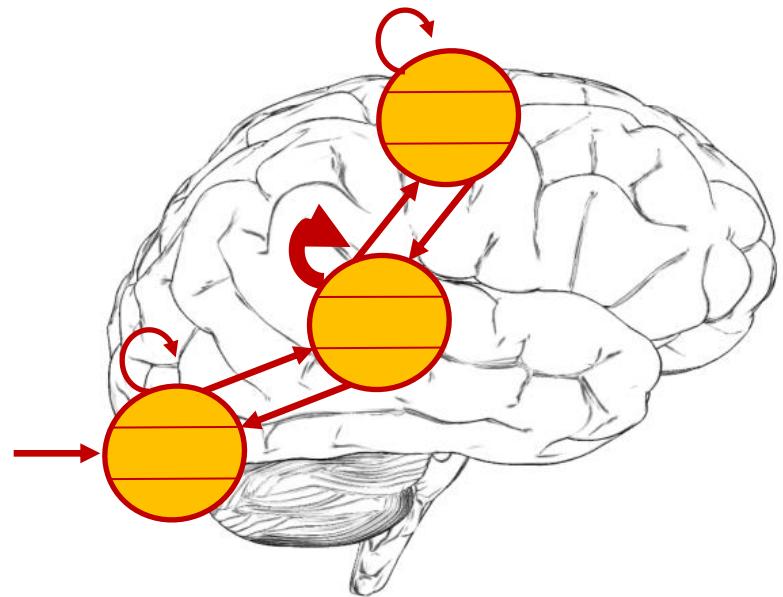


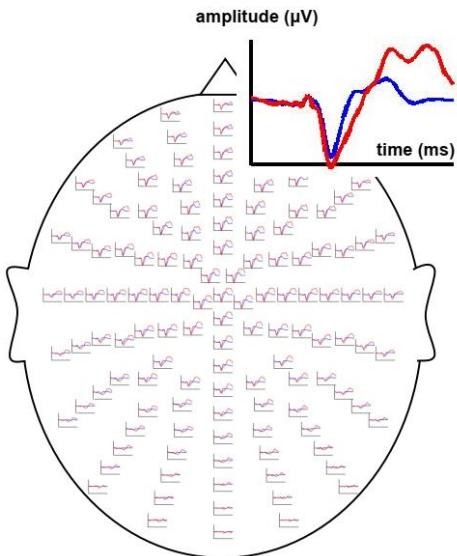
# DCM for evoked responses

Ryszard Auksztulewicz

SPM for M/EEG course



# Modelling aim and approach



Modelling Aim

Explain all data with few parameters

How to ...

Assume data are caused by few interacting brain sources ...

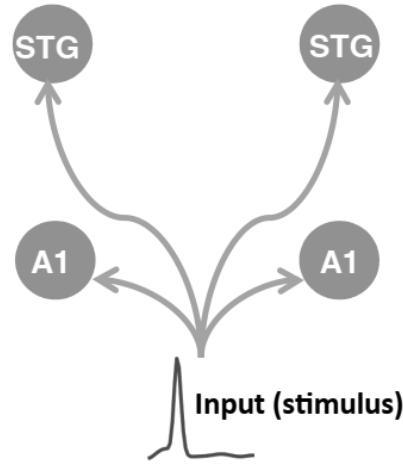
... and / or their respective intrinsic connectivity / intrinsic parameters

\*M/EEG are complex data

Analyses / modelling: in time, frequency,  
time-frequency and space domains

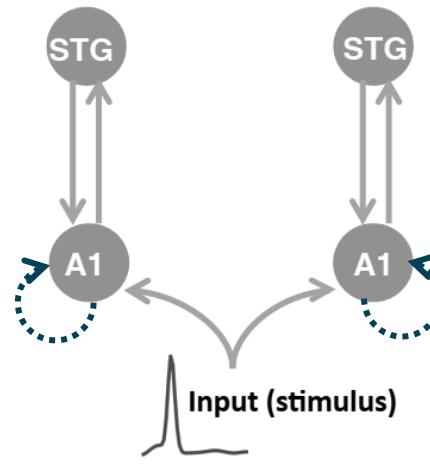
# Conventional analyses vs. DCM

“Conventional” Analysis
Which regions are involved in a task?
Sensor space / functional connectivity



A1 - left and right primary auditory cortex  
 STG - left and right superior temporal gyrus

DCM Analysis
How do regions communicate?
What role do intrinsic connections have?
Source space / effective connectivity



Adapted from Kiebel (n.a.), *Dynamic Causal Modelling for EEG and MEG*, Presentation at TU Dresden;  
 Stoff (n.a.), *DCM for ERP/ERF*, Presentation at UCL

Does network XYZ explain my data better than network XY?

Which XYZ connectivity structure best explains my data?

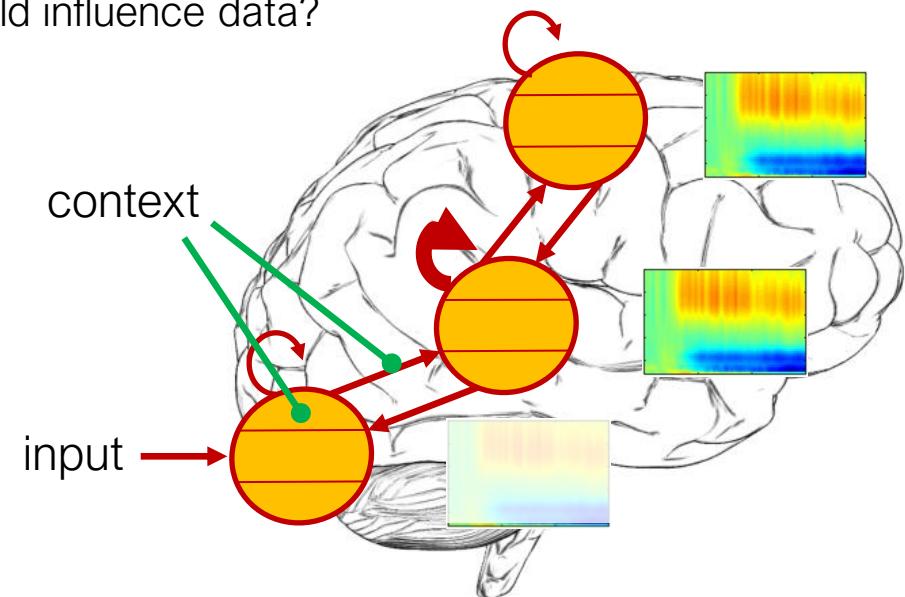
Are X & Y linked in a bottom-up, top-down or recurrent fashion?

Is my effect driven by extrinsic or intrinsic connections?

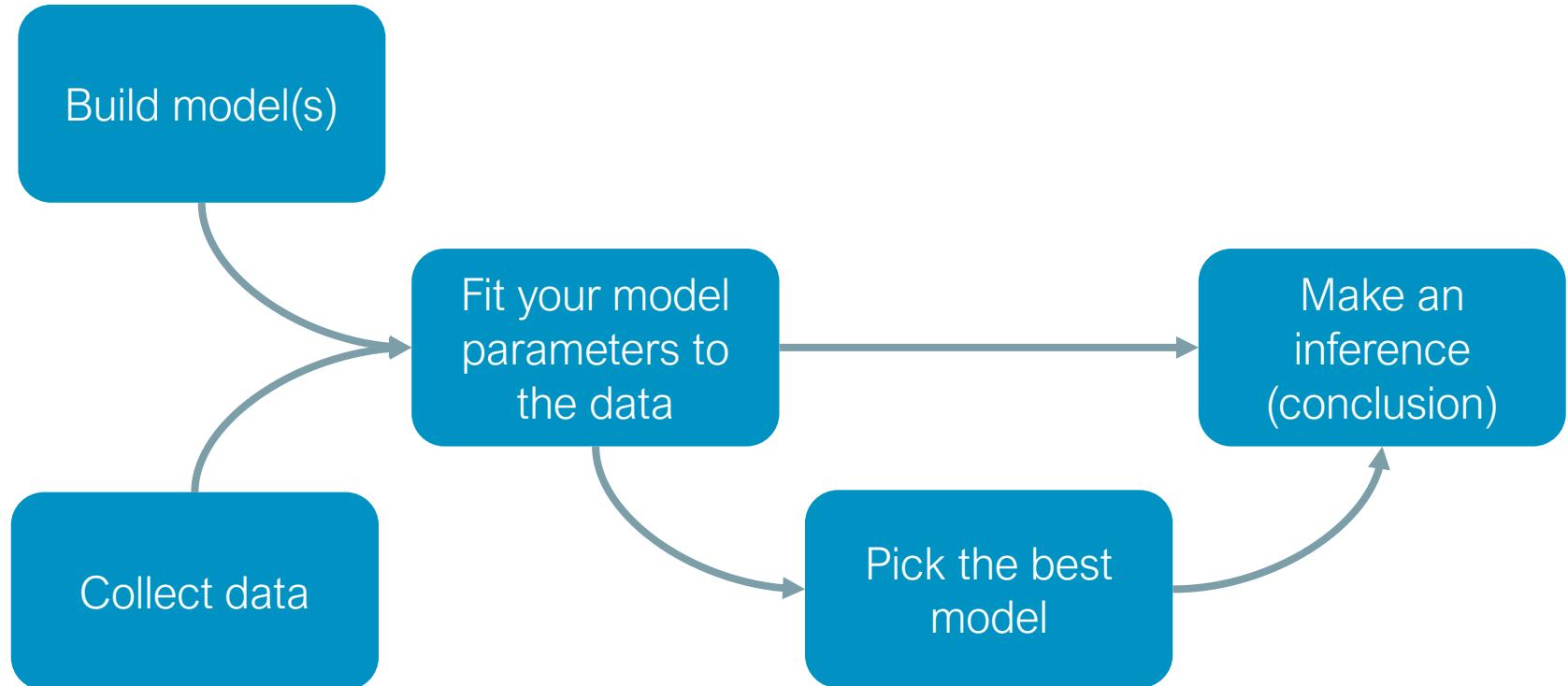
Which neural populations are affected by contextual factors?

Which connections determine observed frequency coupling?

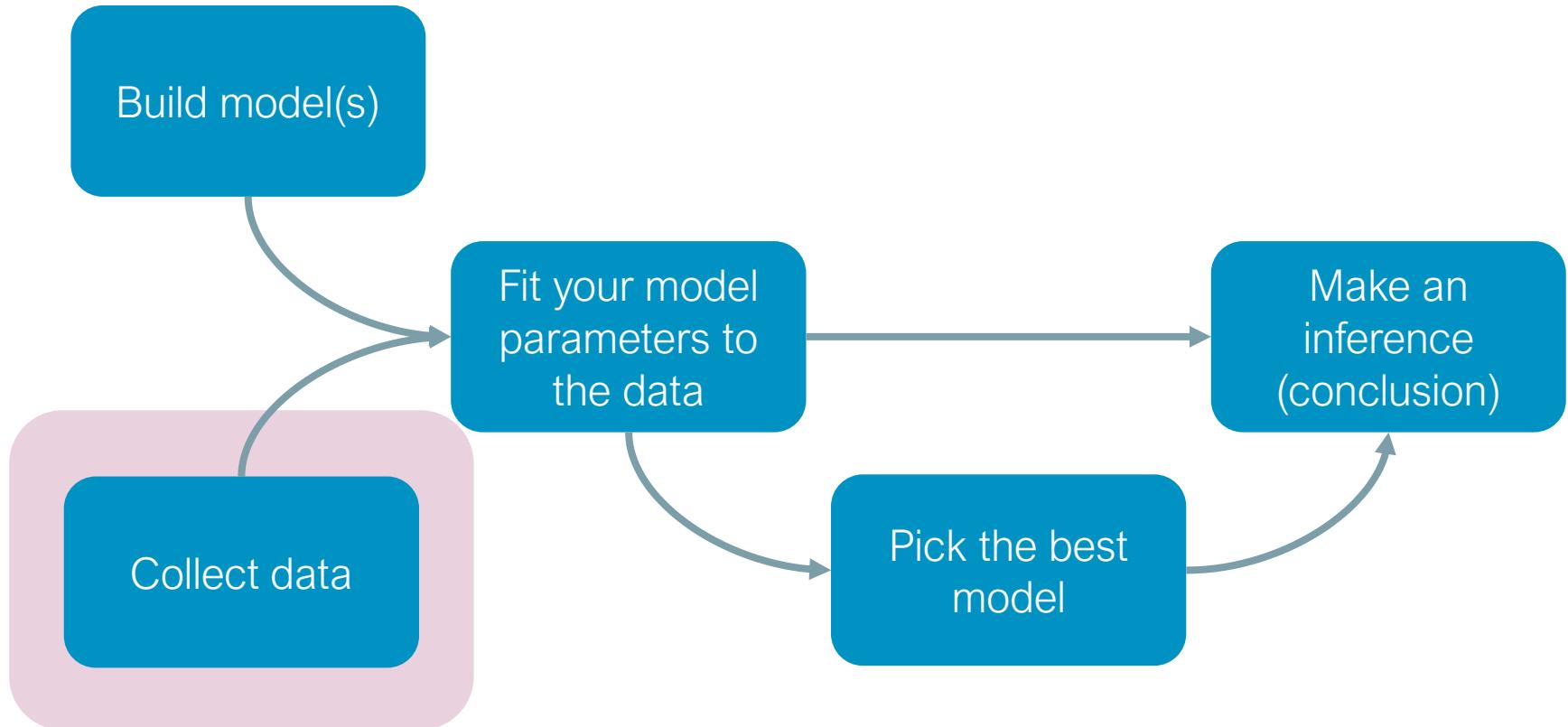
How changing a connection/parameter would influence data?



# The DCM analysis pathway

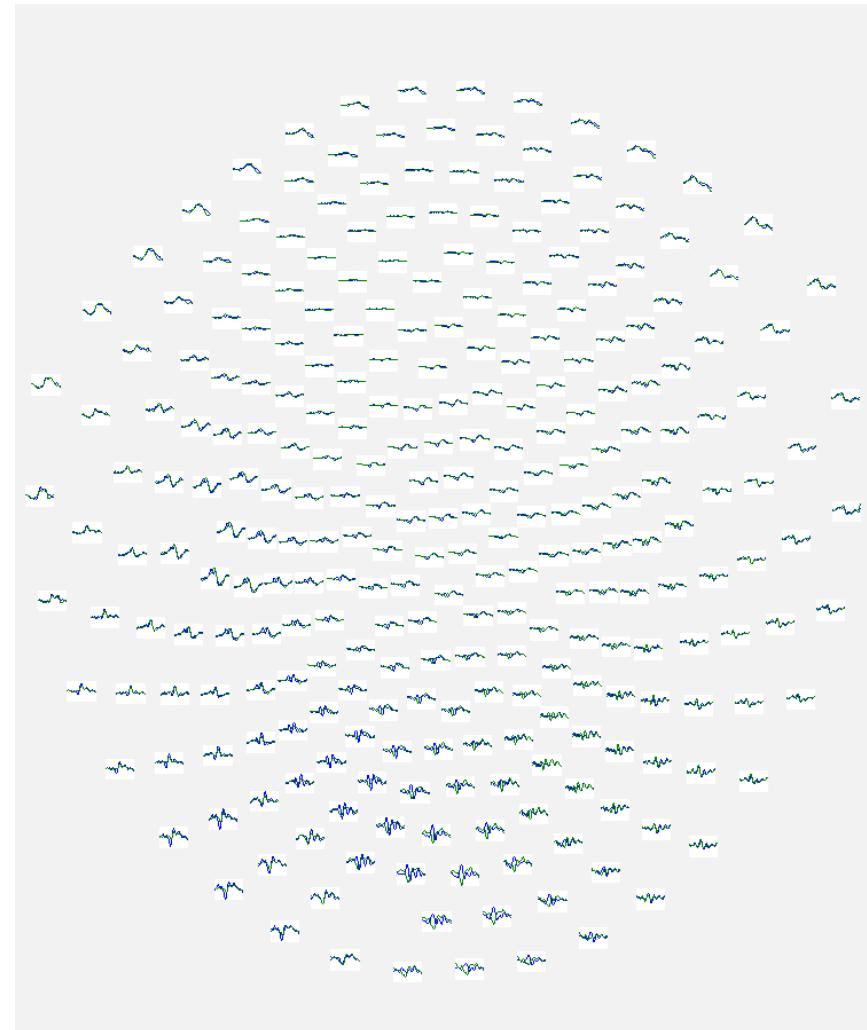


# The DCM analysis pathway

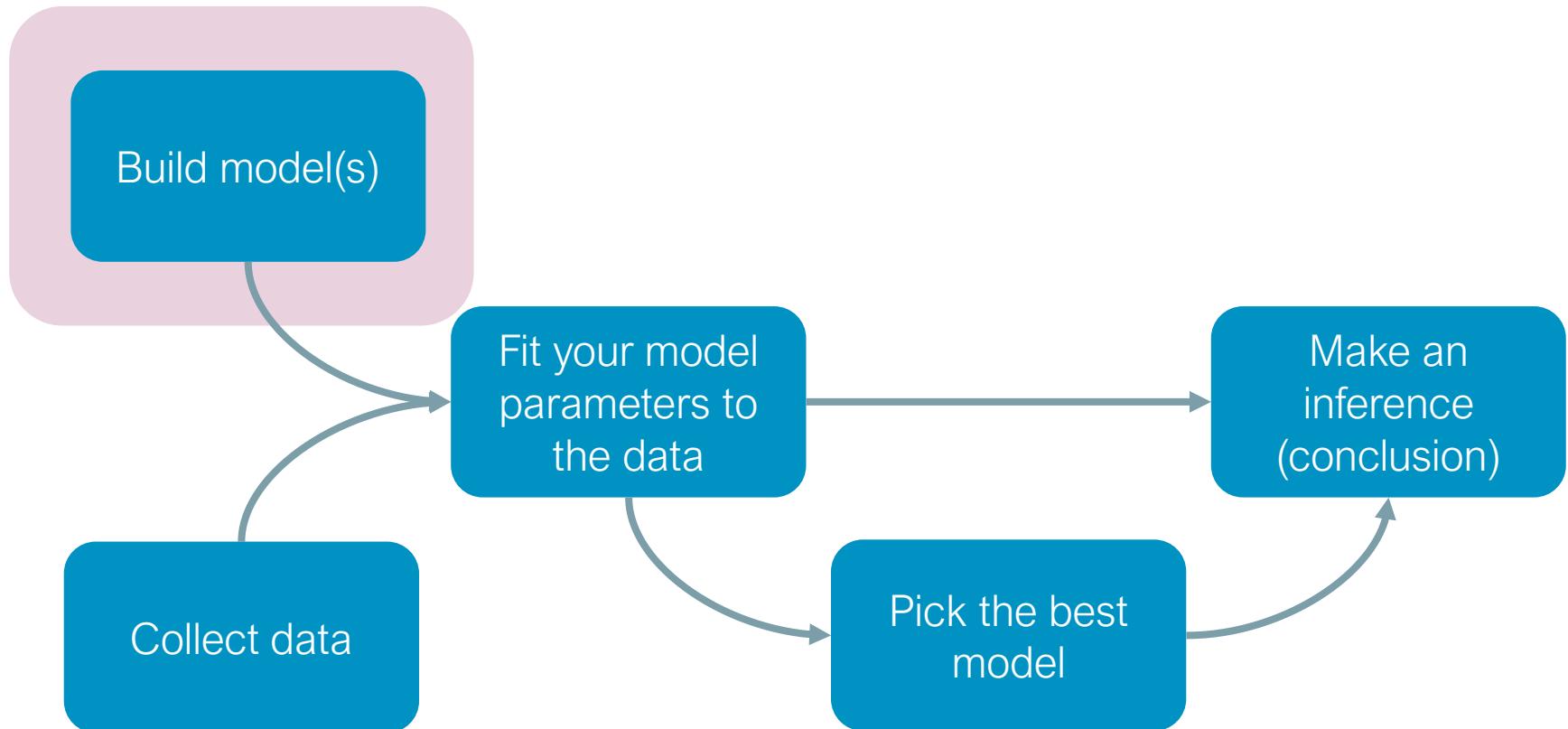


# Data for DCM for ERPs / ERFs

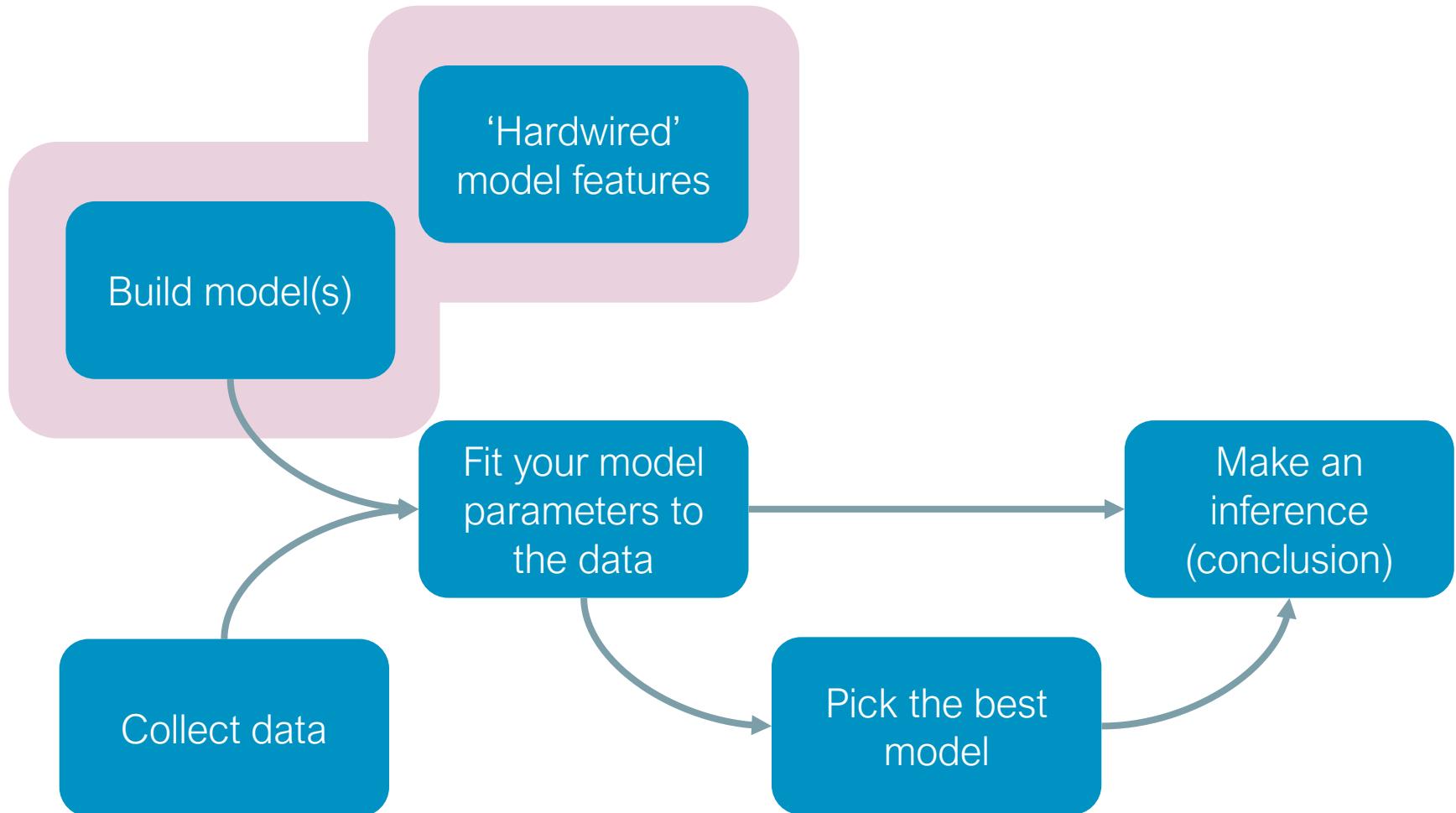
1. Downsample
2. Filter (e.g. 1-40Hz)
3. Epoch
4. Remove artefacts
5. Average
  - Per subject
  - Grand average
6. Plausible sources
  - Literature / a priori
  - Dipole fitting
  - Source reconstruction



