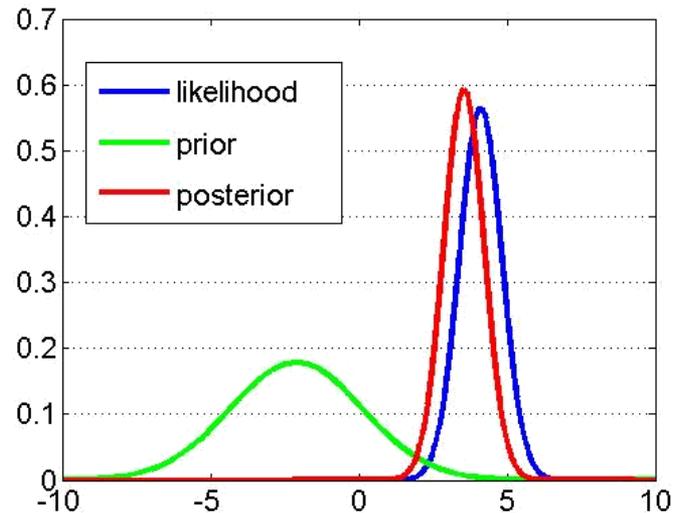
generative model  $m$



Likelihood:  $p(y|\theta, m)$

Prior:  $p(\theta|m)$

Bayes rule:  $p(\theta|y, m) = \frac{p(y|\theta, m) p(\theta|m)}{p(y|m)}$

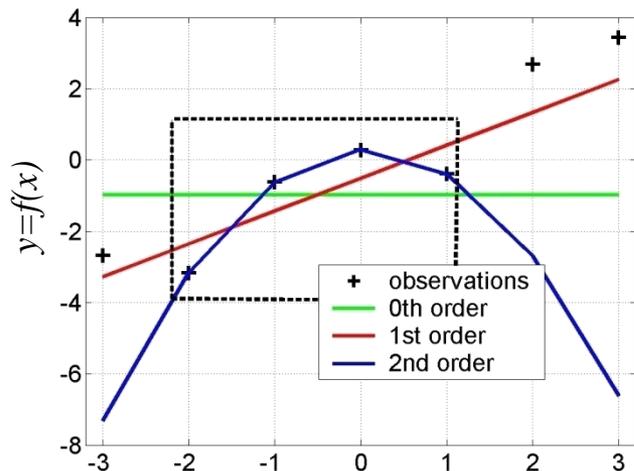
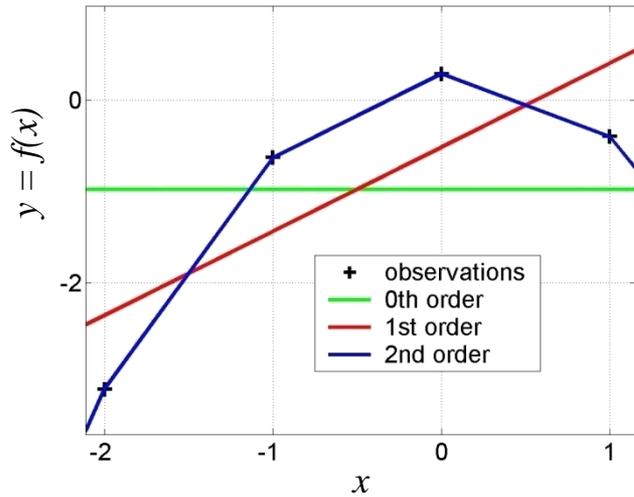


# Bayesian inference

## model comparison

*Principle of parsimony :*

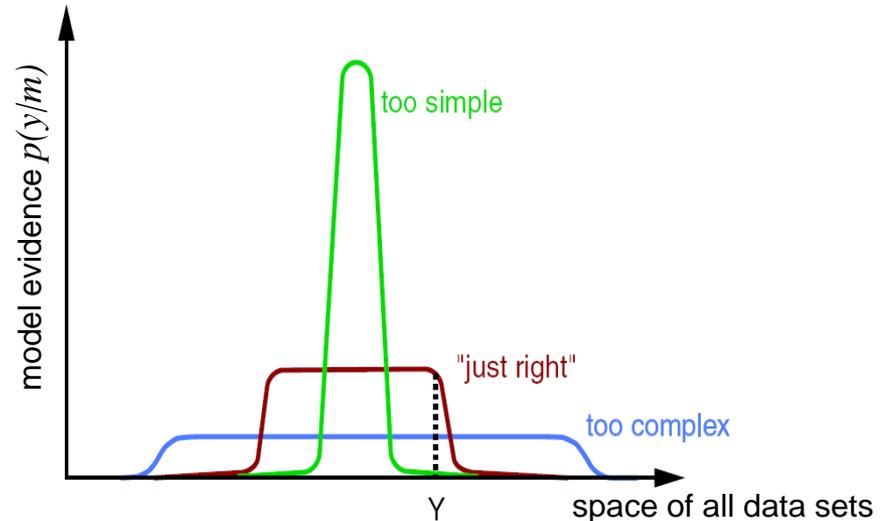
« plurality should not be assumed without necessity »



Model evidence:

$$p(y|m) = \int p(y|\mathcal{G}, m) p(\mathcal{G}|m) d\mathcal{G}$$

“Occam’s razor” :