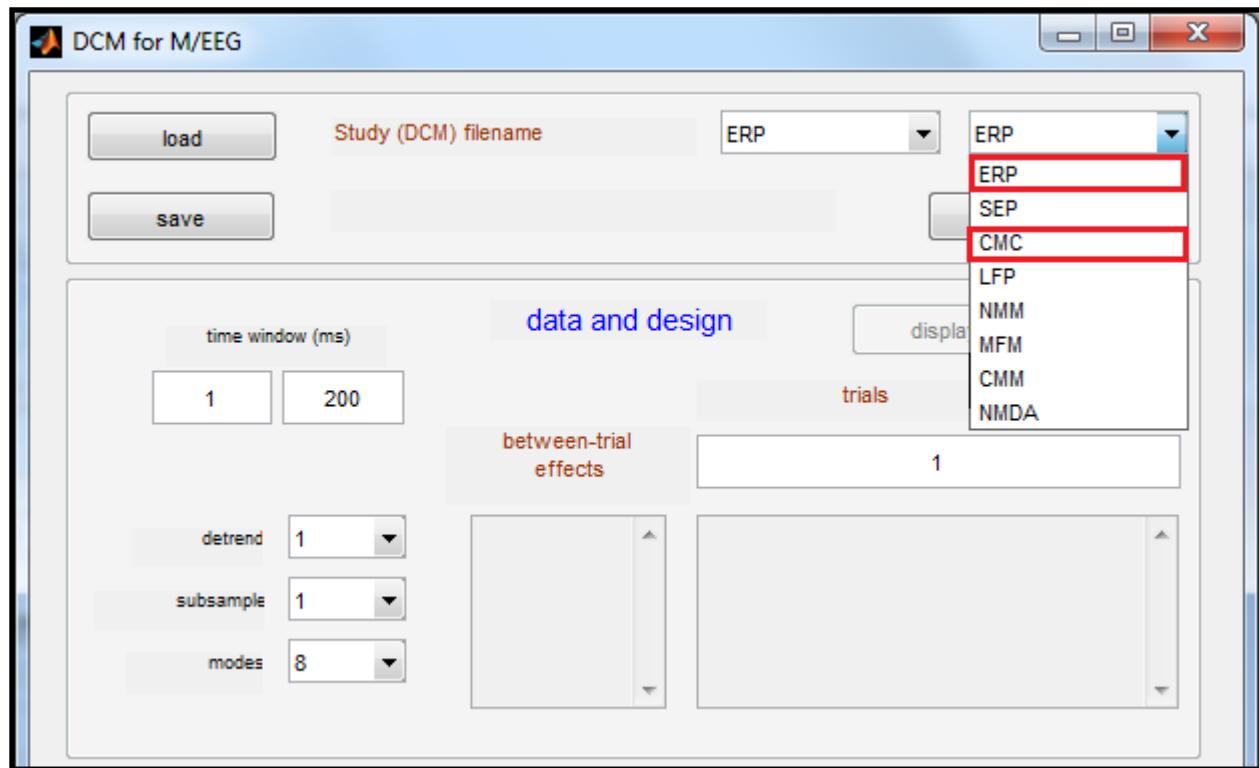
# The DCM analysis pathway



# The DCM analysis pathway



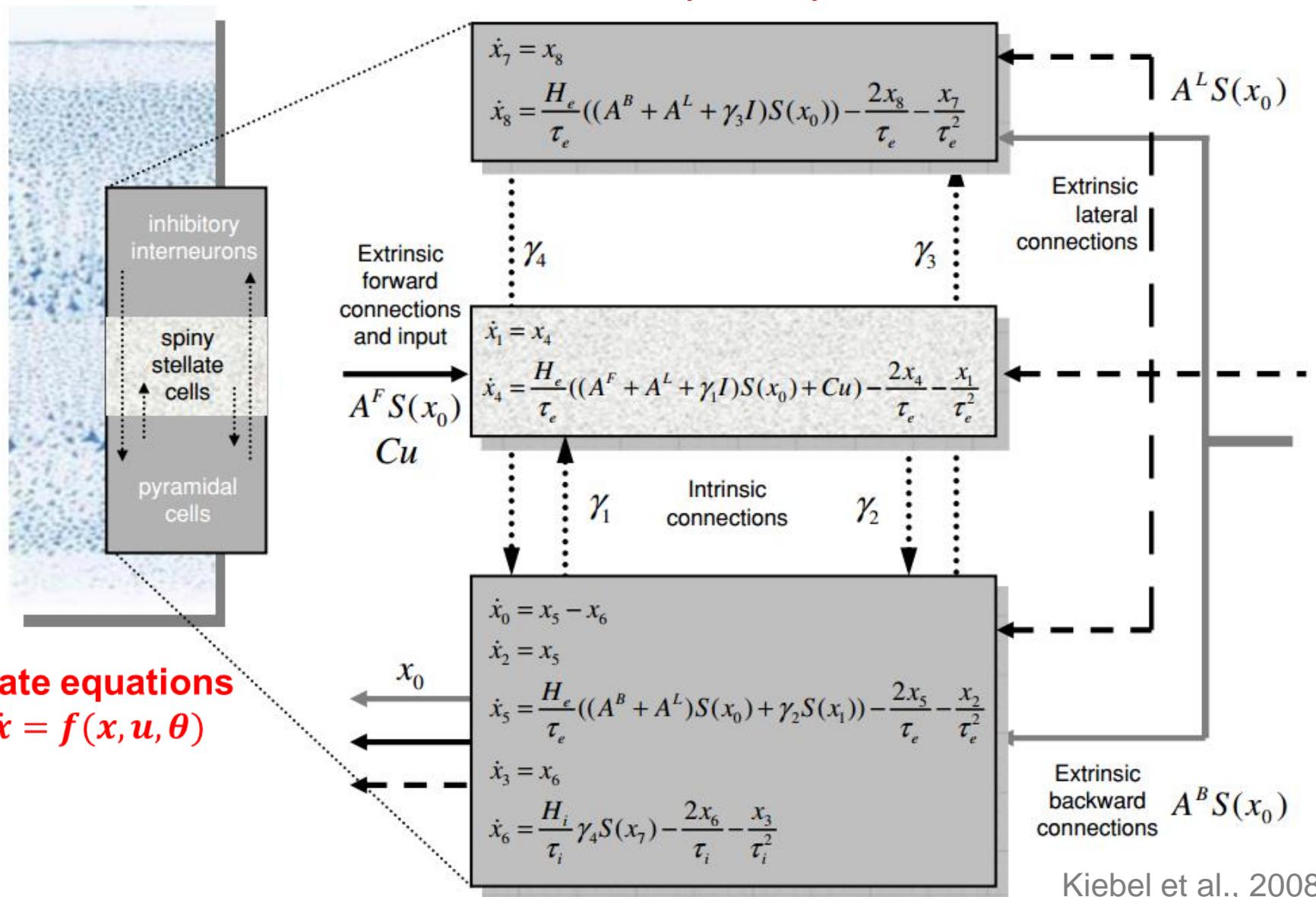
# Models

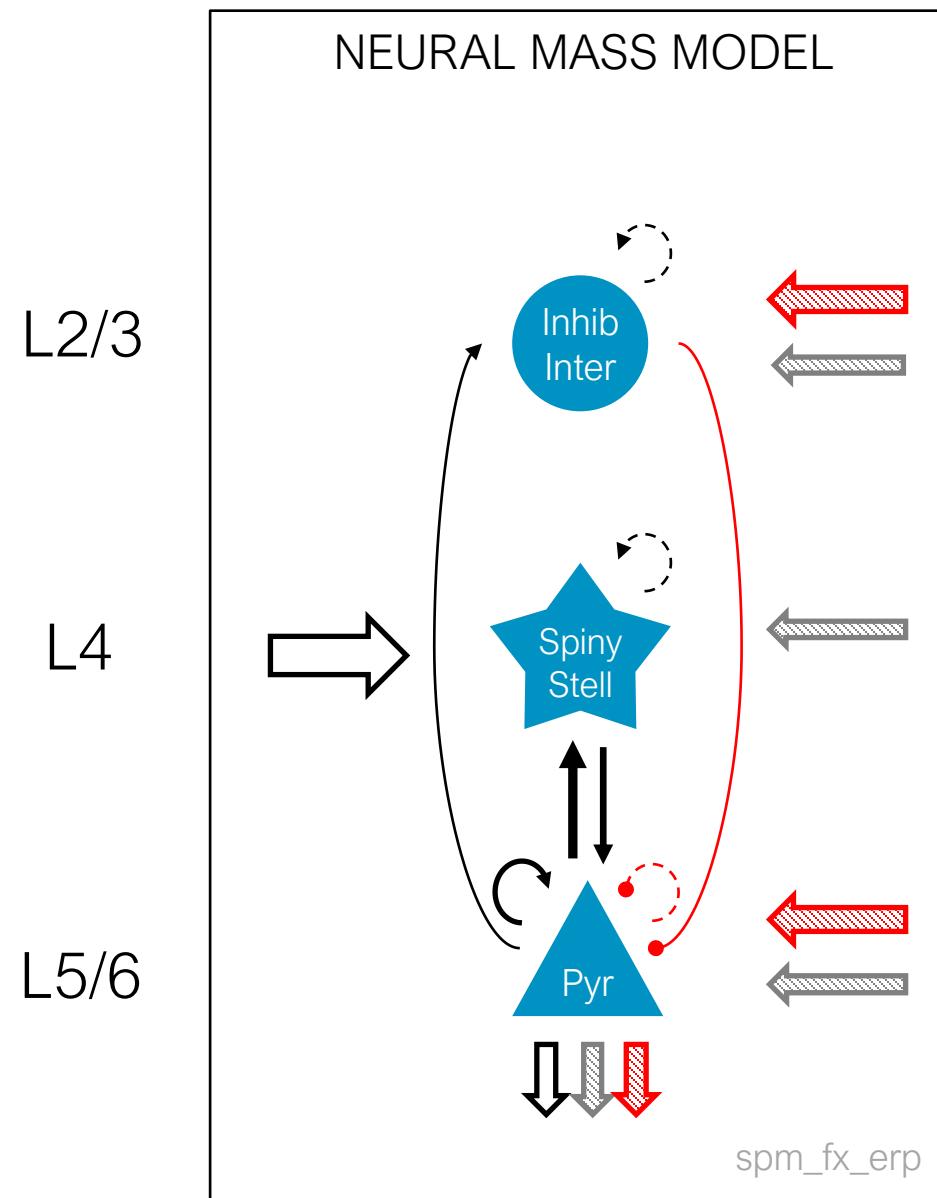


## Neural masses and fields in dynamic causal modeling

Rosalyn Moran<sup>1,2,3\*</sup>, Dimitris A. Pinotsis<sup>1†</sup> and Karl Friston<sup>1</sup>

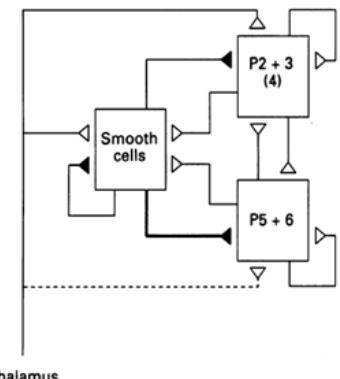
## Neuronal (source) model



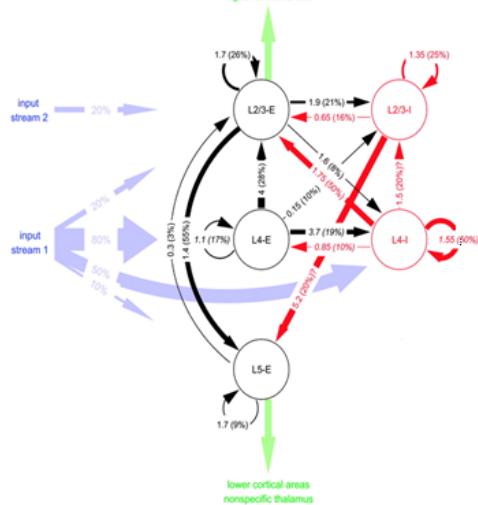


# Canonical Microcircuit Model ('CMC')

Original microcircuit

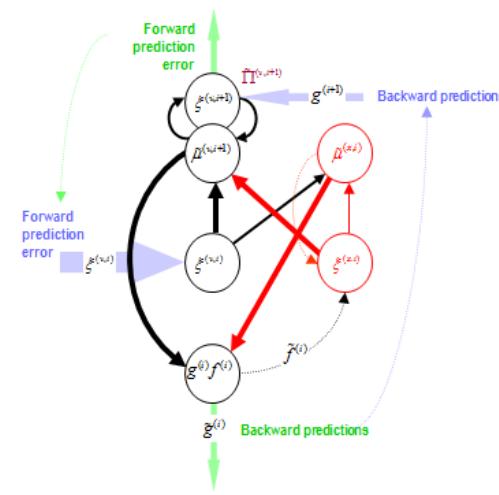


Updated microcircuit



Douglas & Martin (1991)

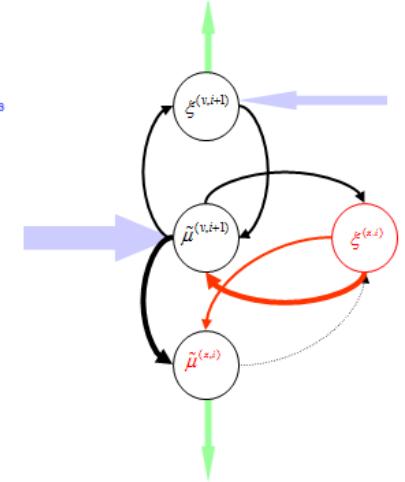
Canonical microcircuit  
(predictive coding)



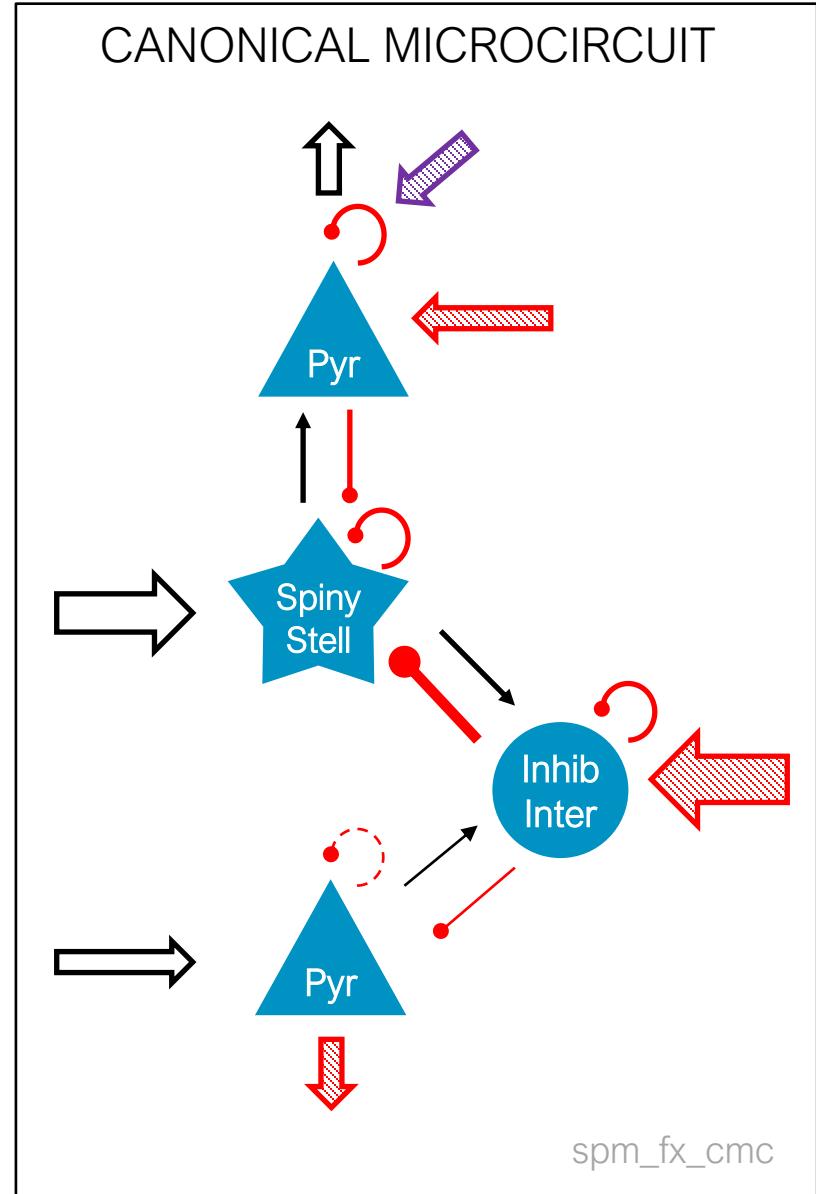
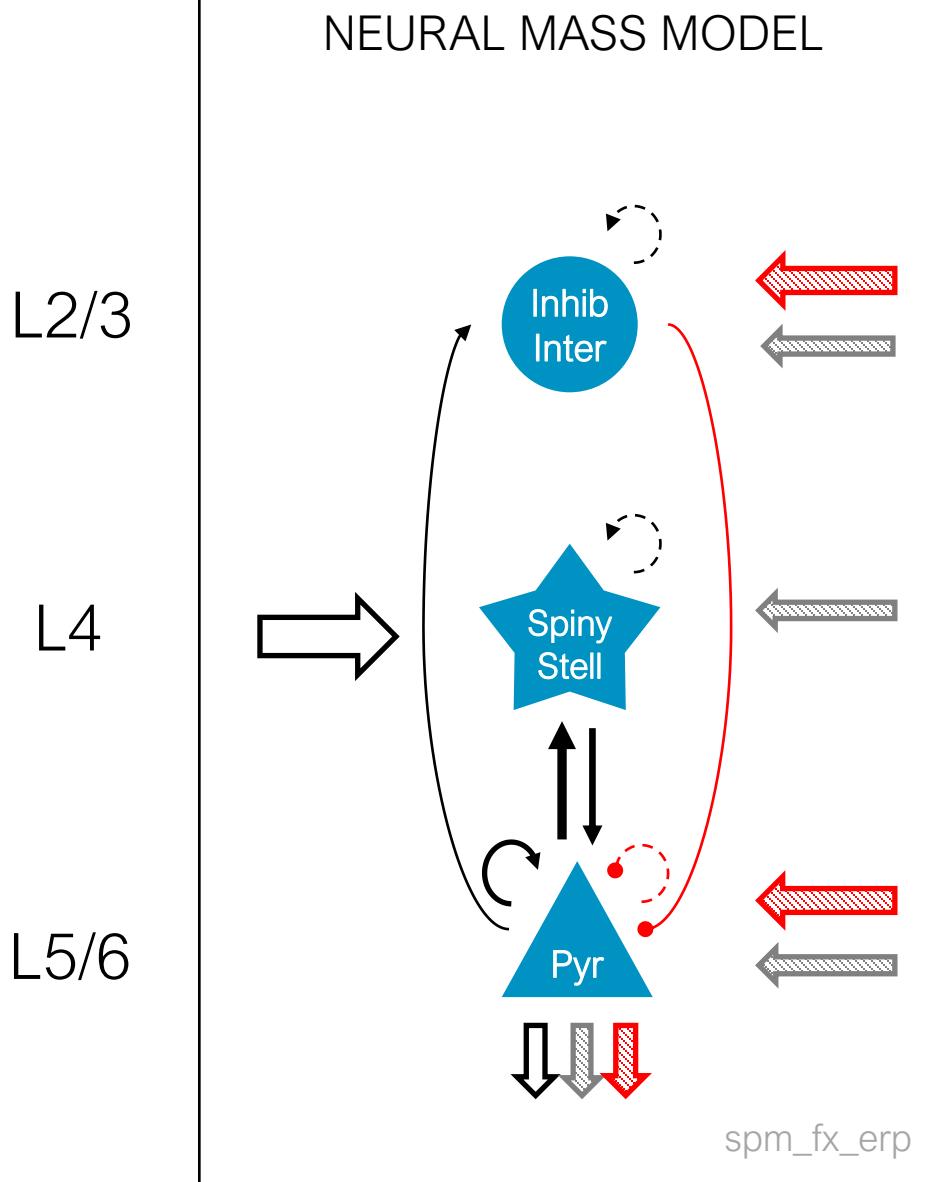
Adapted from Haeusler & Maass (2006)

Bastos et al. (2012)

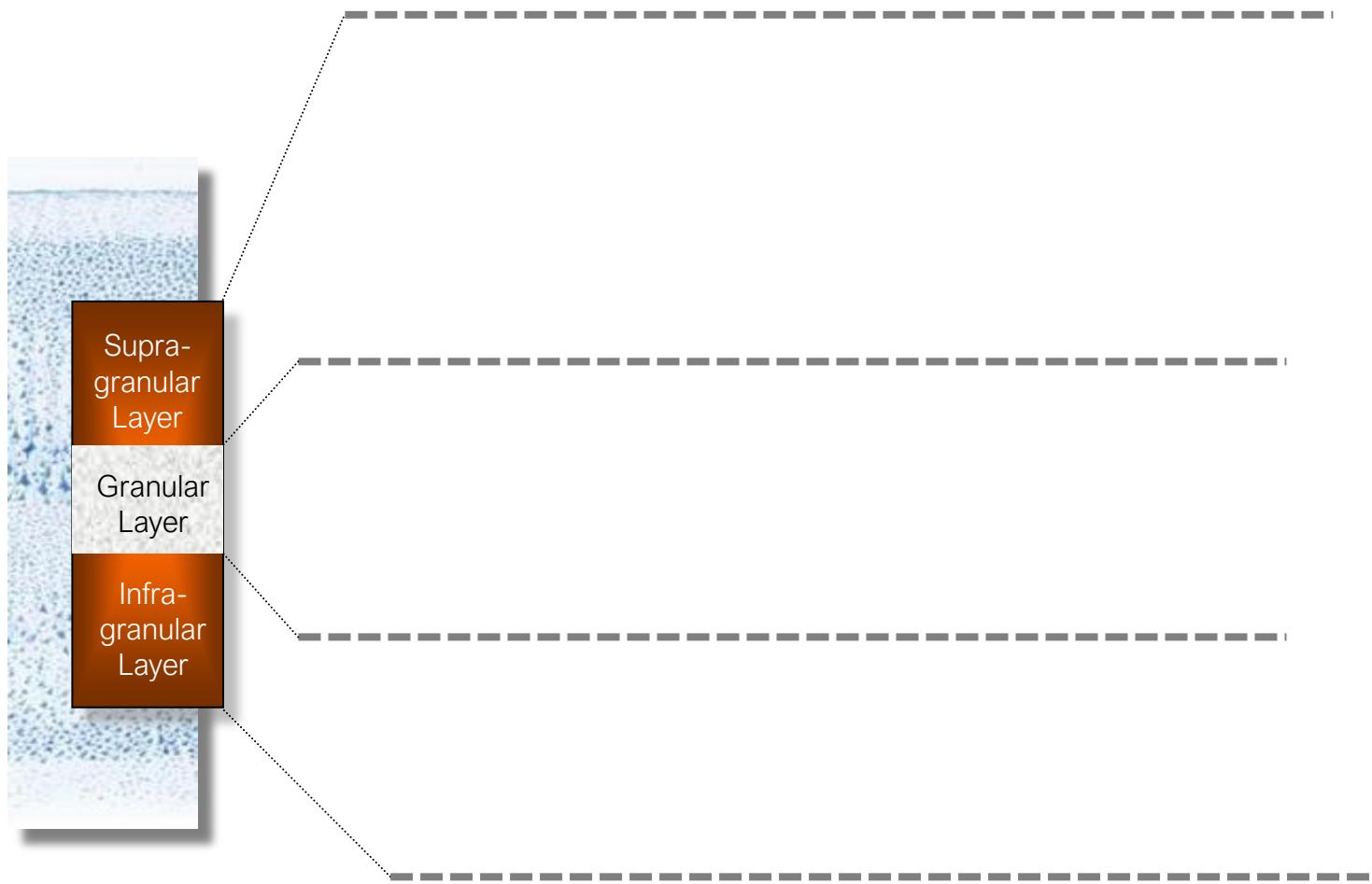
Reduced model  
(DCM)



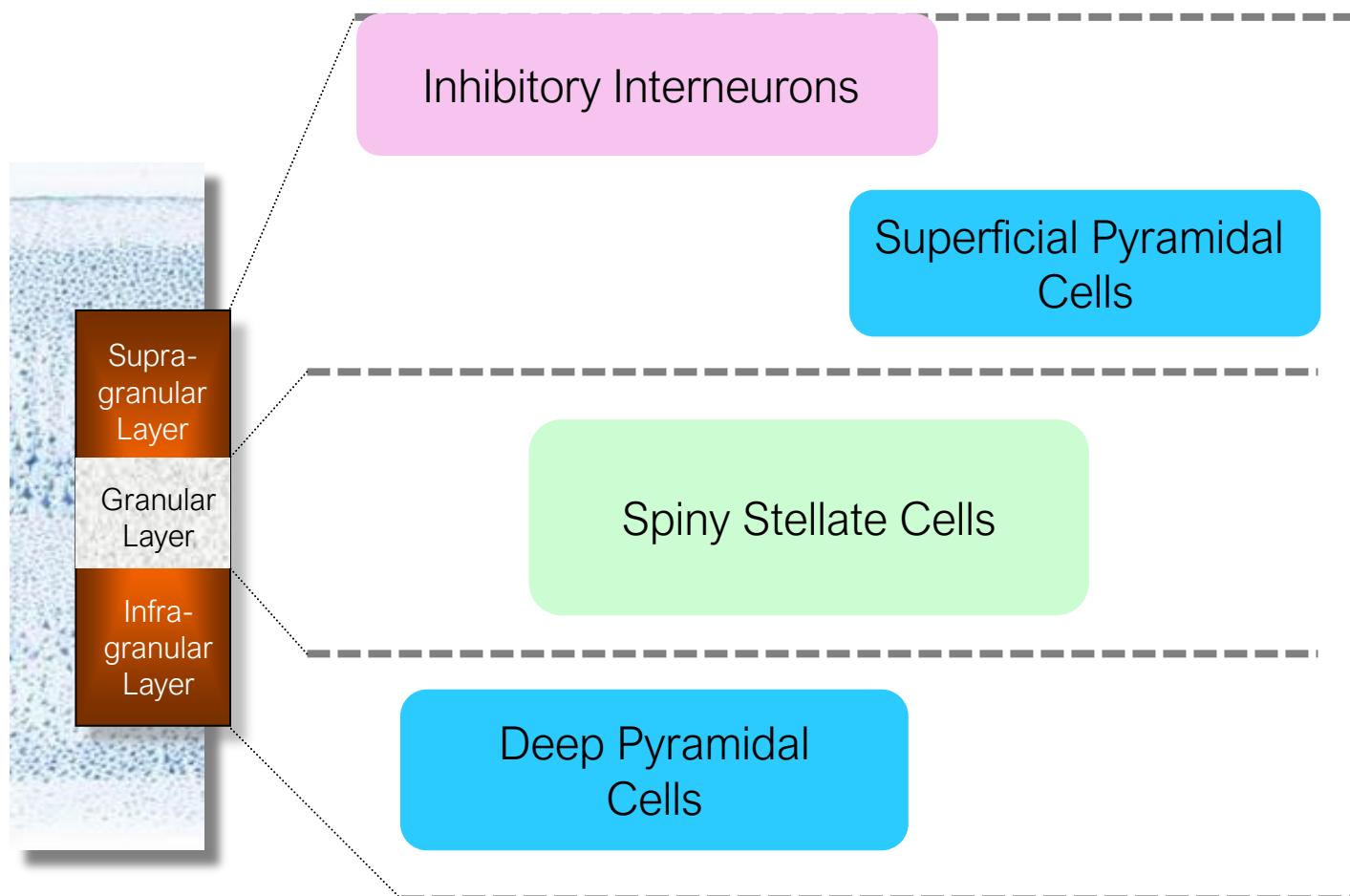
Pinotsis et al. (2012)



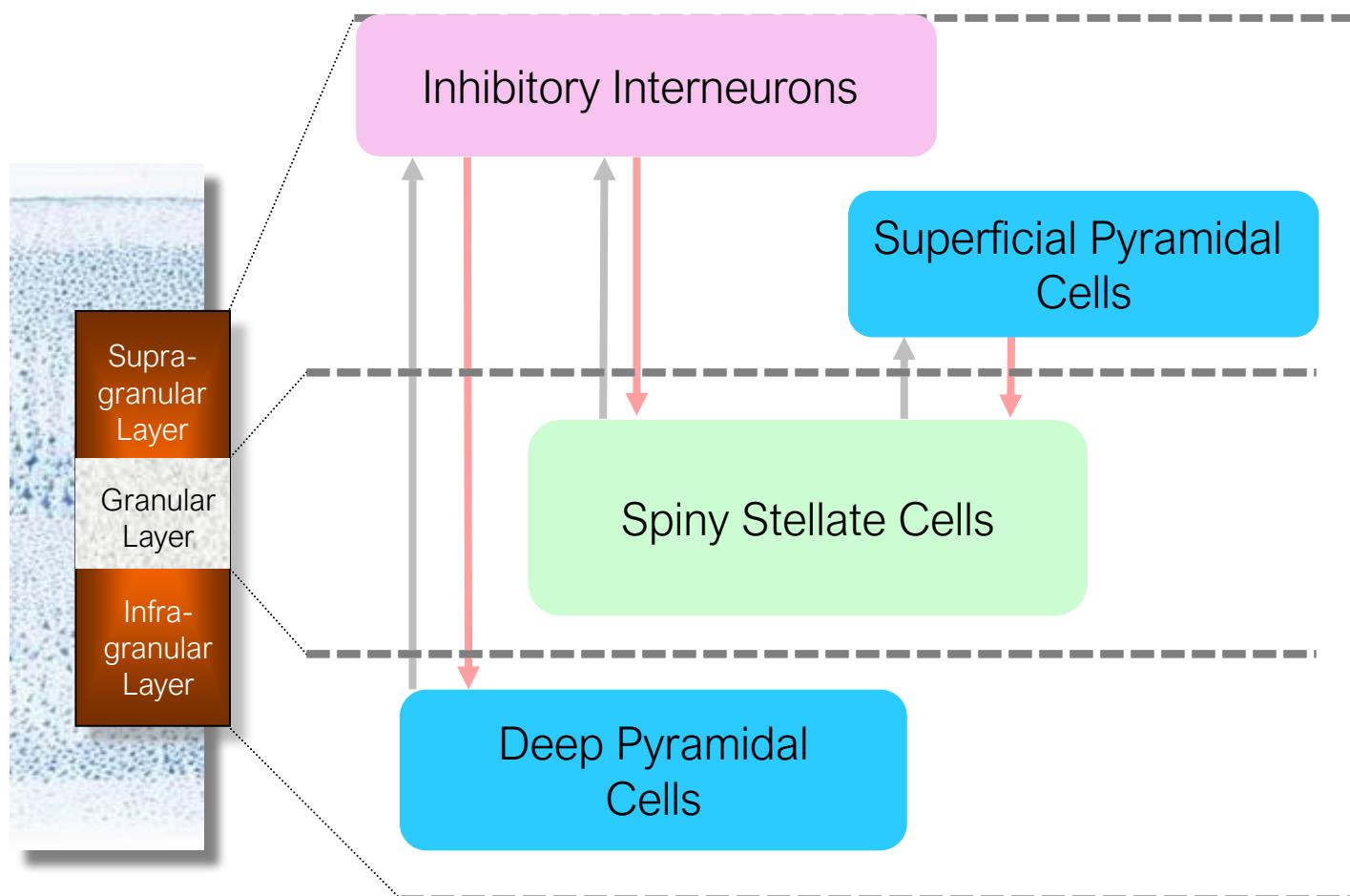
# Canonical Microcircuit Model ('CMC')



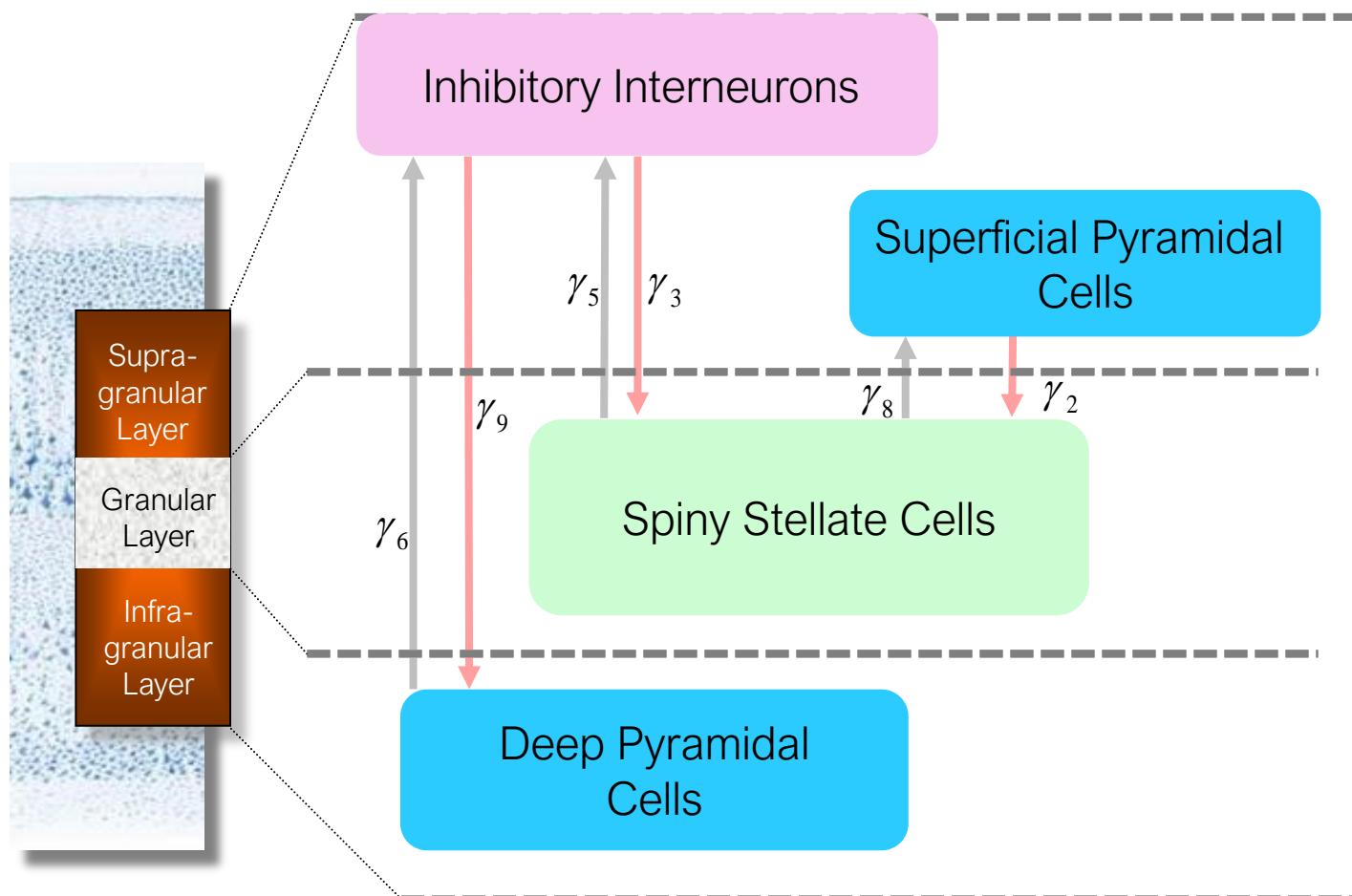
# Canonical Microcircuit Model ('CMC')



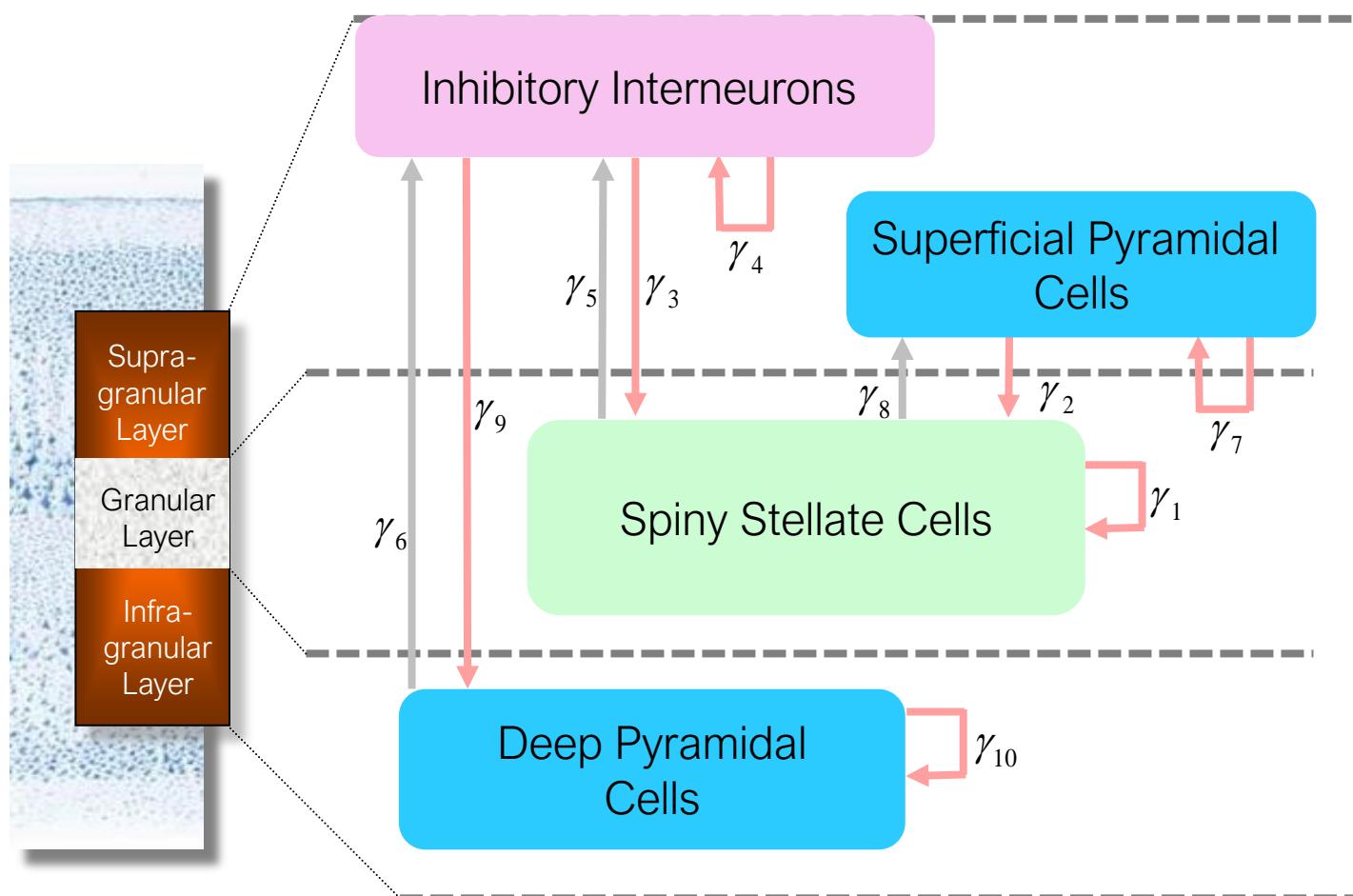
# Canonical Microcircuit Model ('CMC')



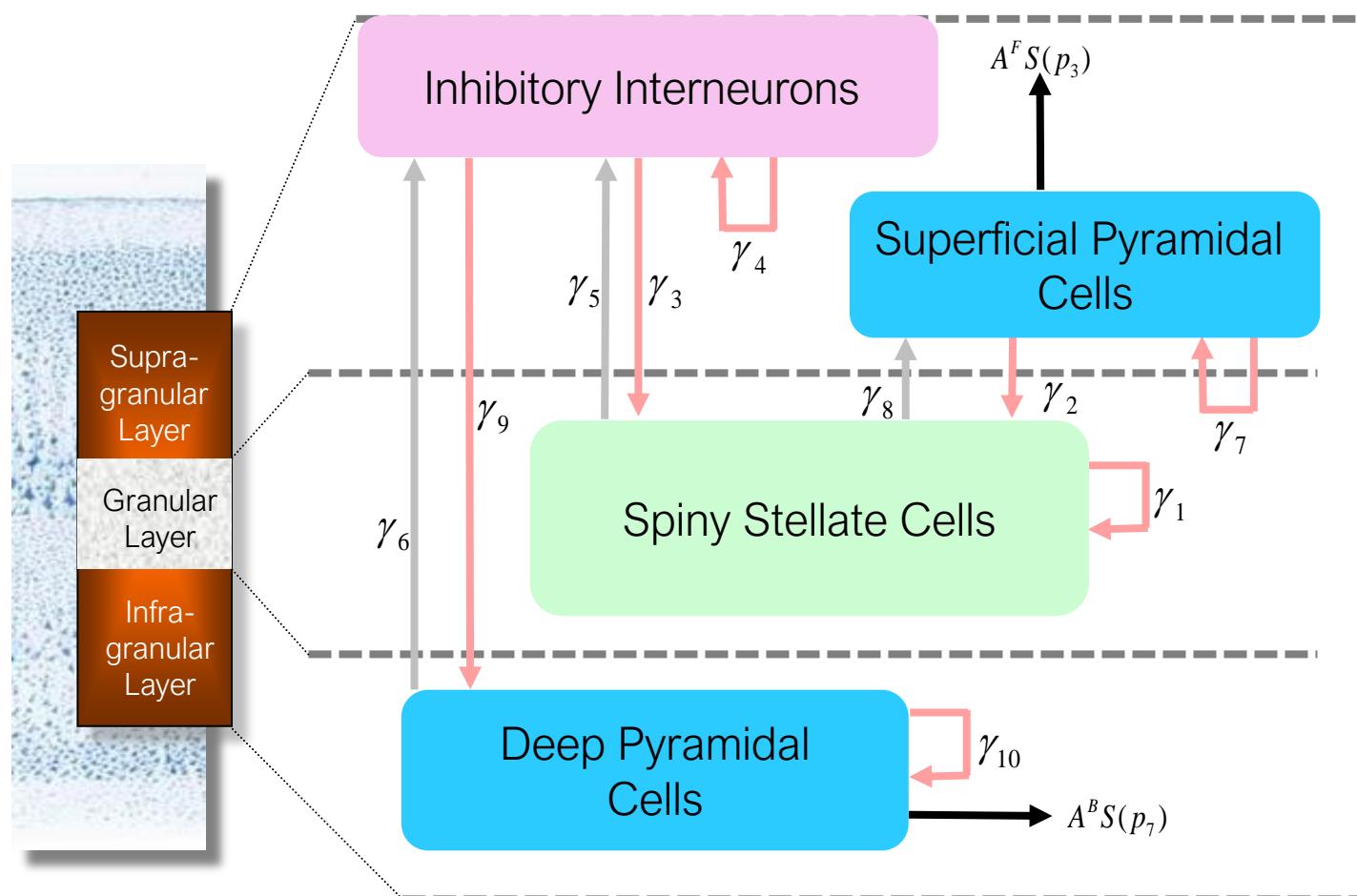
# Canonical Microcircuit Model ('CMC')



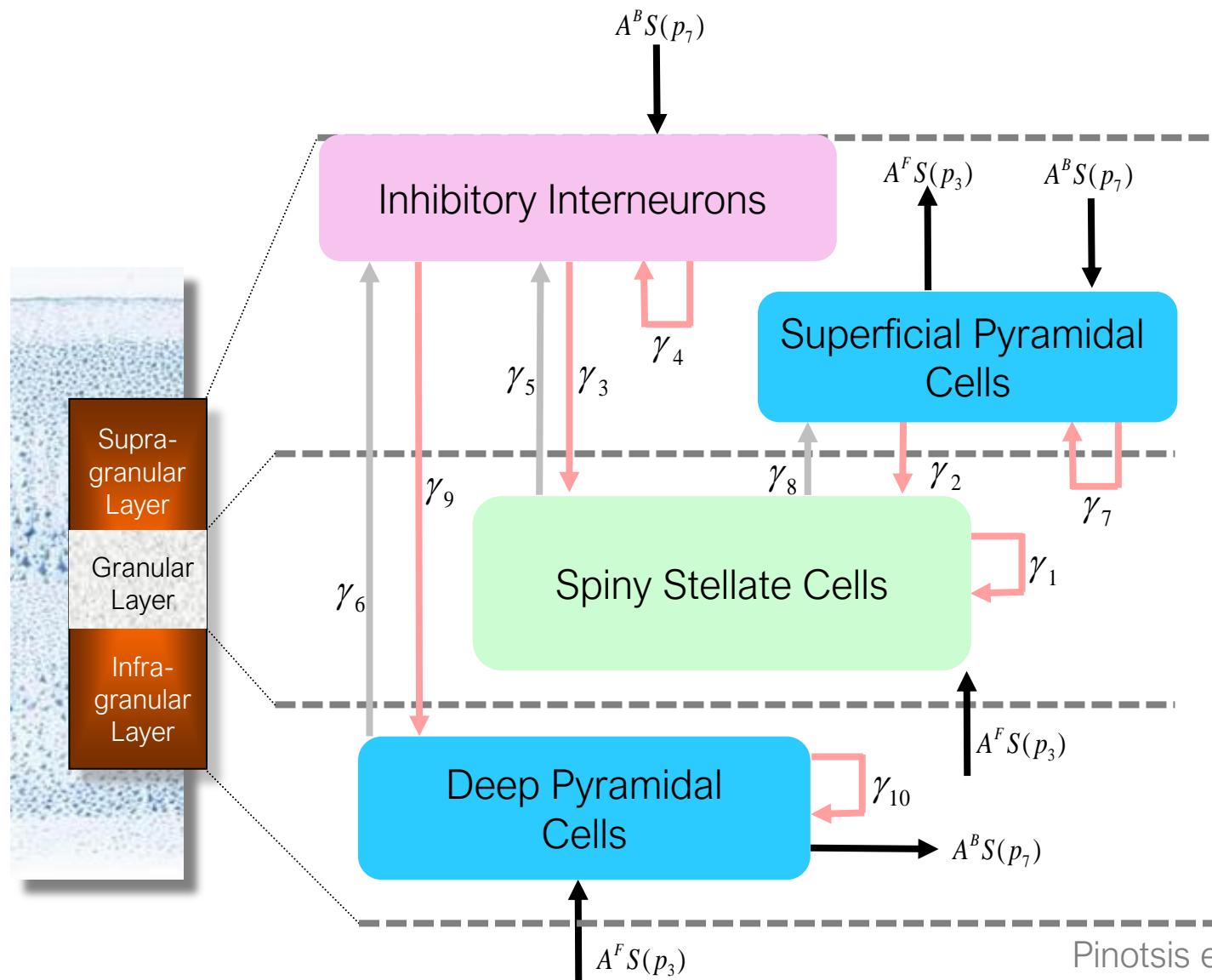
# Canonical Microcircuit Model ('CMC')