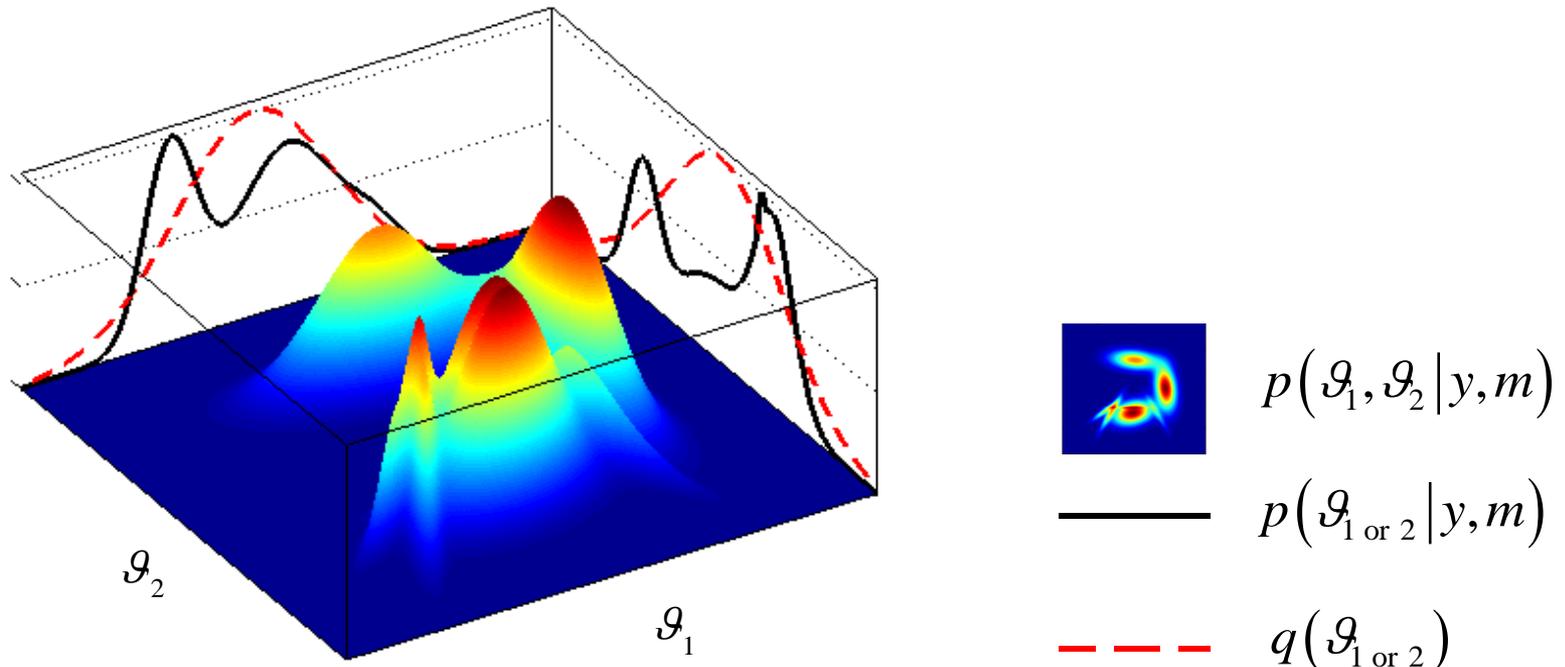
# Bayesian inference

*the variational Bayesian approach*

$$\ln p(y|m) = \underbrace{\langle \ln p(\mathcal{G}, y|m) \rangle_q + S(q)}_{\text{free energy : functional of } q} + D_{KL}(q(\mathcal{G}); p(\mathcal{G}|y, m))$$

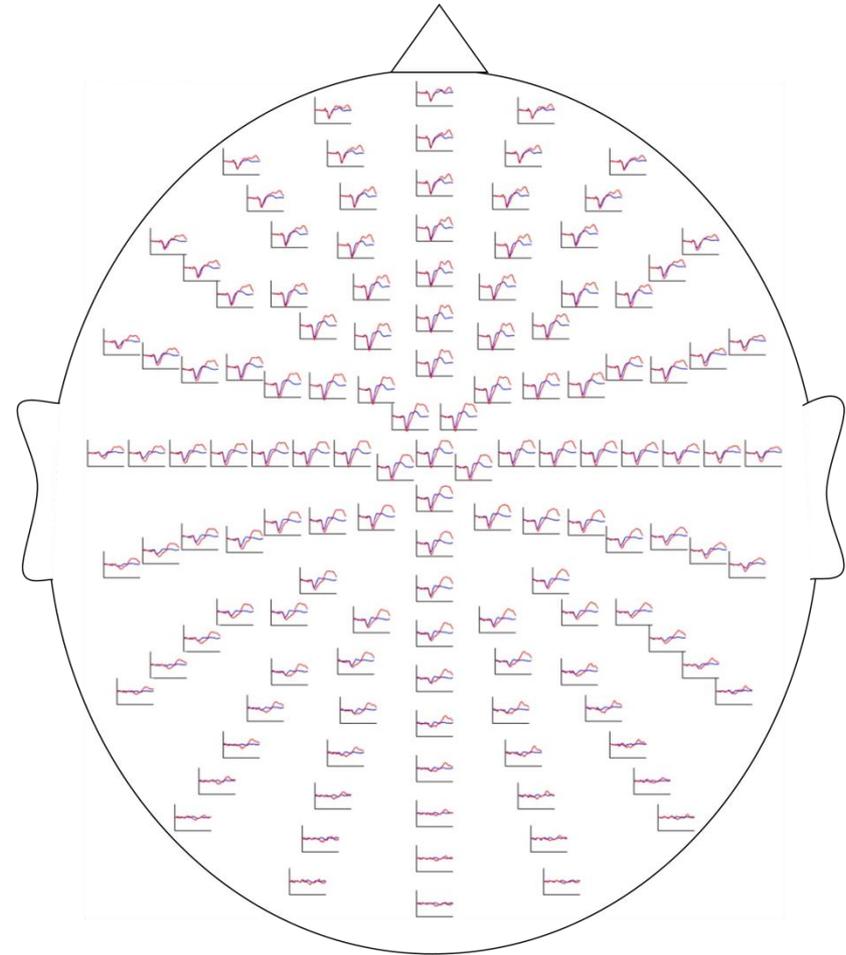
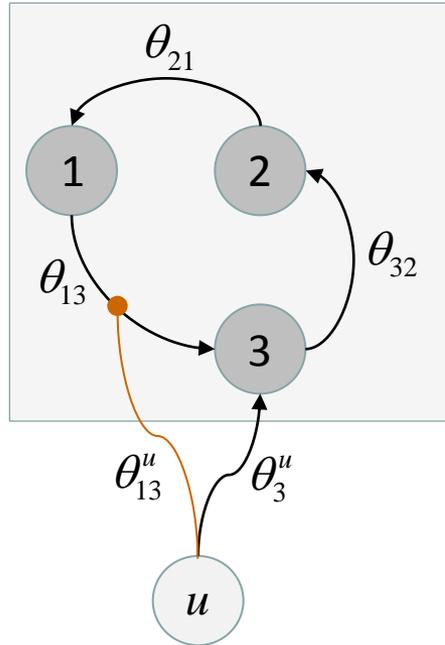
free energy : functional of  $q$