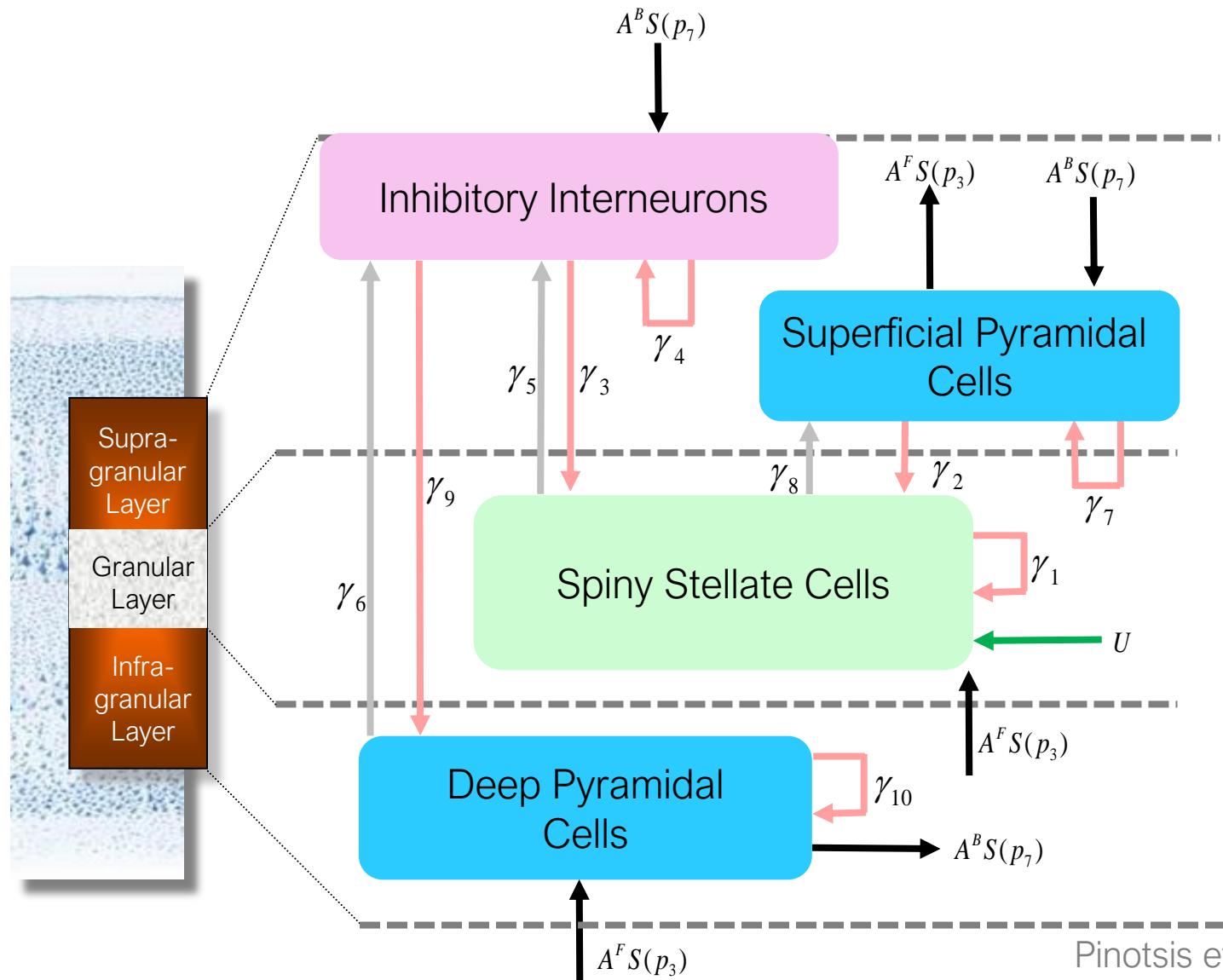
# Canonical Microcircuit Model ('CMC')



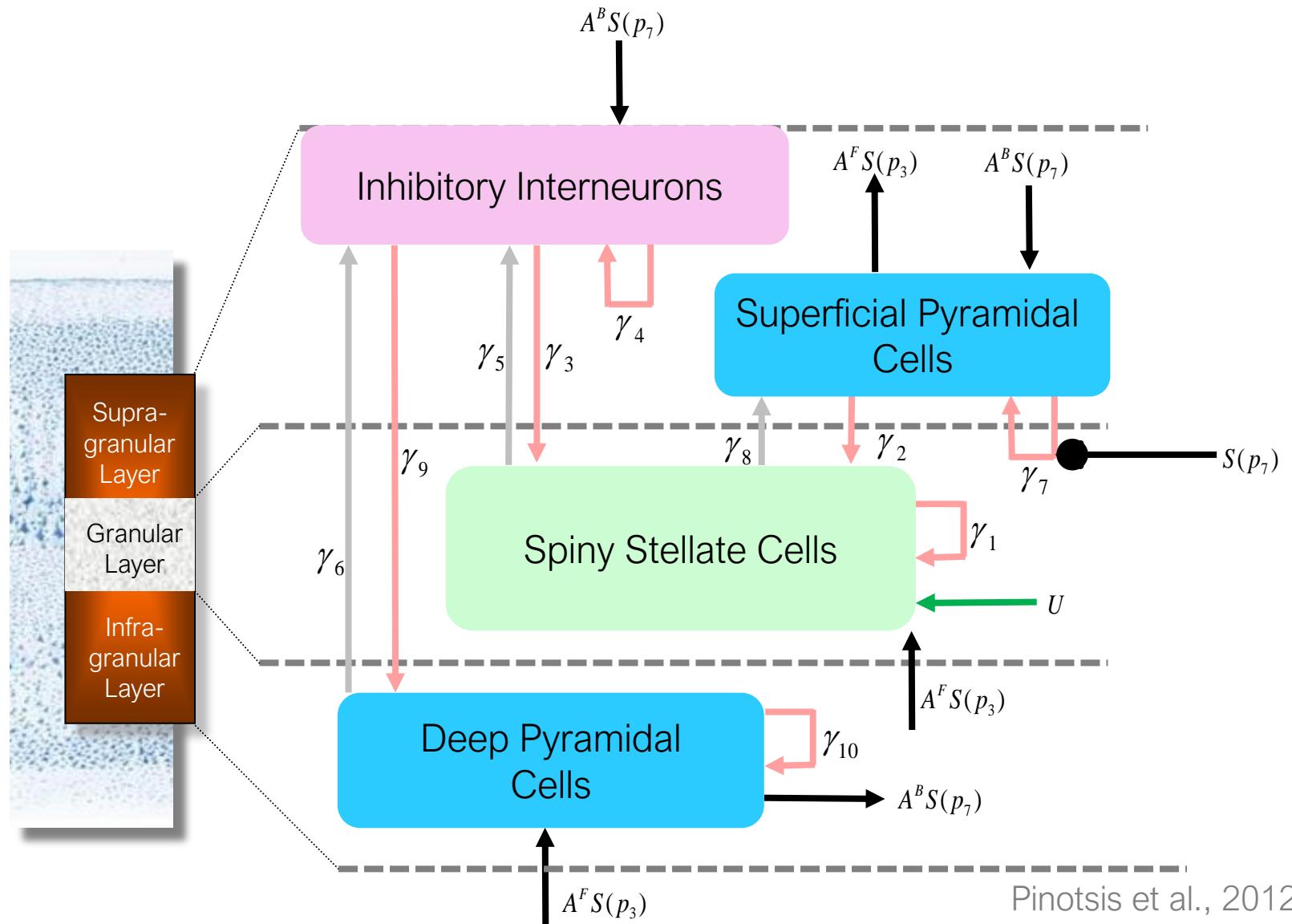
# Canonical Microcircuit Model ('CMC')



# Canonical Microcircuit Model ('CMC')



# Canonical Microcircuit Model ('CMC')



# Canonical Microcircuit Model ('CMC')

$$\dot{p}_7 = p_8$$

Voltage change rate: f(current)

Current change rate: f(voltage,current)

$$\dot{p}_8 = \frac{H_4}{\tau_4} (A^F S(p_2) - \gamma_{10} S(p_7) - \gamma_9 S(p_5)) - \frac{2p_8}{\tau_4} - \frac{p_7}{\tau_4^2}$$

# Canonical Microcircuit Model ('CMC')

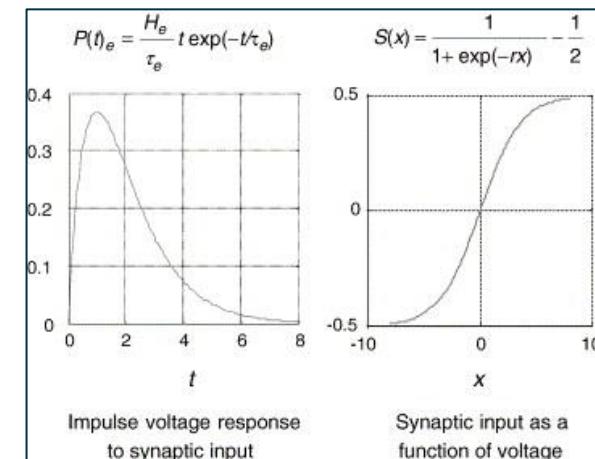
$$\dot{p}_7 = p_8$$

Voltage change rate: f(current)  
 Current change rate: f(voltage,current)

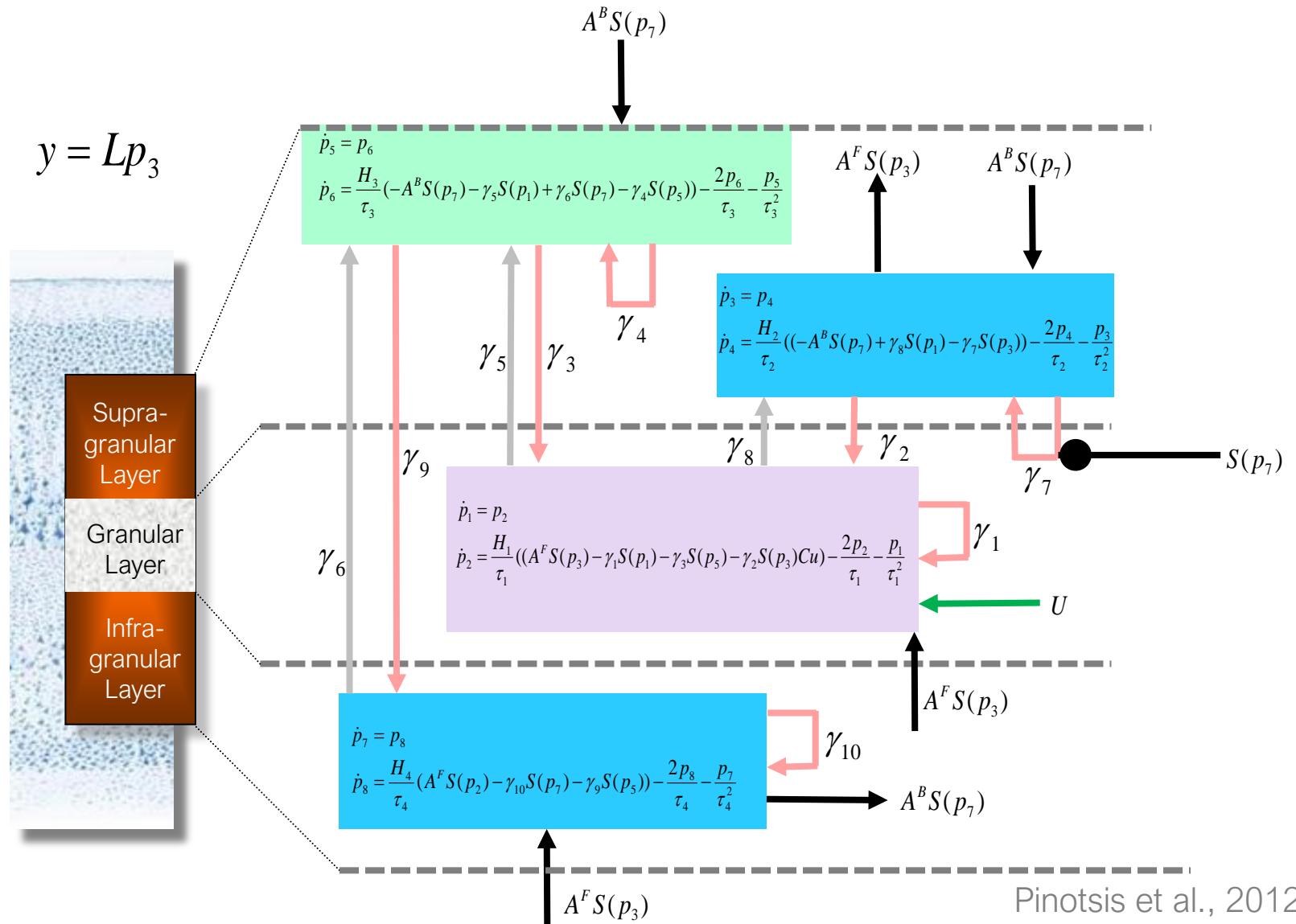
$$\dot{p}_8 = \frac{H_4}{\tau_4} (A^F S(p_2) - \gamma_{10} S(p_7) - \gamma_9 S(p_5)) - \frac{2p_8}{\tau_4} - \frac{p_7}{\tau_4^2}$$

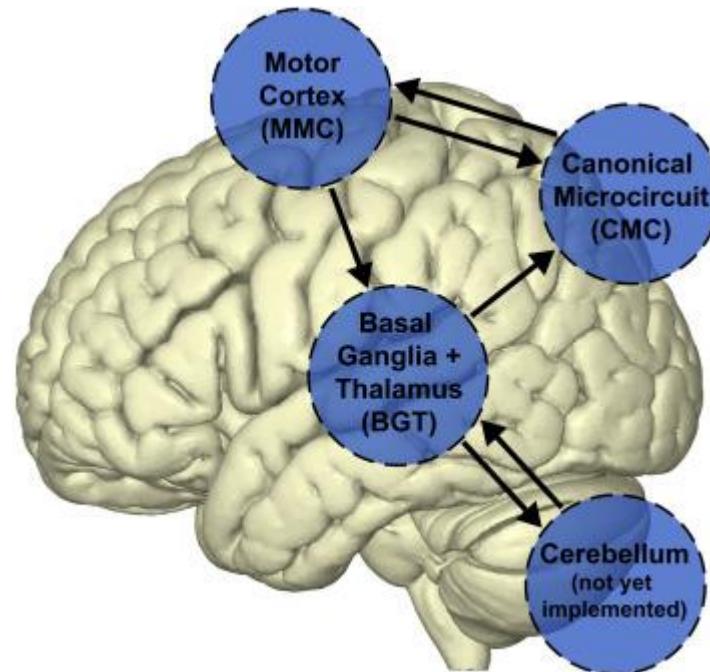
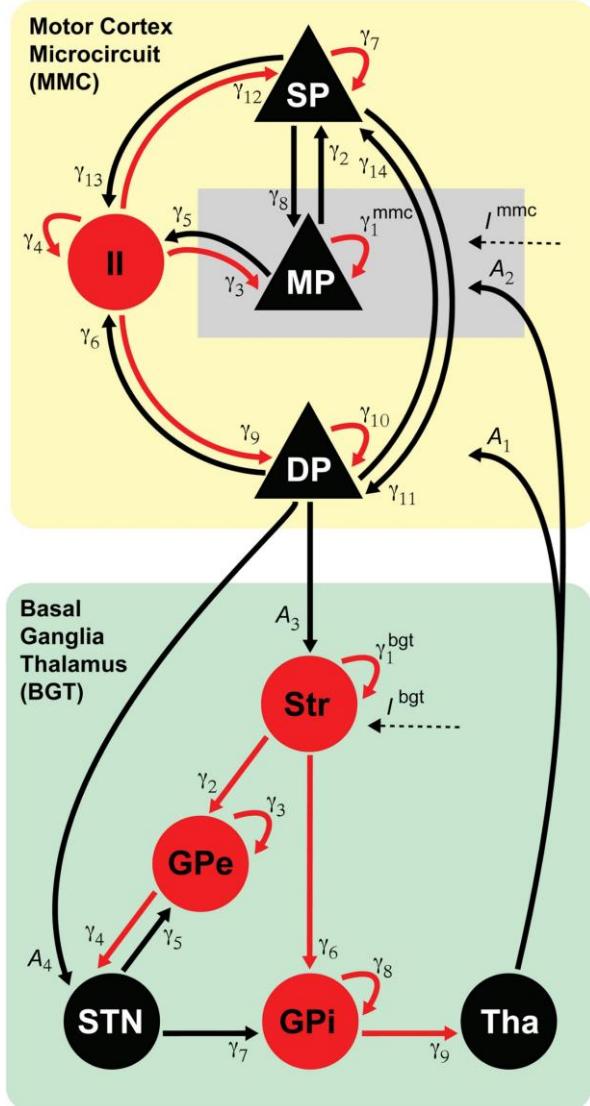
$H, \tau$  Kernels: pre-synaptic inputs  $\rightarrow$  post-synaptic membrane potentials  
 [  $H$ : max PSP;  $\tau$ : rate constant ]

$S$  Sigmoid operator: PSP  $\rightarrow$  firing rate

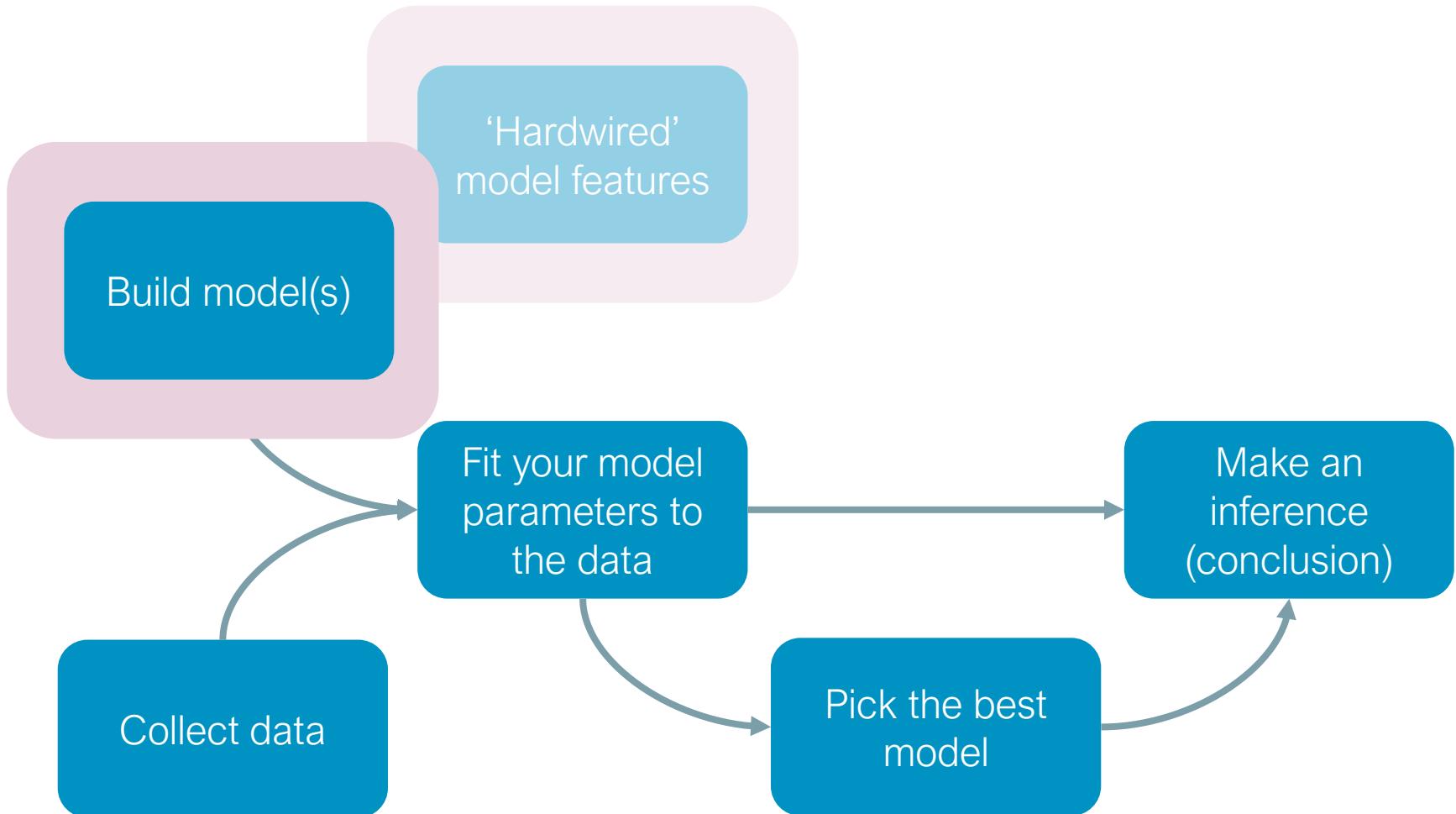


# Canonical Microcircuit Model ('CMC')





# The DCM analysis pathway



**electromagnetic model**

source names and locations: prior mean (mm)

onsets (ms)	right A1 left A1 right STG left STG right IPS	46 -14 8 -42 -22 7 56 -40 18 -60 -48 20 34 -66 46
20		
duration (sd)		
16		

**neuronal model**

forward back Modulatory input

reset invert DCM

B att-noatt B dev-std

dipolar symmetry  optimise source locations  lock trial-specific effects  trial-specific inputs

Wavelet transform frequency window Hz 4 48 wavelet number 7 image API

ERPs (mode) initialise priors BMS post hoc reduce

5

3

4

2

1

**electromagnetic model**

source names and locations: prior mean (mm)

onsets (ms)	right A1 left A1 right STG left STG right IPS	46 -14 8 -42 -22 7 56 -40 18 -60 -48 20 34 -66 46
duration (sd)	load	
20		
16		

**neuronal model**

forward back Modulatory input

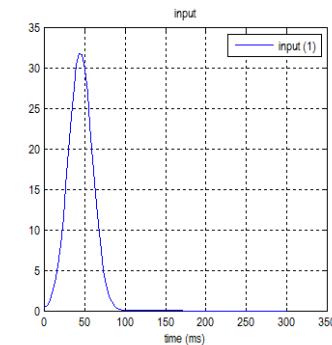
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dipolar symmetry optimise source locations lock trial-specific effects trial-specific inputs

Wavelet transform frequency window Hz 4 48 wavelet number 7 image API

ERPs (mode) initialise priors BMS post hoc reduce



5

3

4

1

Input

2

3

**ECD**

### electromagnetic model

source names and locations: prior mean (mm)

onsets (ms)	right A1 left A1 right STG left STG right IPS	46 -14 8 -42 -22 7 56 -40 18 -60 -48 20 34 -66 46
20		
duration (sd)		
16		

**load**

### neuronal model

reset

forward

back

Modulatory

input

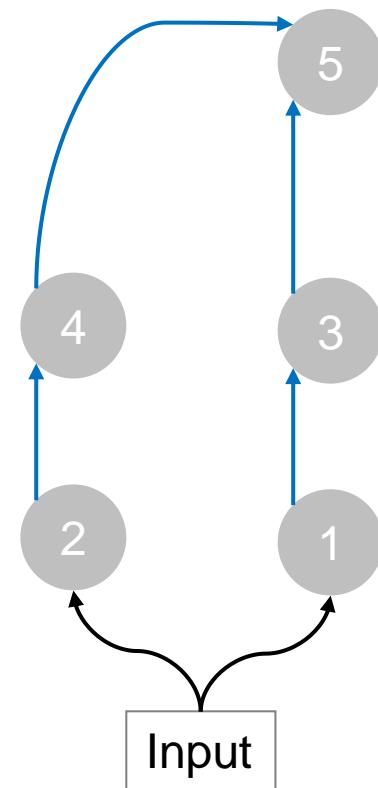
invert DCM

B att-noatt      B dev-std

dipolar symmetry     optimise source locations     lock trial-specific effects     trial-specific inputs

Wavelet transform      frequency window Hz      4      48      wavelet number      7      image API

ERPs (mode)      initialise      priors      BMS      post hoc      reduce



**electromagnetic model**

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20		
duration (sd)		
16		

**neuronal model**

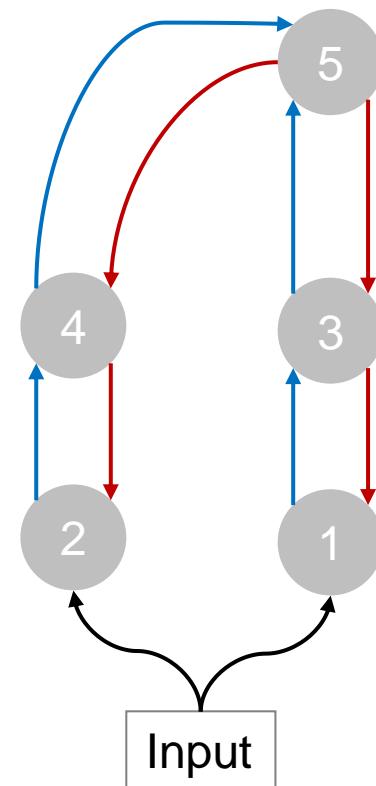
forward      back      Modulatory      input

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dipolar symmetry   optimise source locations   lock trial-specific effects   trial-specific inputs

Wavelet transform   frequency window Hz   4   48   wavelet number   7   image API

ERPs (mode)   initialise   priors   BMS   post hoc   reduce



**electromagnetic model**

source names and locations: prior mean (mm)

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20		
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16		

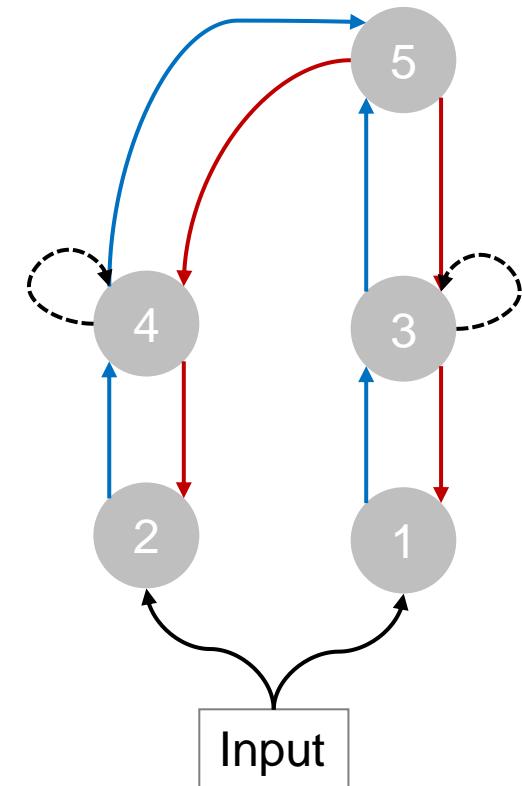
**neuronal model**

forward back Modulatory input

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Wavelet transform frequency window Hz 4 48 wavelet number 7 image API

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**ECD**

### electromagnetic model

source names and locations: prior mean (mm)

onsets (ms)	right A1 left A1 right STG left STG right IPS	46 -14 8 -42 -22 7 56 -40 18 -60 -48 20 34 -66 46
20		
duration (sd)		
16		

**neuronal model**

forward back Modulatory input invert DCM

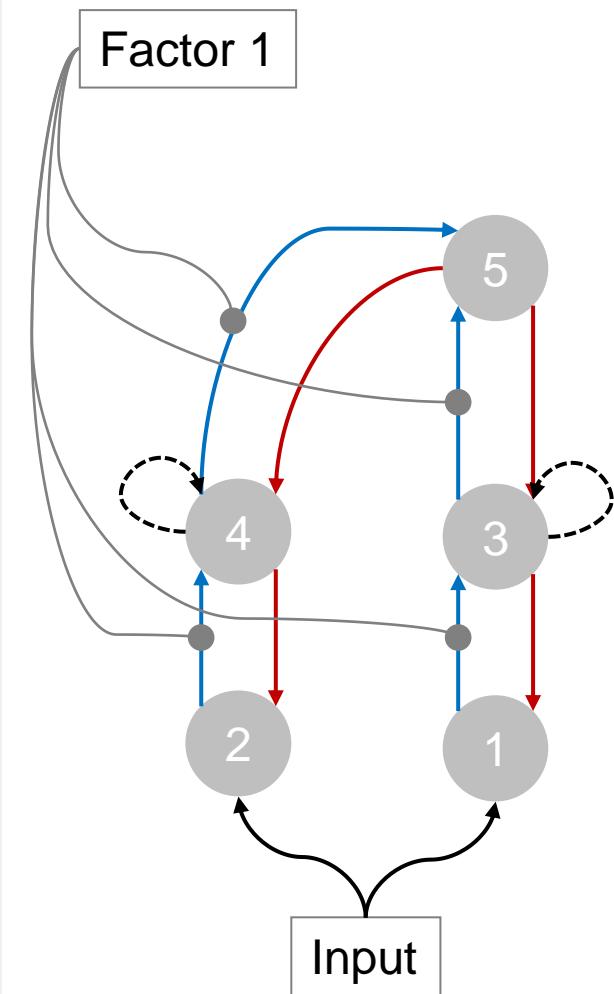
forward	back	Modulatory	input
5	5	5	5
4	4	4	4
3	3	3	3
2	2	2	2
1	1	1	1

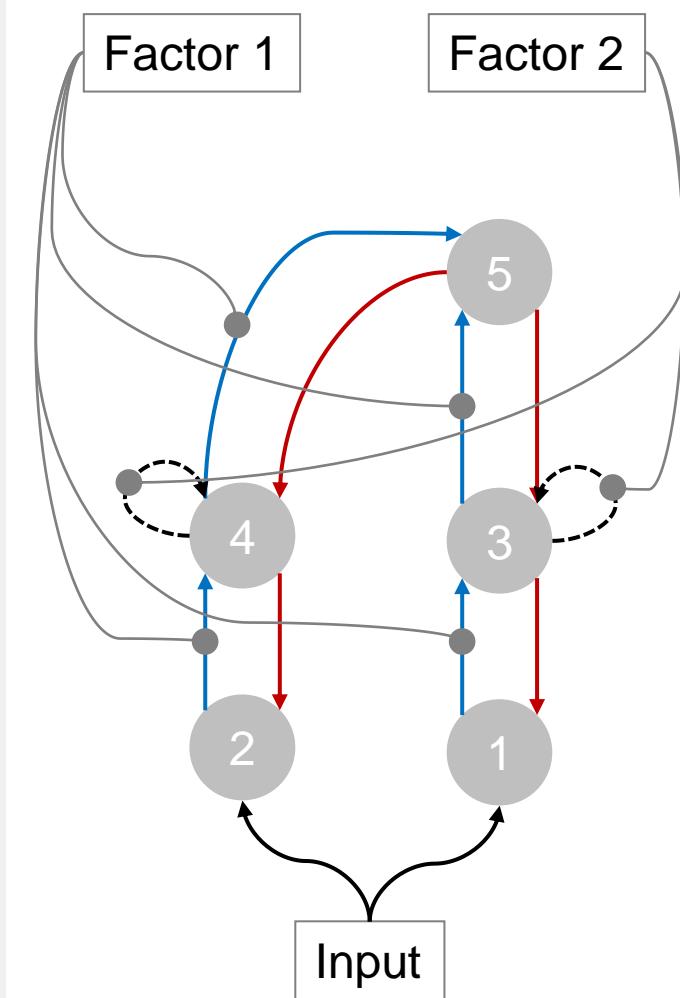
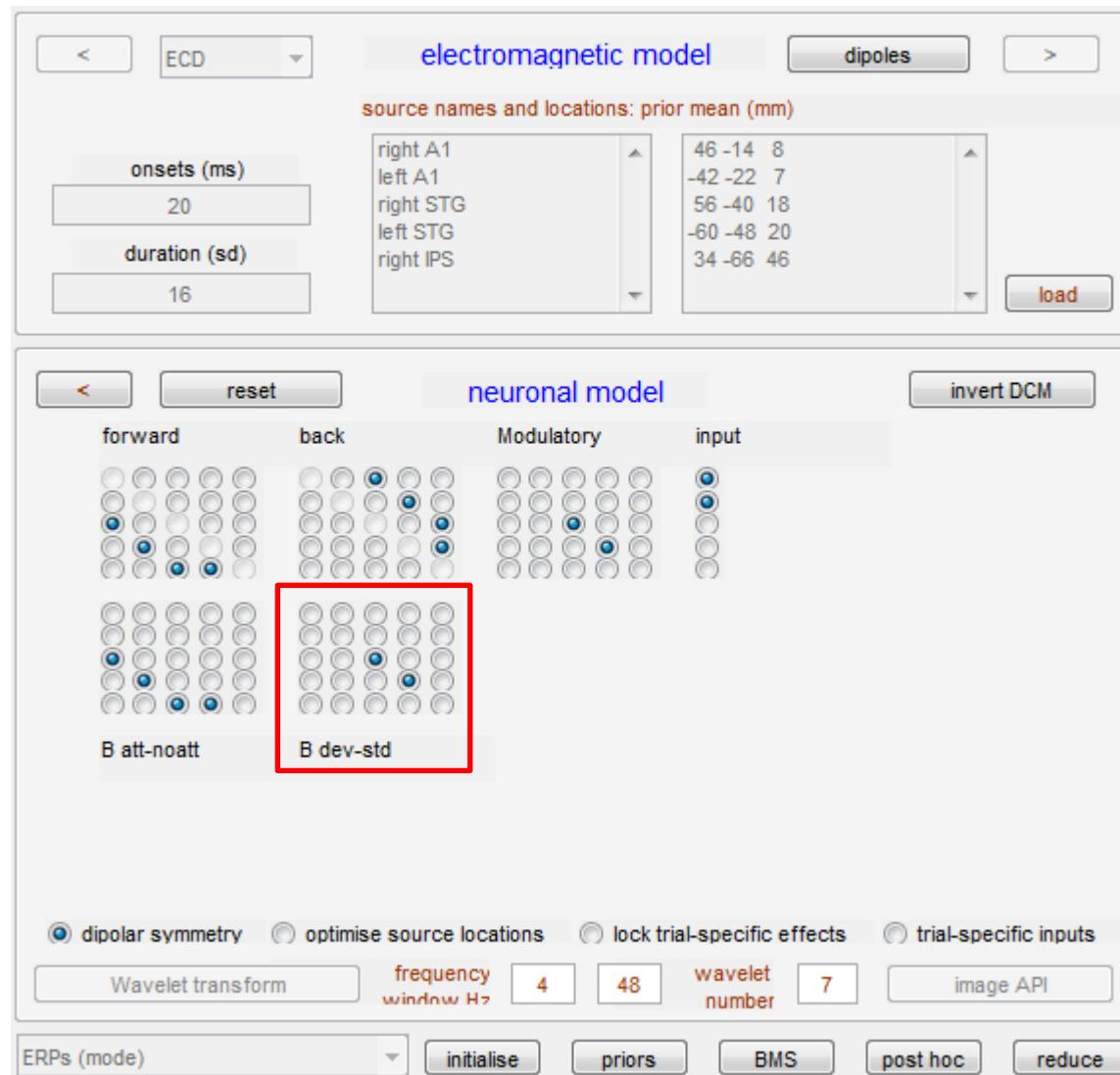
B att-noatt      B dev-std

dipolar symmetry     optimise source locations     lock trial-specific effects     trial-specific inputs

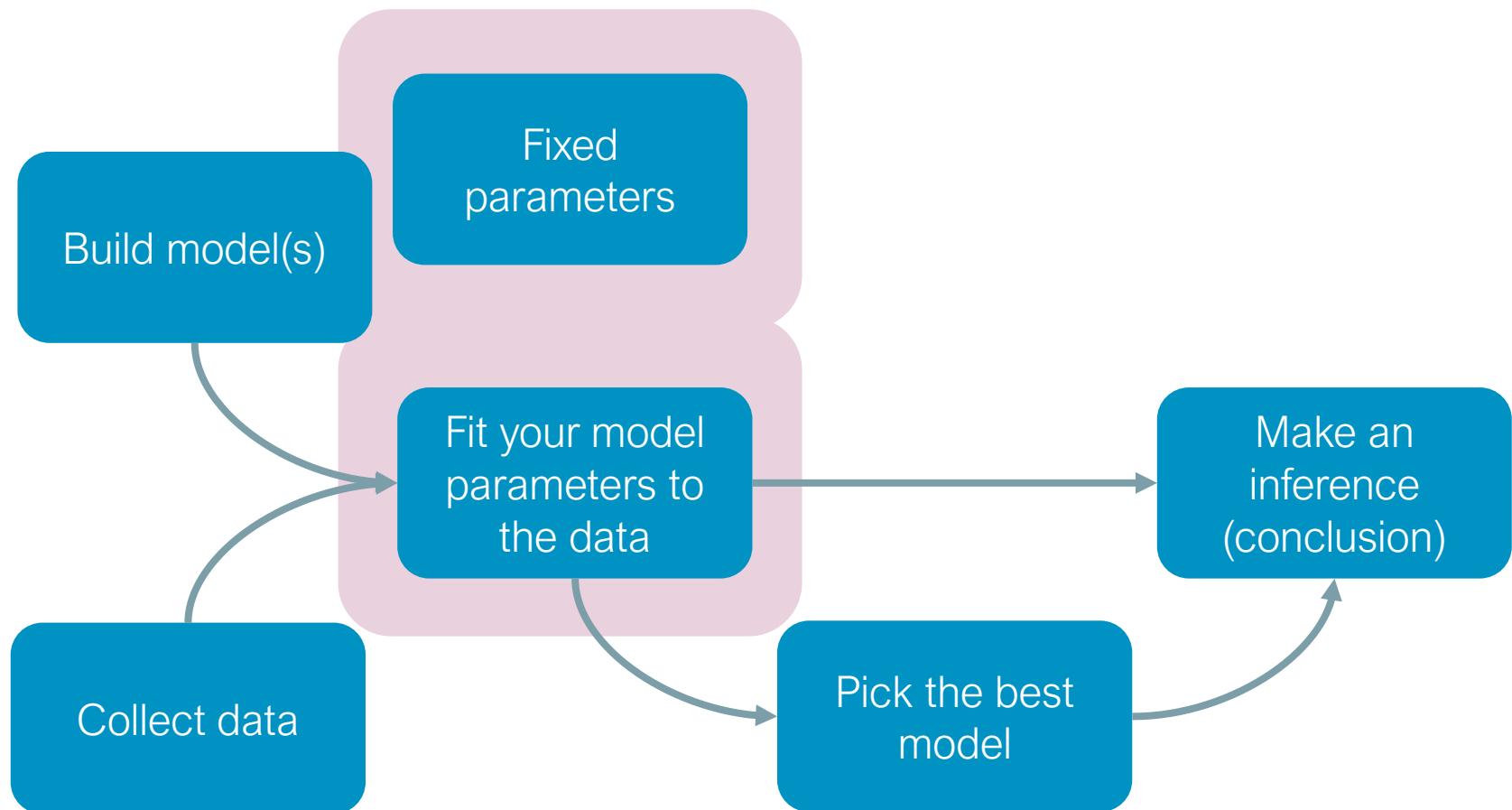
Wavelet transform      frequency window Hz      4      48      wavelet number      7      image API

ERPs (mode)      initialise      priors      BMS      post hoc      reduce

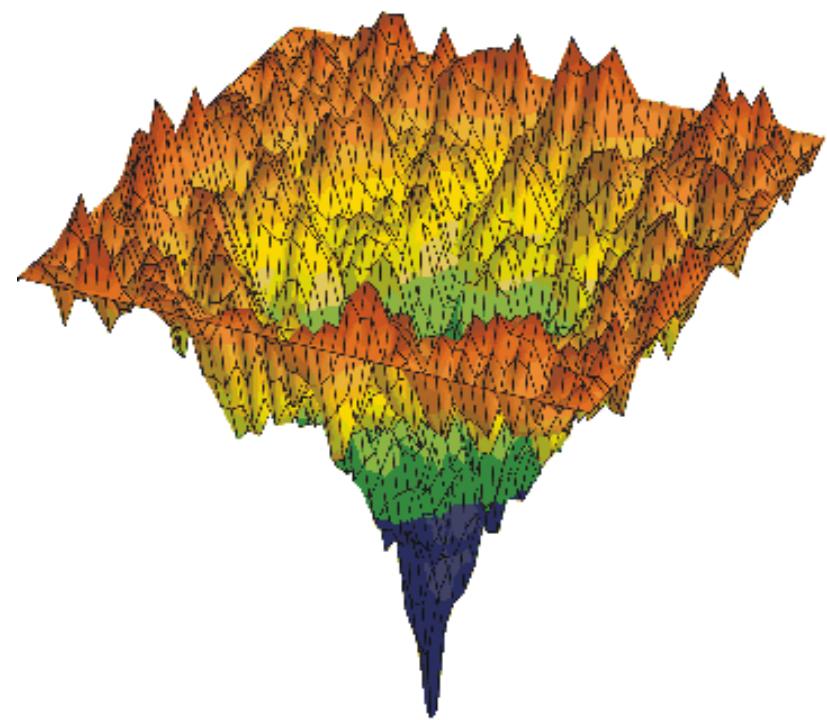
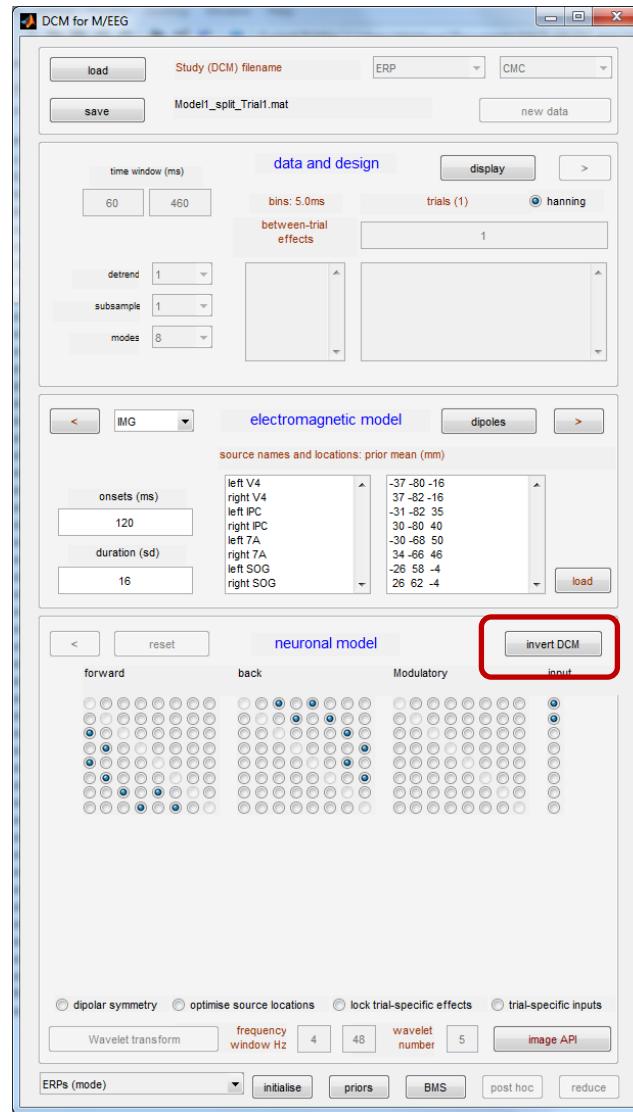