*mean-field*: approximate marginal posterior distributions:  $\{q(\mathcal{G}_1), q(\mathcal{G}_2)\}$



# Bayesian inference

*DCM: key model parameters*



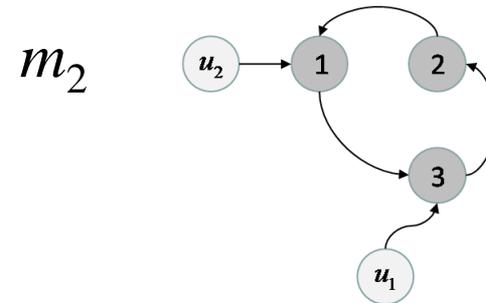
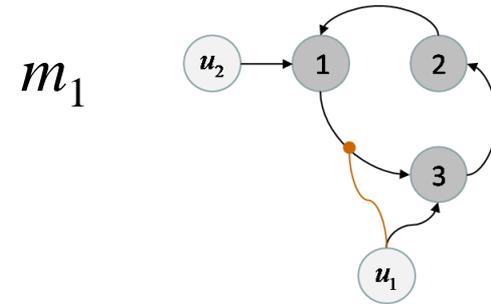
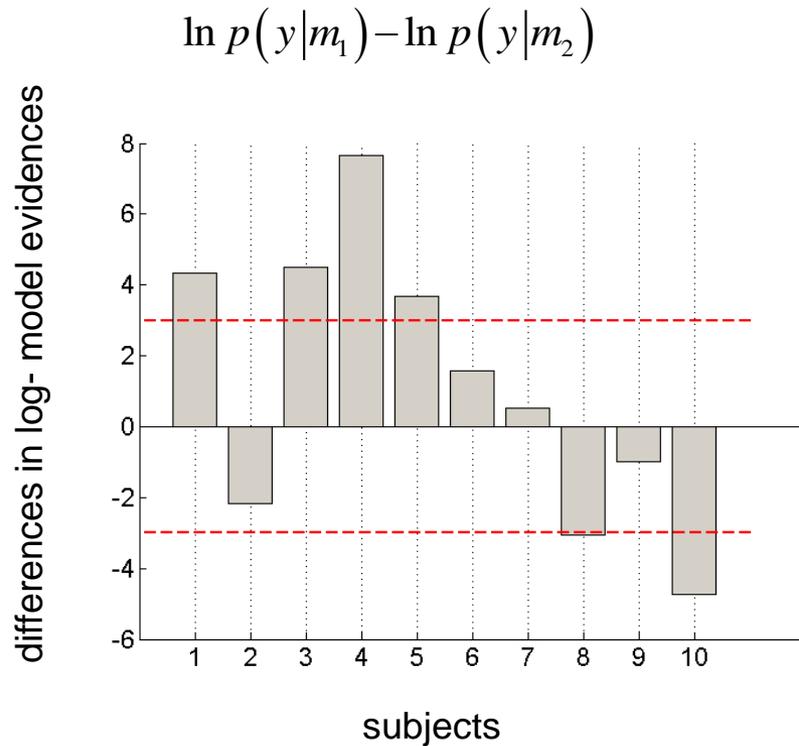
$(\theta_{21}, \theta_{32}, \theta_{13})$  state-state coupling