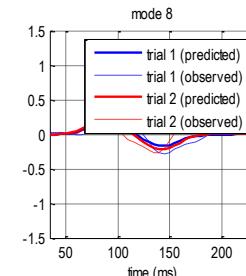
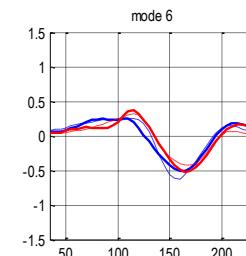
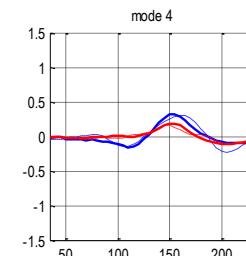
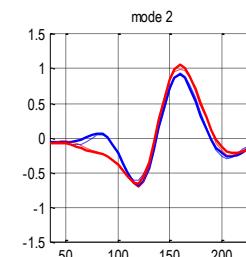
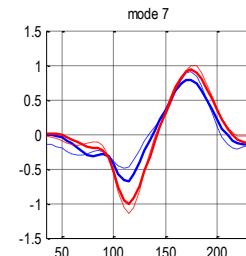
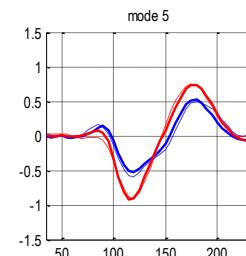
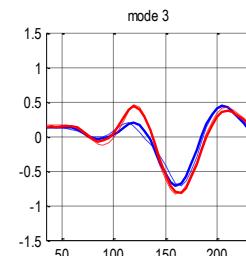
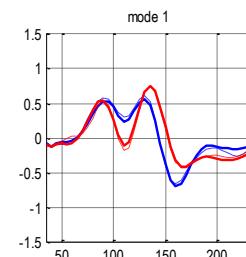
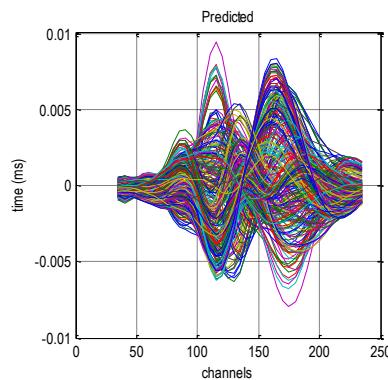
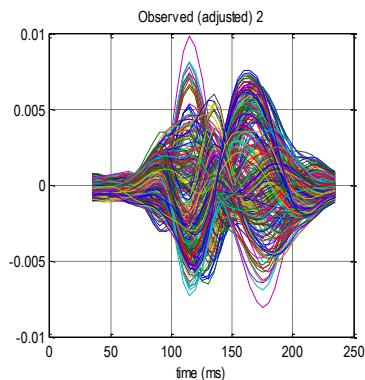
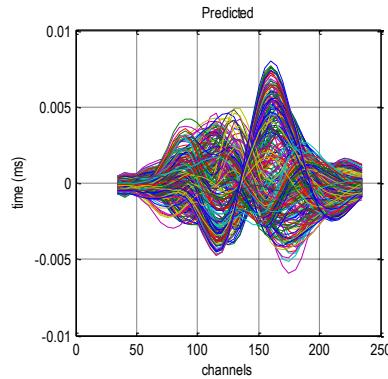
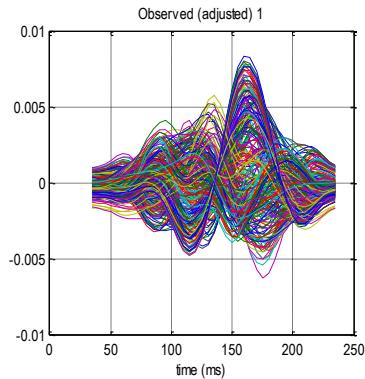
# The DCM analysis pathway



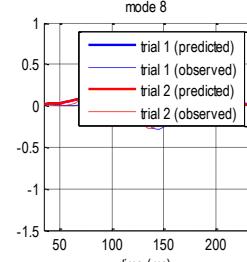
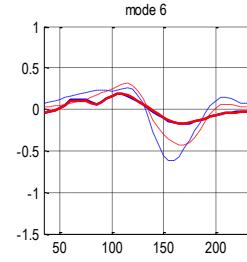
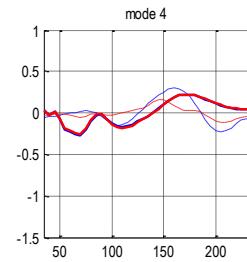
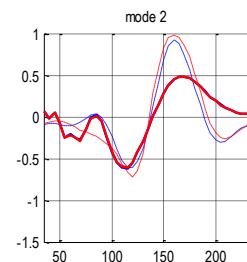
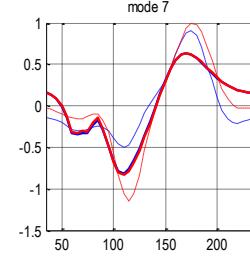
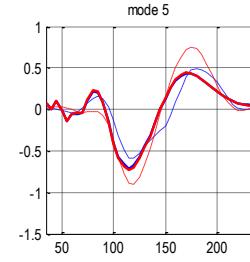
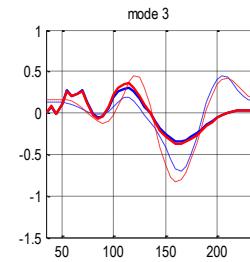
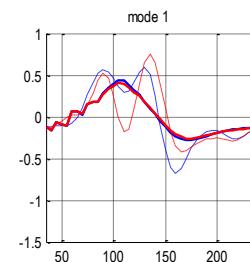
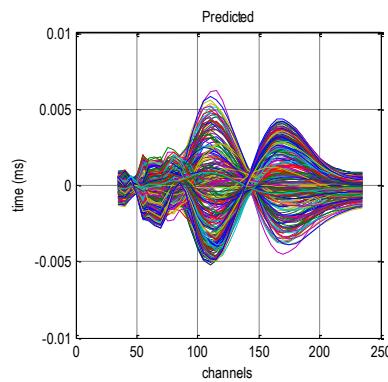
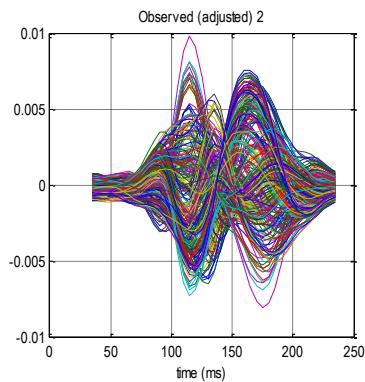
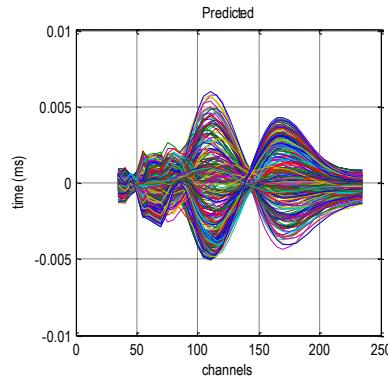
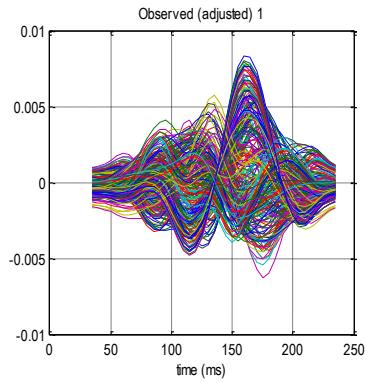
# Fitting DCMs to data



# Fitting DCMs to data

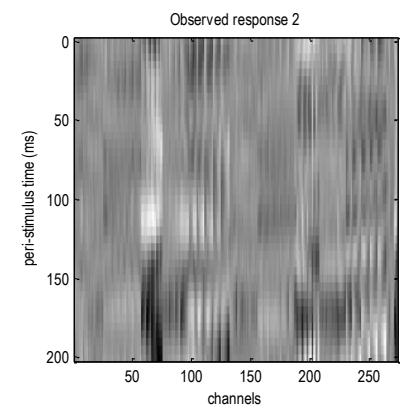
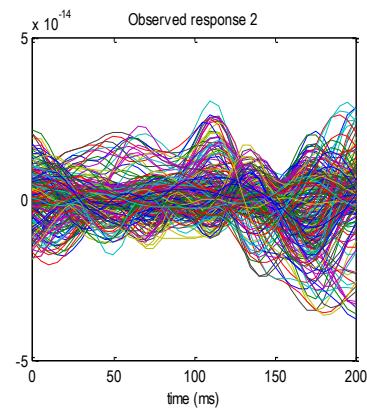
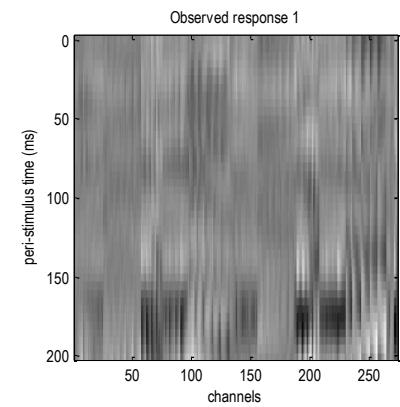
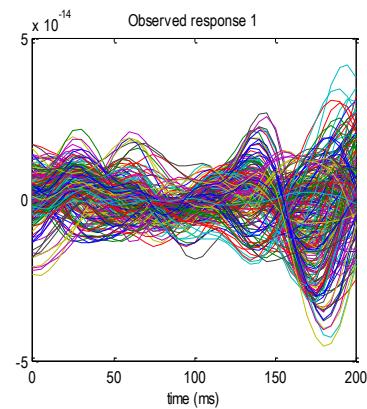


# Fitting DCMs to data



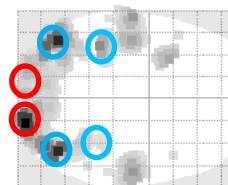
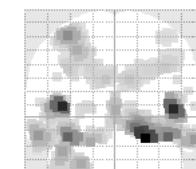
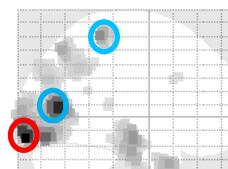
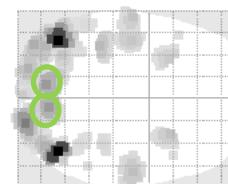
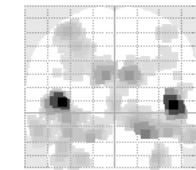
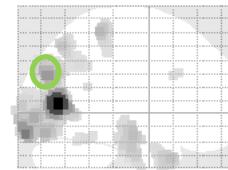
# Fitting DCMs to data

## 1. Check your data



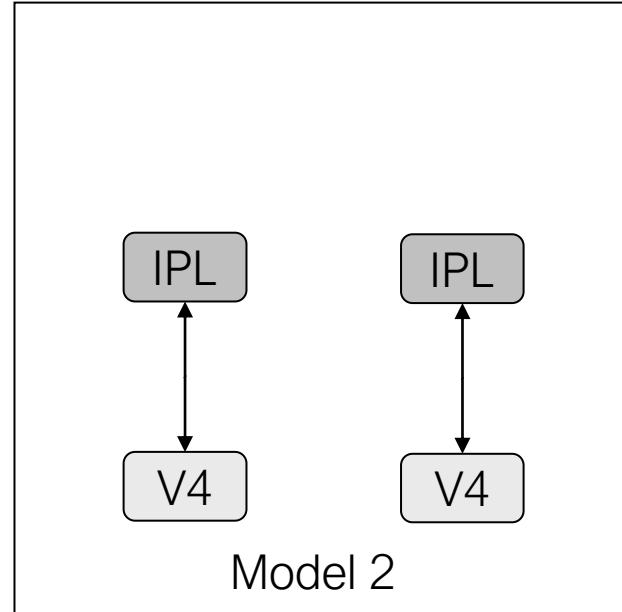
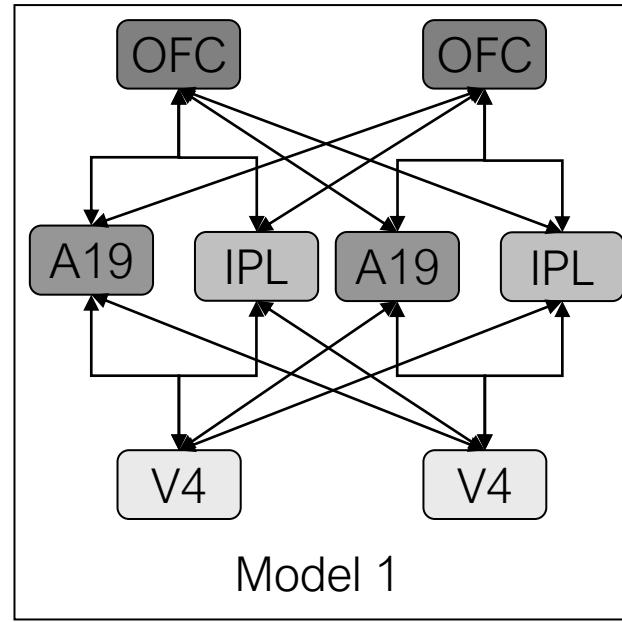
# Fitting DCMs to data

1. Check your data
2. Check your sources



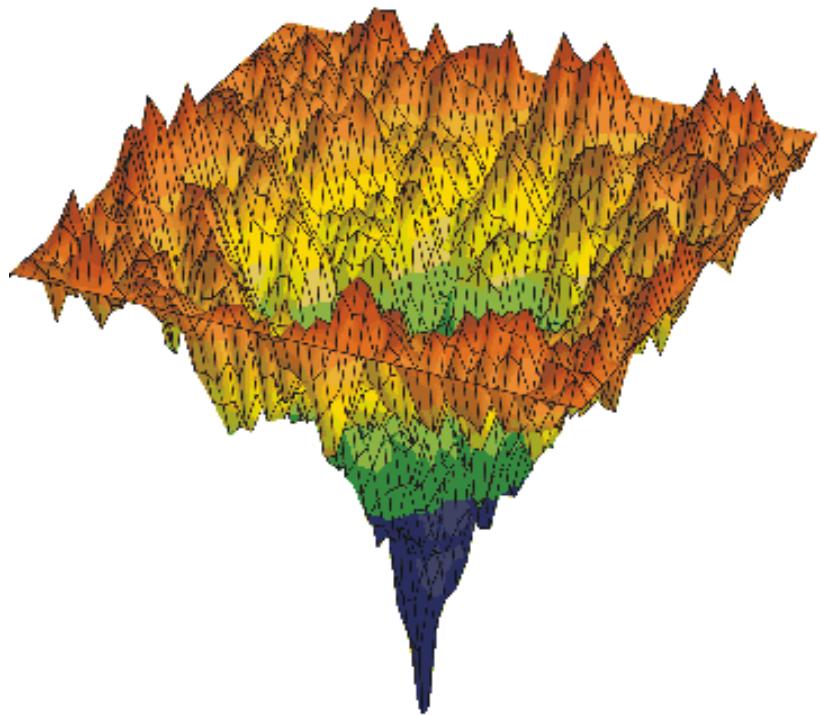
# Fitting DCMs to data

1. Check your data
2. Check your sources
3. Check your model

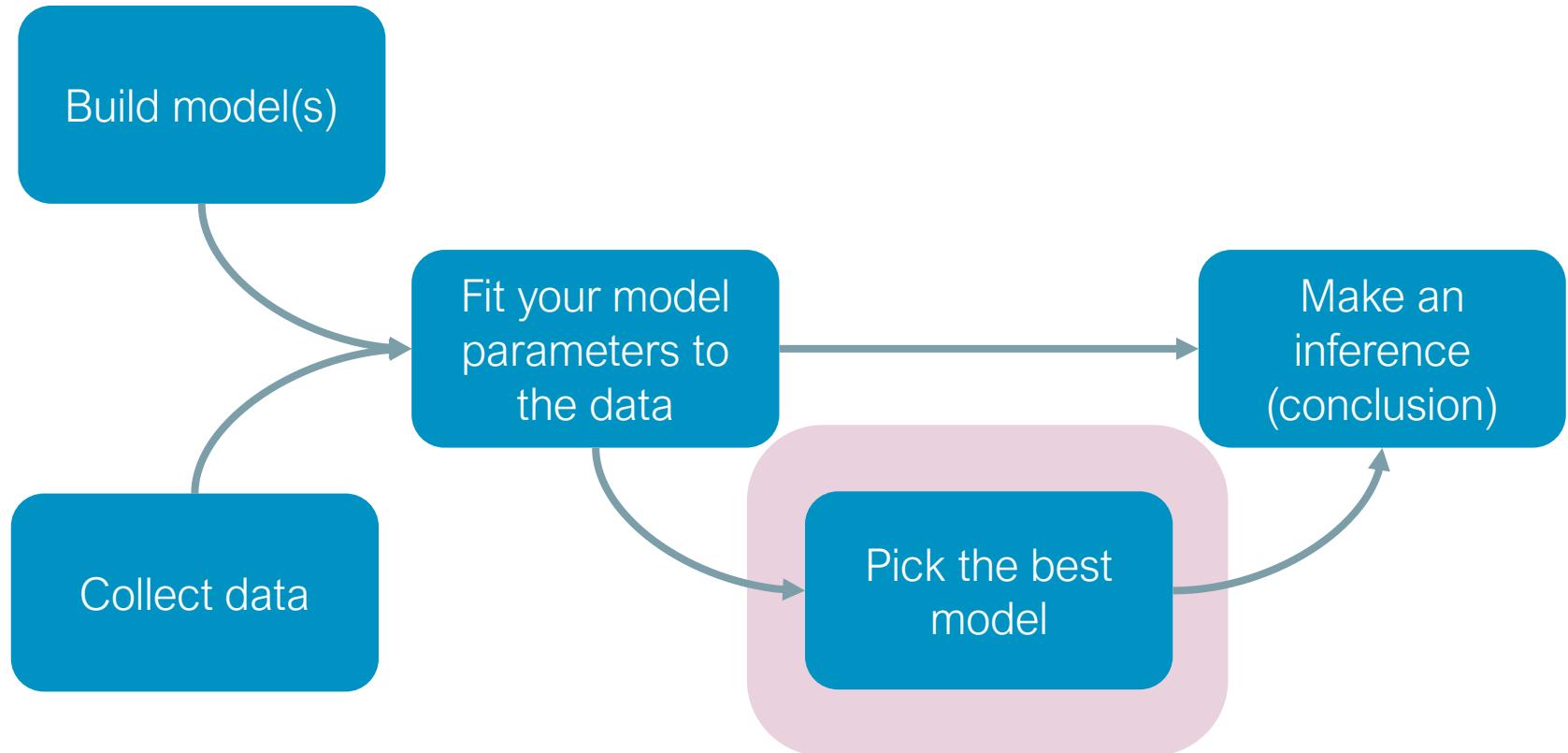


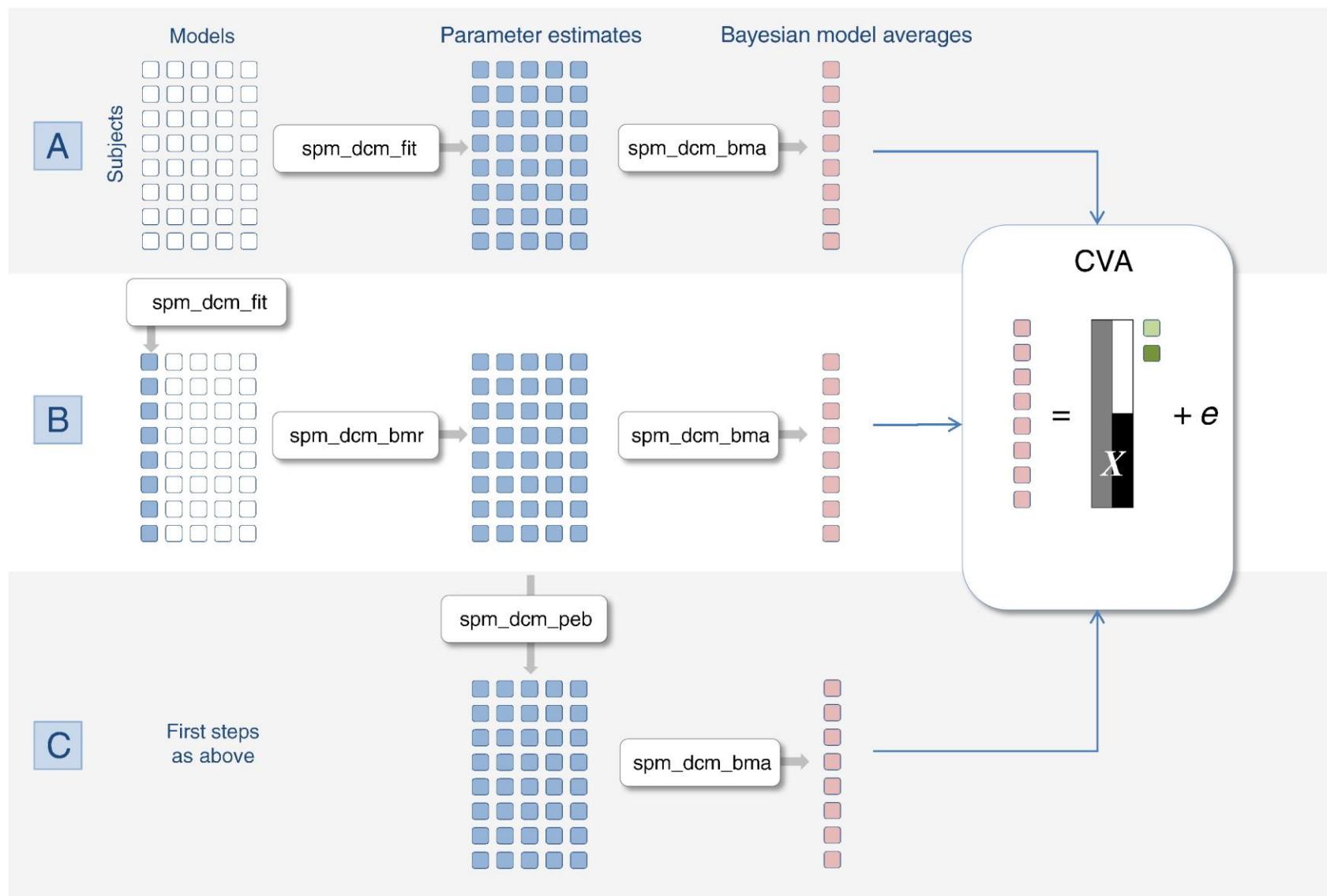
## Fitting DCMs to data

1. Check your data
2. Check your sources
3. Check your model
4. Re-run model fitting

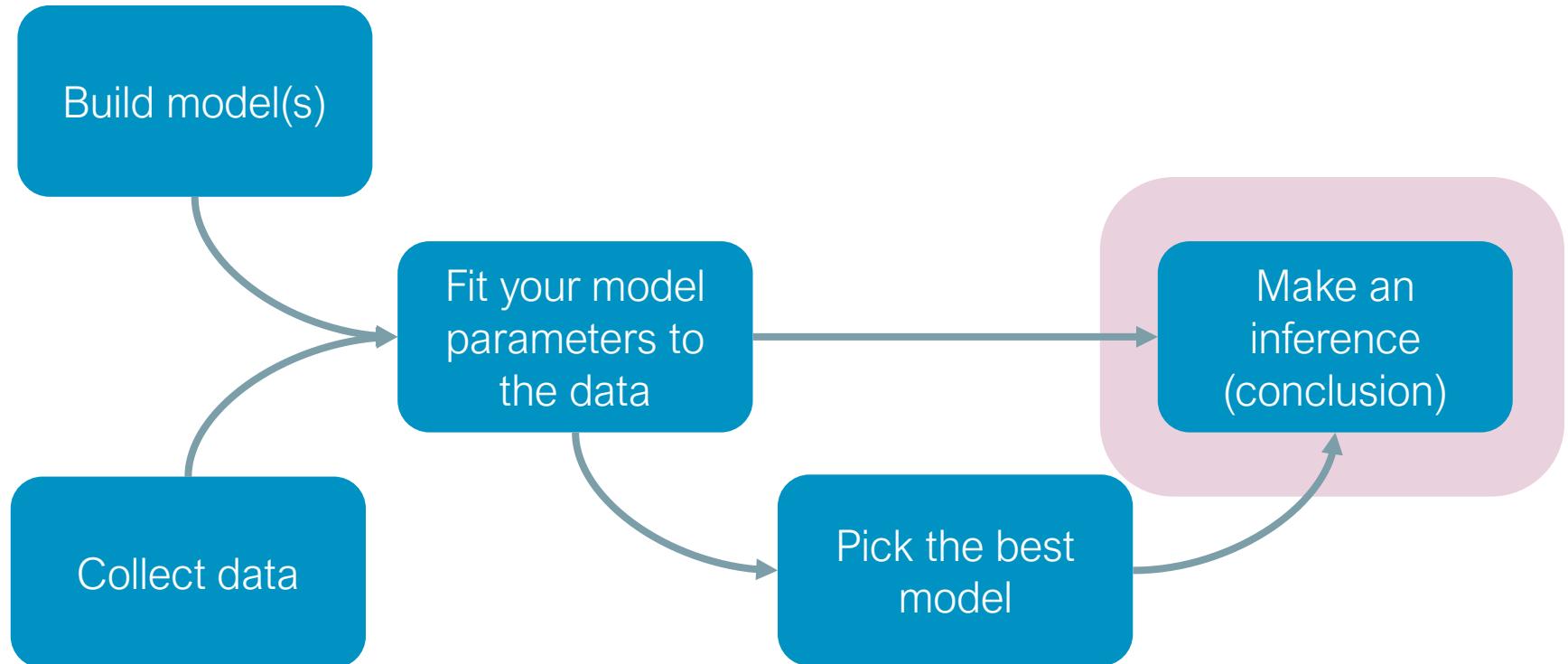


# The DCM analysis pathway





# The DCM analysis pathway



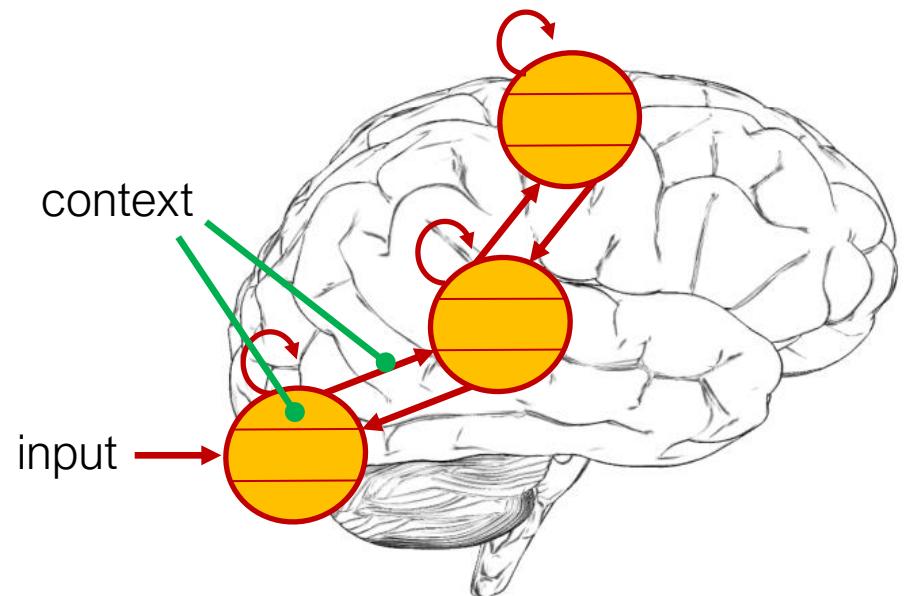
Does network XYZ explain my data better than network XY?

Which XYZ connectivity structure best explains my data?

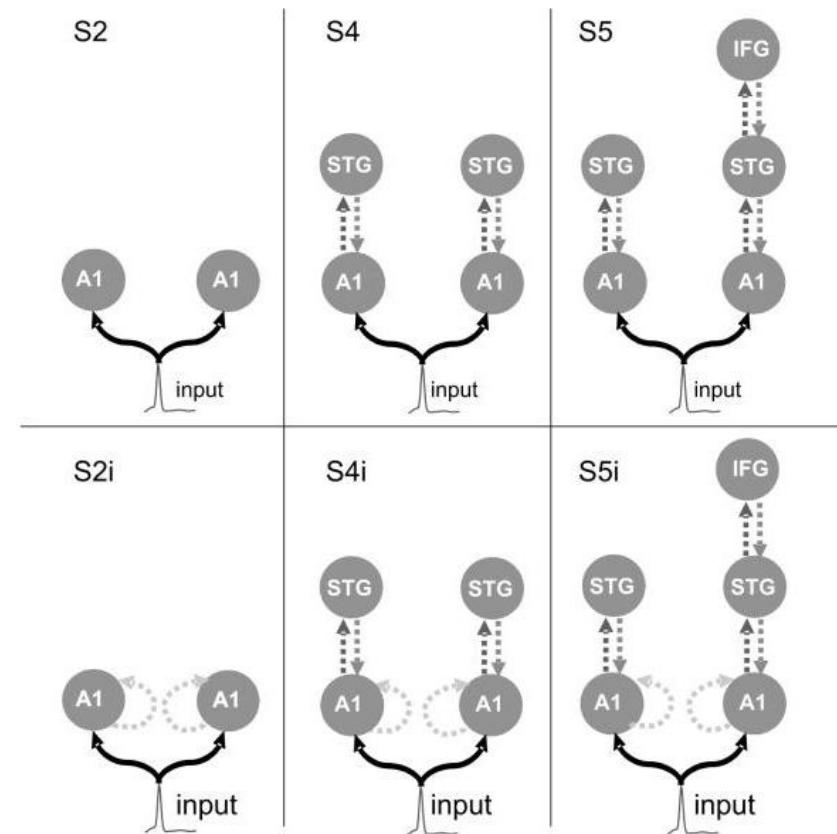
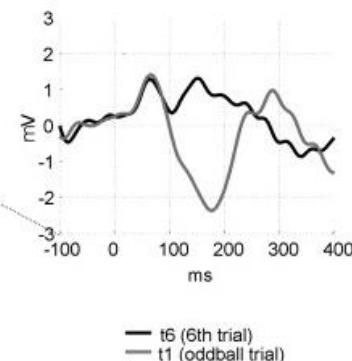
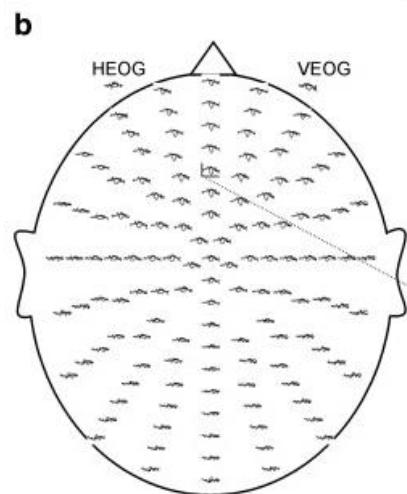
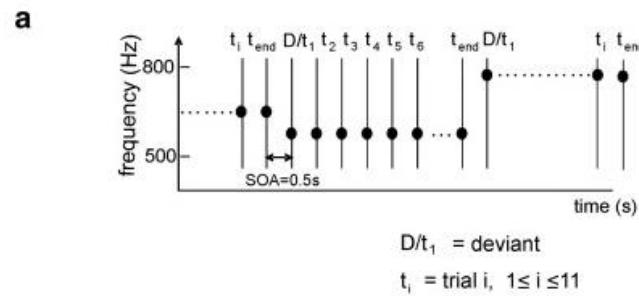
Are X & Y linked in a bottom-up, top-down or recurrent fashion?

Is my effect driven by extrinsic or intrinsic connections?

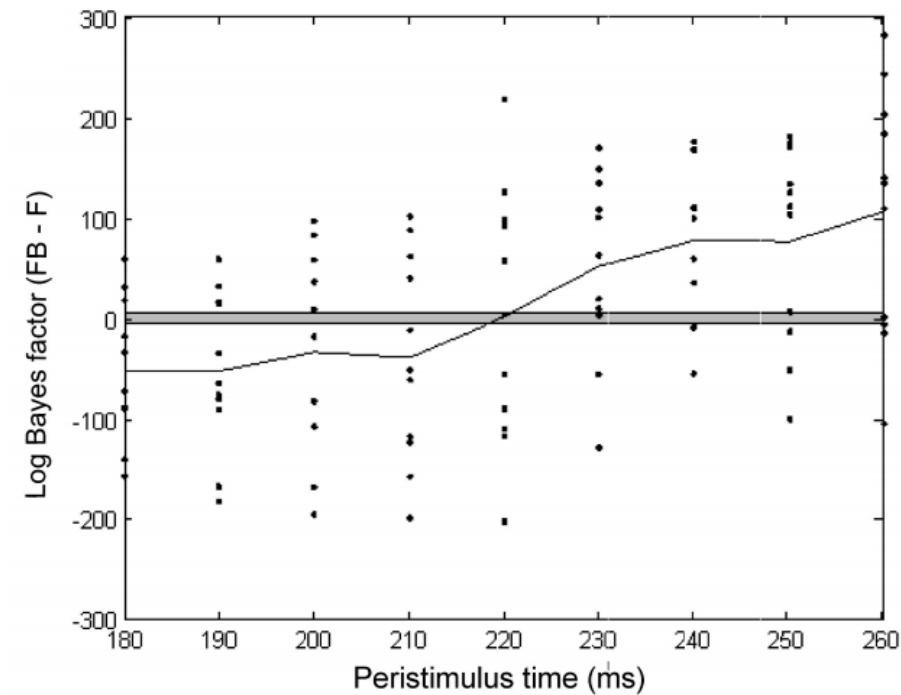
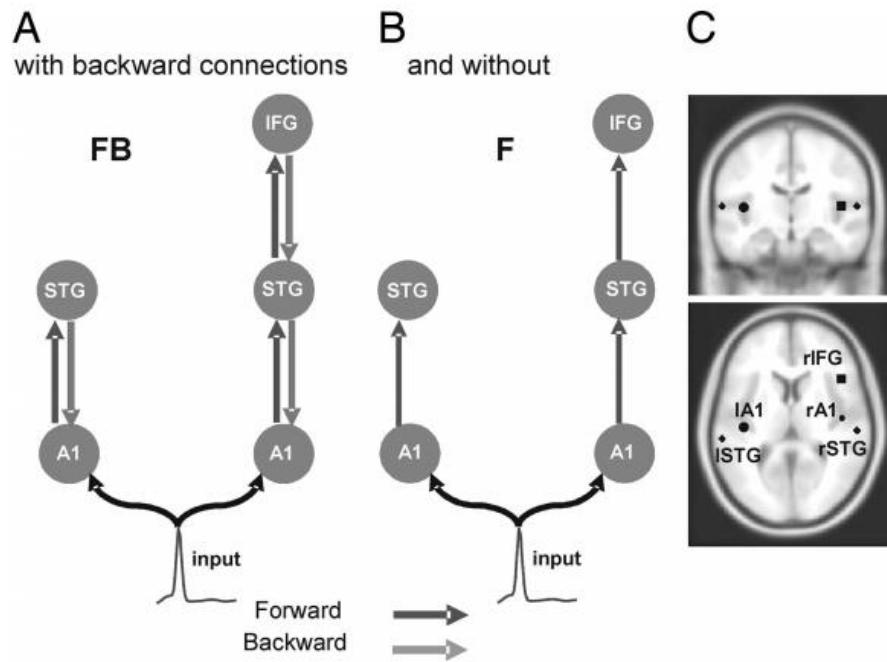
Which connections/populations are affected by contextual factors?



# Example #1: Architecture of MMN

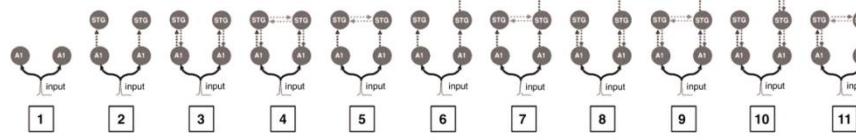


## Example #2: Role of feedback connections

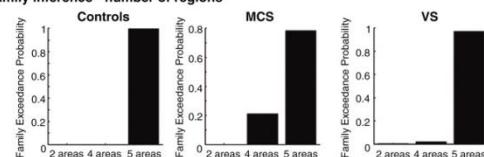


# Example #3: Group differences

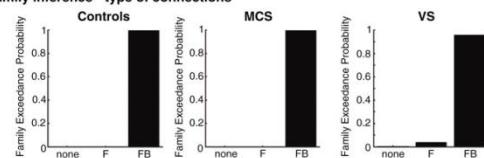
**A DCM models**



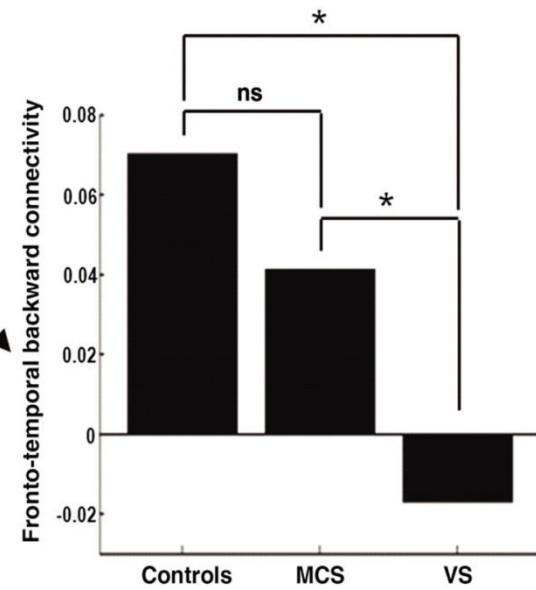
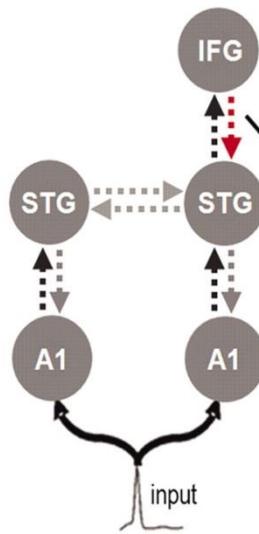
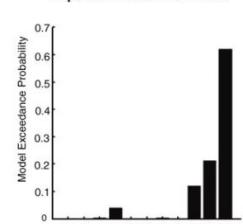
**B Family inference - number of regions**



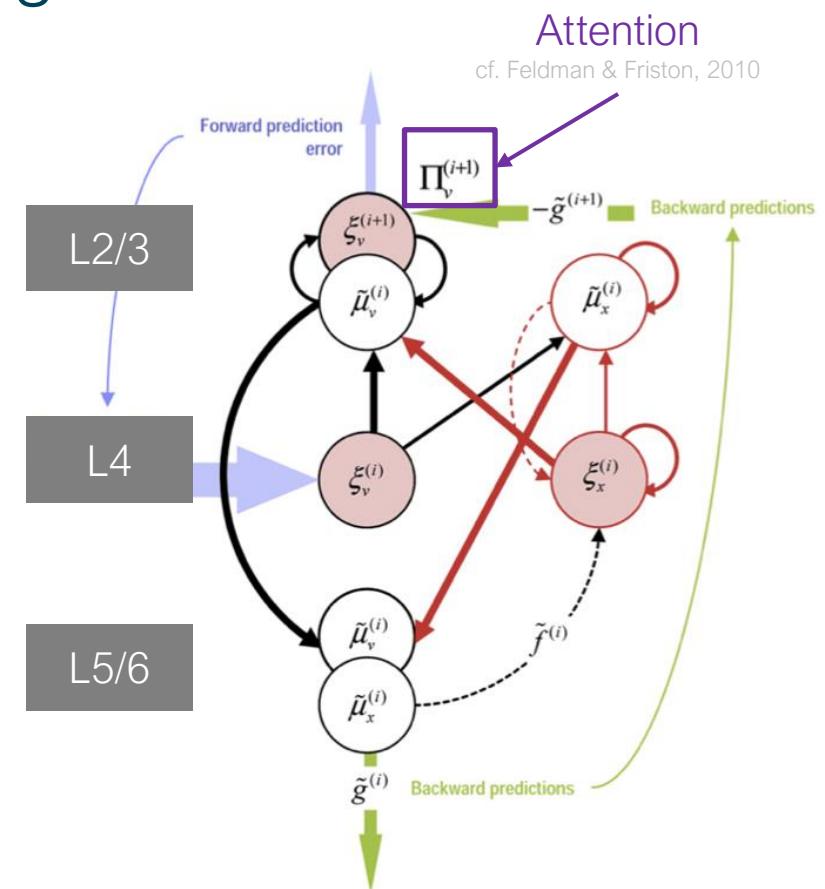
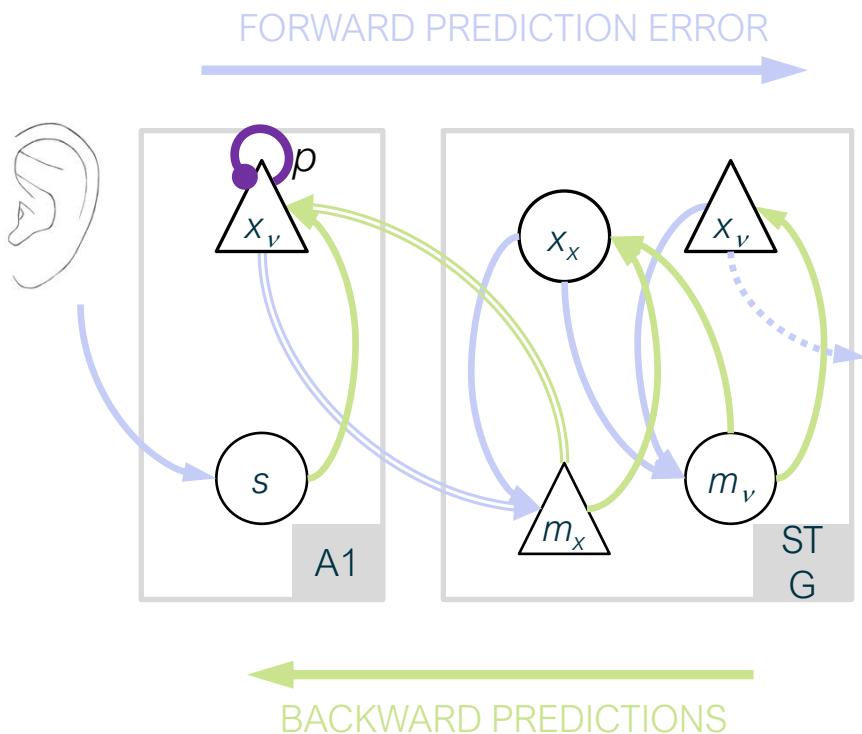
**C Family inference - type of connections**



**D Population-level best model**

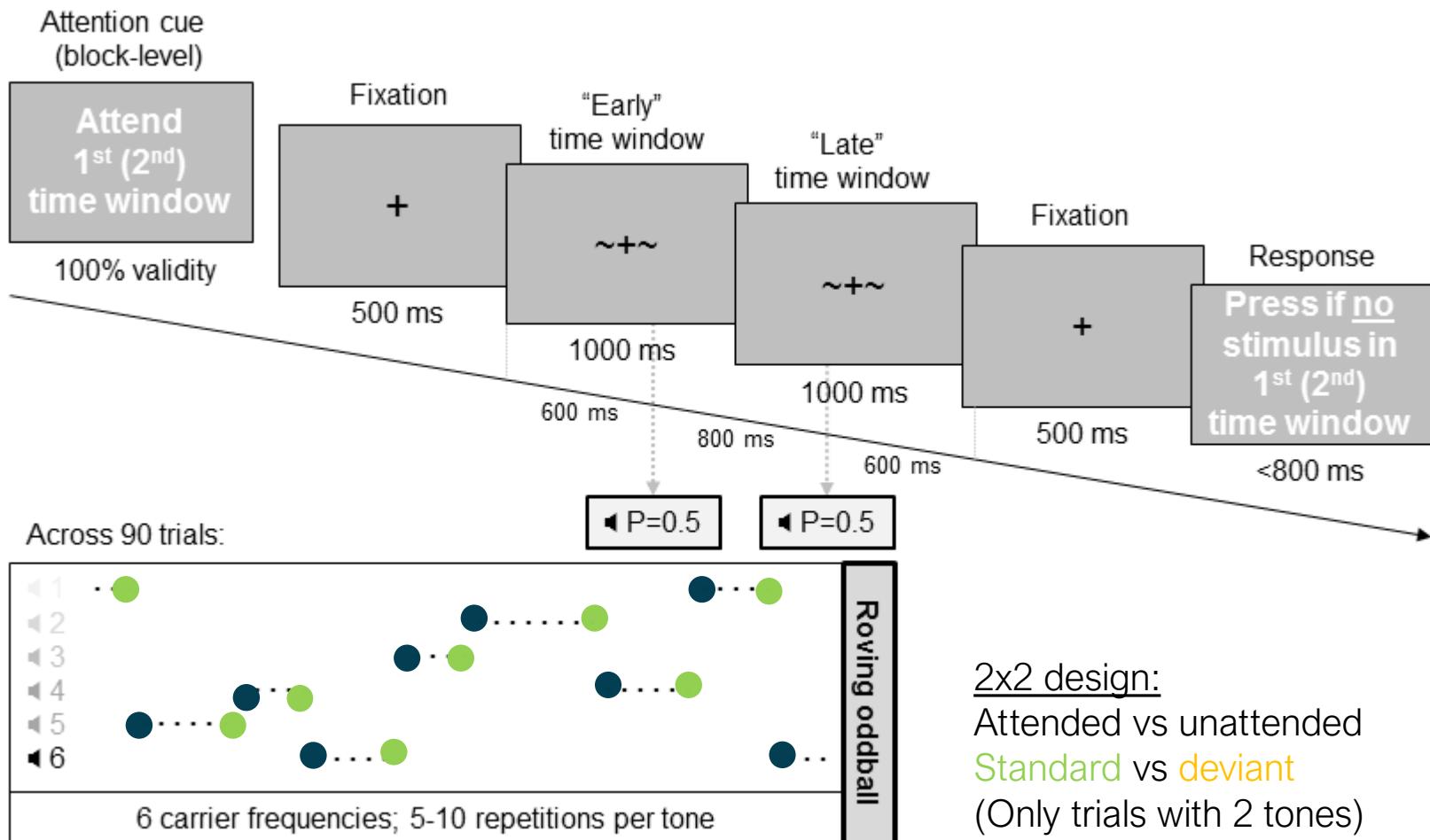


# Example #4: Factorial design & CMC



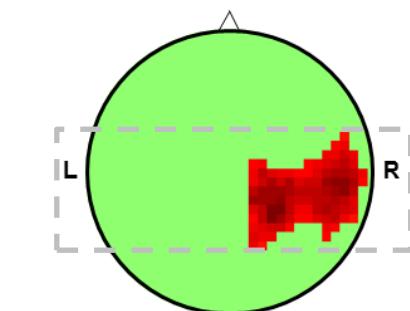
Bastos et al., *Neuron* 2012

Auksztulewicz & Friston, 2015

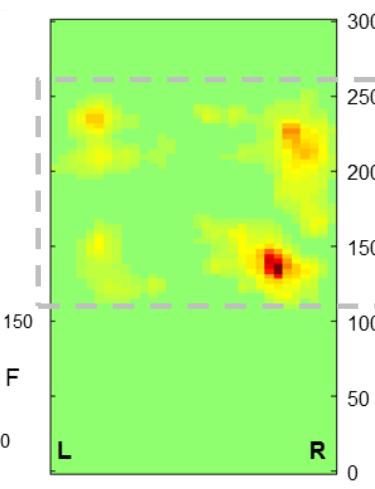
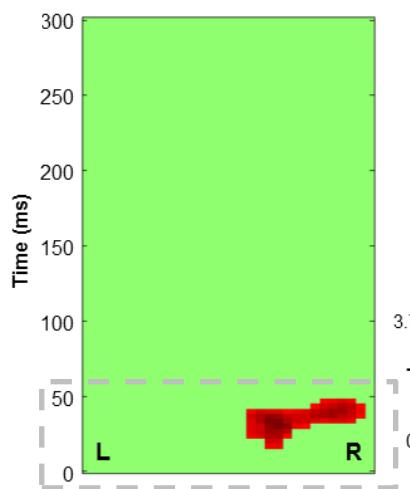
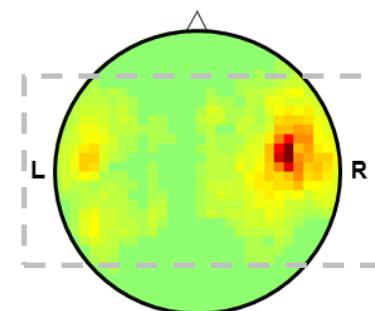