$\theta_3^u$  input-state coupling

$\theta_{13}^u$  input-dependent modulatory effect

# Bayesian inference

## *model comparison for group studies*



fixed effect

assume all subjects correspond to the same model

random effect

assume different subjects might correspond to different models

# Overview

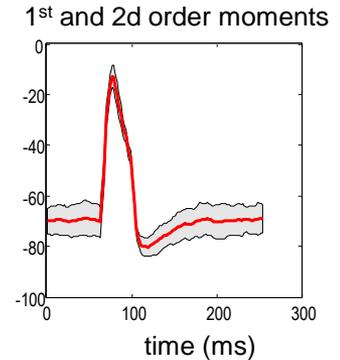
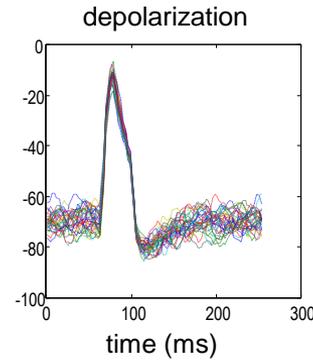
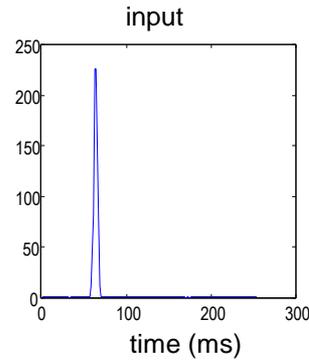
- 1 DCM: introduction
- 2 Dynamical systems theory
- 3 Neural states dynamics
- 4 Bayesian inference
- 5 Conclusion



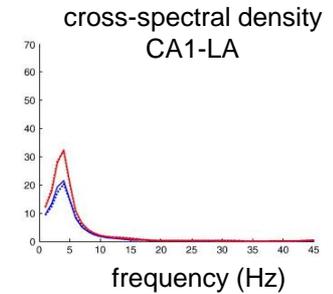
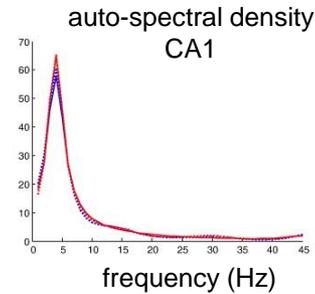
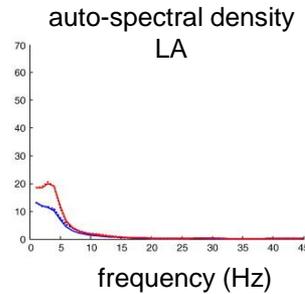
# Conclusion

## DCM for EEG/MEG: variants

- second-order mean-field DCM

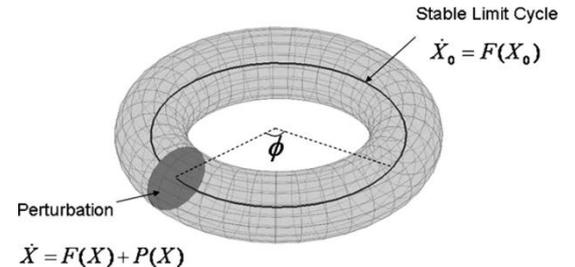
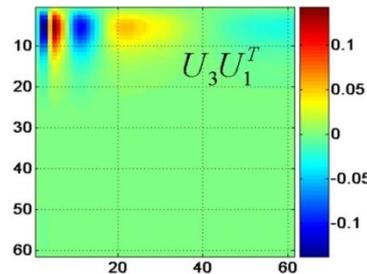


- DCM for steady-state responses



- DCM for induced responses

- DCM for phase coupling



# Conclusion

## *planning a compatible DCM study*

- **Suitable experimental design:**
  - any design that is suitable for a GLM
  - preferably multi-factorial (e.g. 2 x 2)
    - e.g. one factor that varies the **driving** (sensory) input
    - and one factor that varies the **modulatory** input
- **Hypothesis and model:**
  - define specific *a priori* hypothesis
  - which models are relevant to test this hypothesis?
  - check **existence of effect** on data features of interest
  - there exists formal methods for optimizing the experimental design for the ensuing bayesian model comparison  
[Daunizeau et al., PLoS Comp. Biol., 2011]

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