N=20

Attention

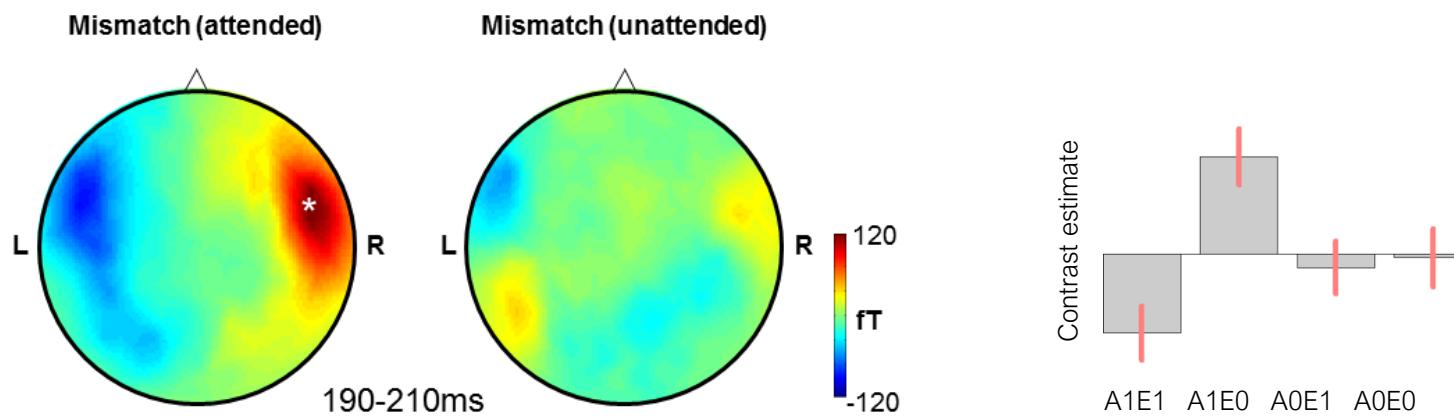


Expectation

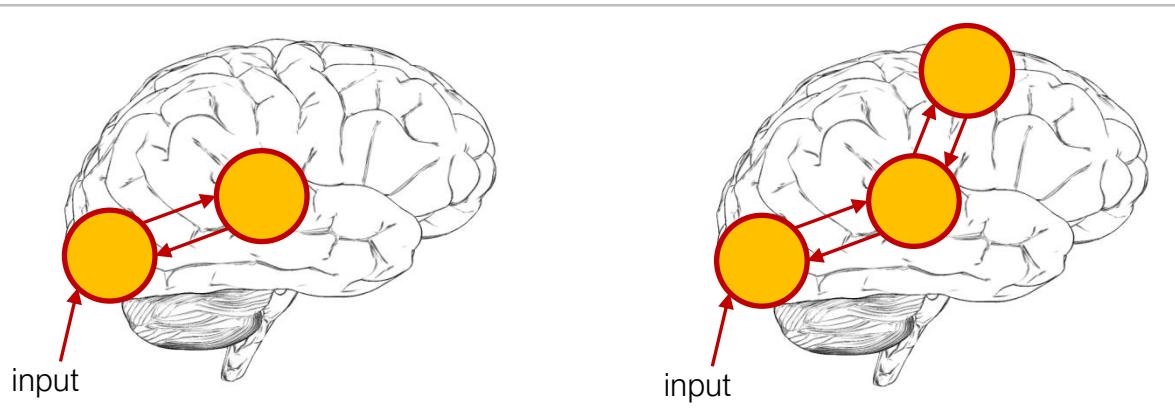


T  
F  
0  
3.7

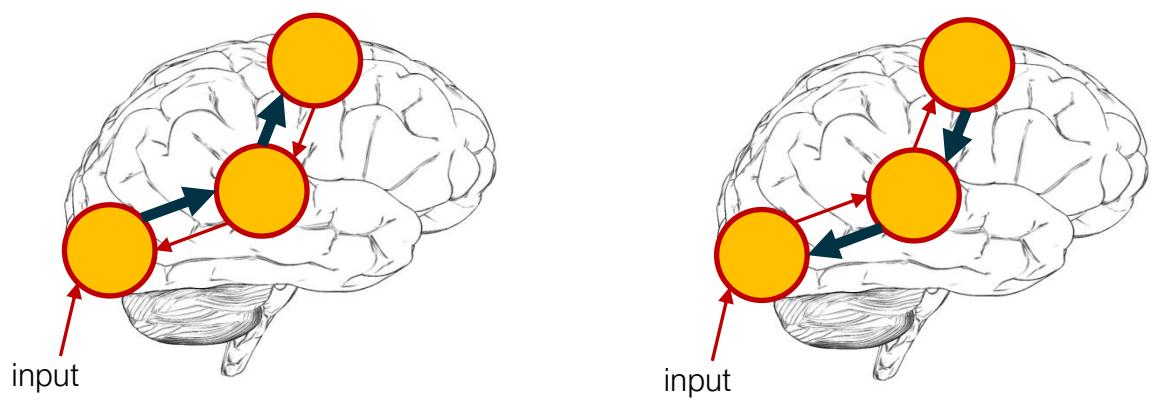
Flexible factorial design  
Thresholded at  $p < .005$  peak-level  
Corrected at a cluster-level  $p_{\text{FWE}} < .05$



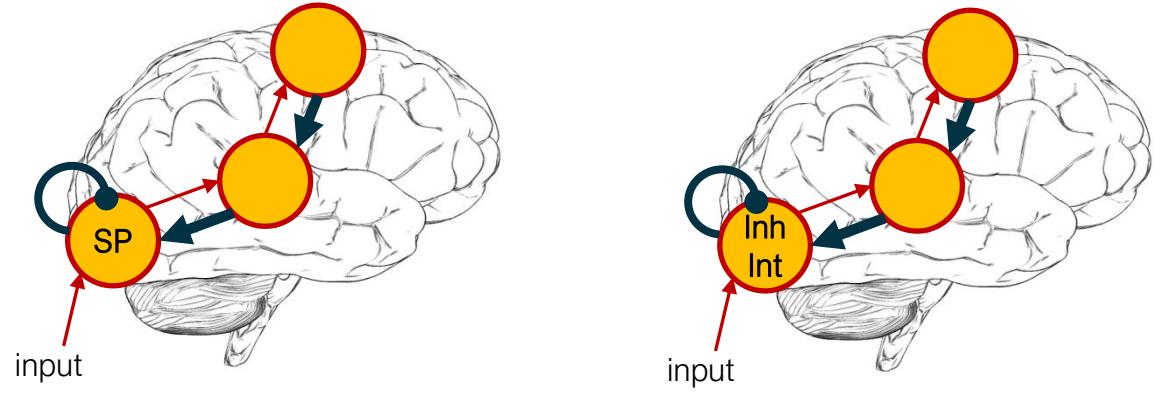
Connectivity structure

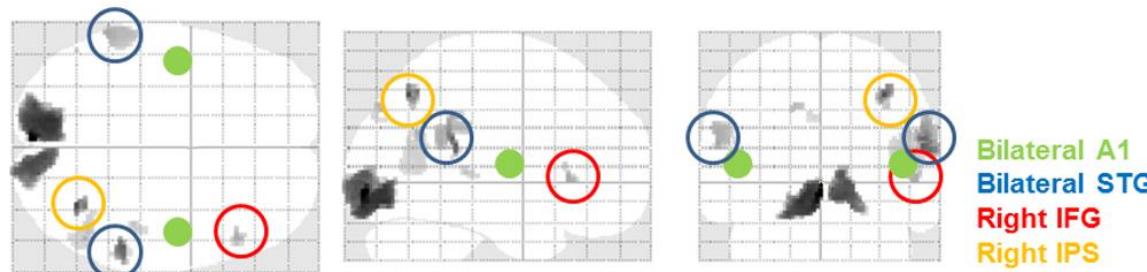


Extrinsic modulation

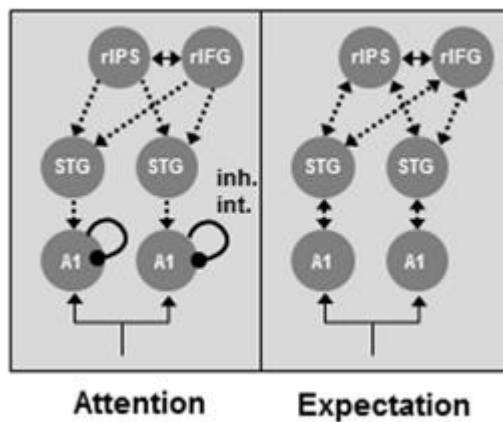


Intrinsic modulation

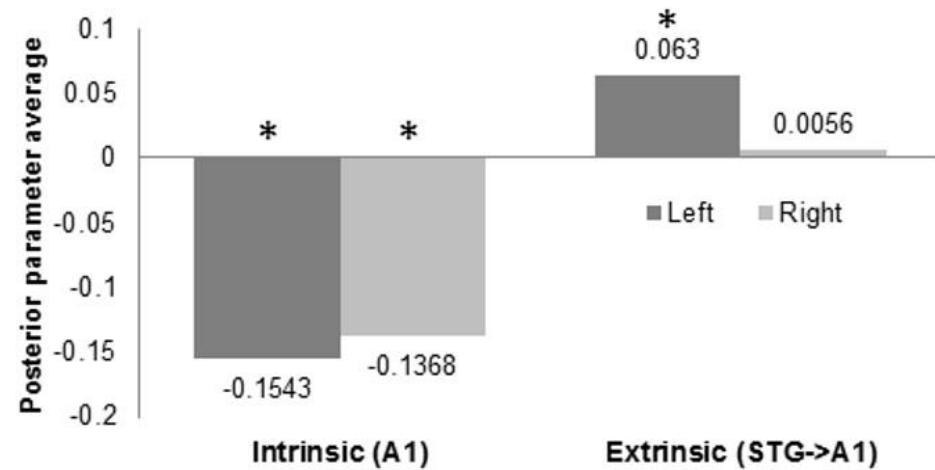


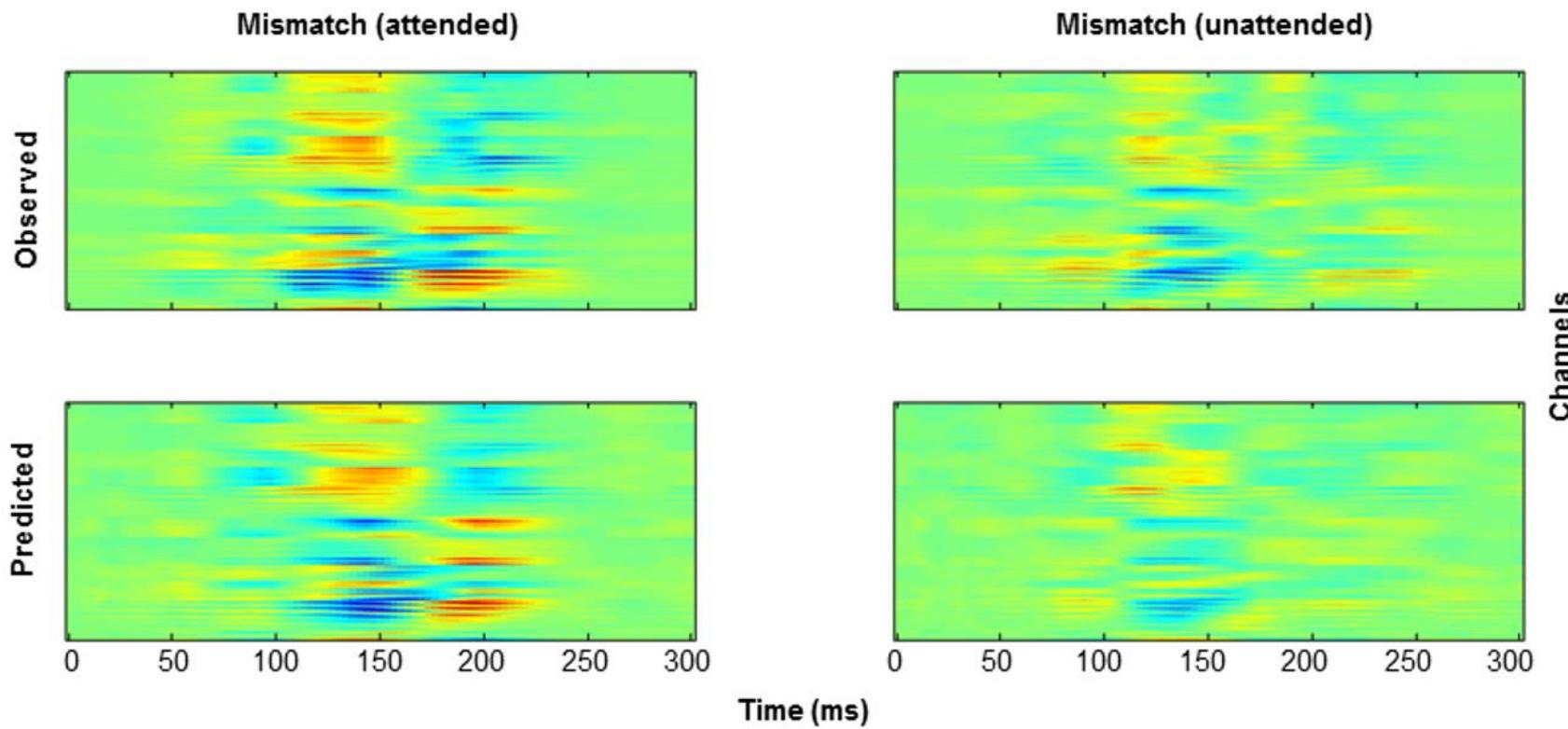


### Winning model



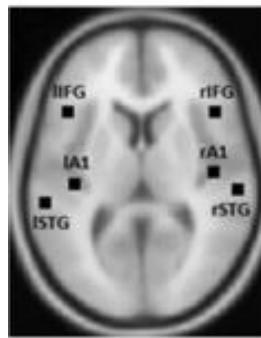
### Parameter inference



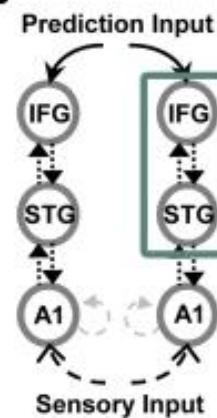


# Example #5: Same paradigm, different data

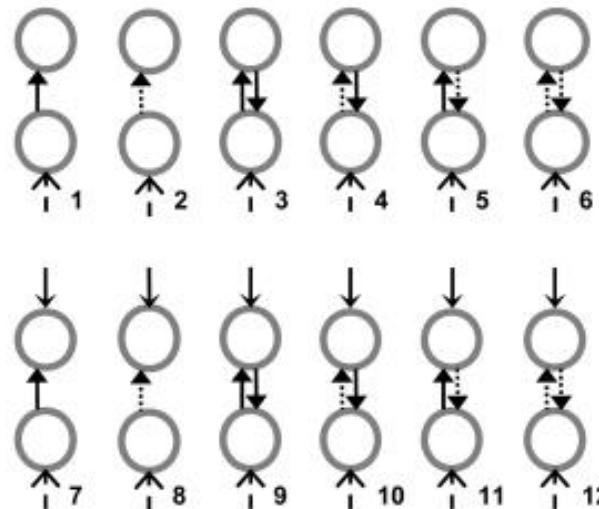
**A**



**B**

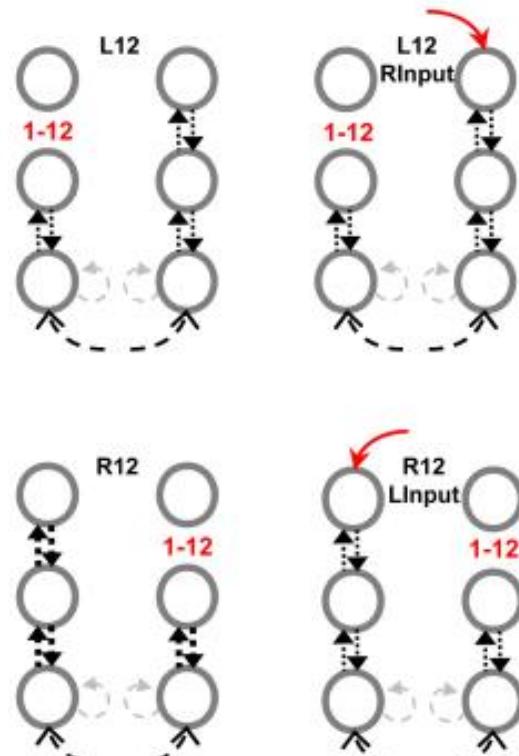


**C**

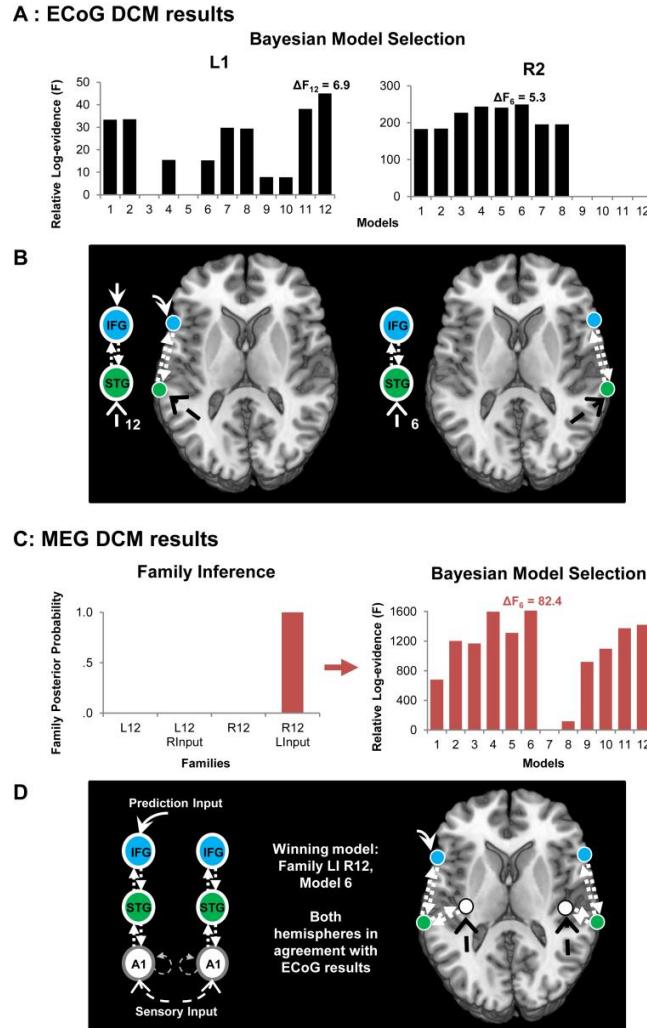


**D**

MEG Model families

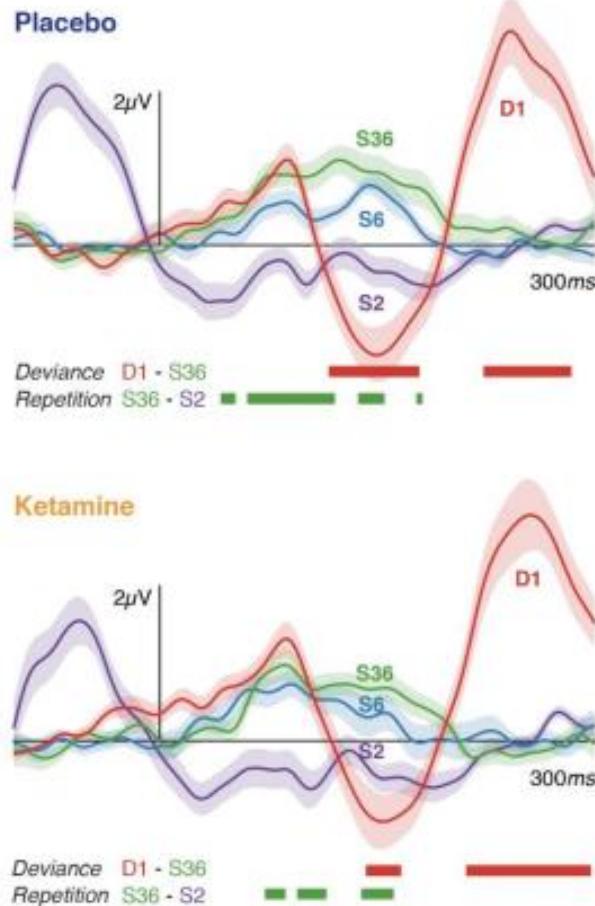


# Example #5: Same paradigm, different data

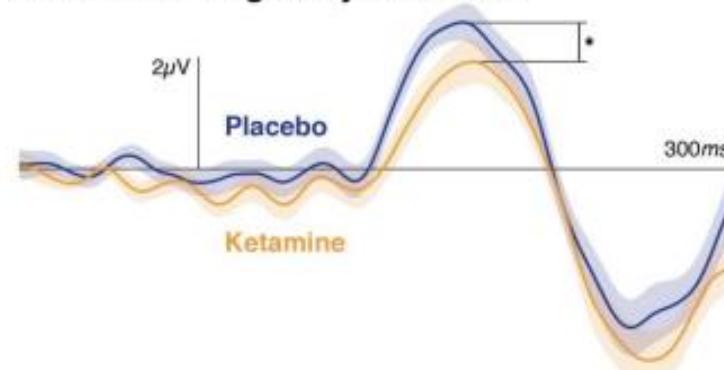


# Example #6: Hierarchical modelling

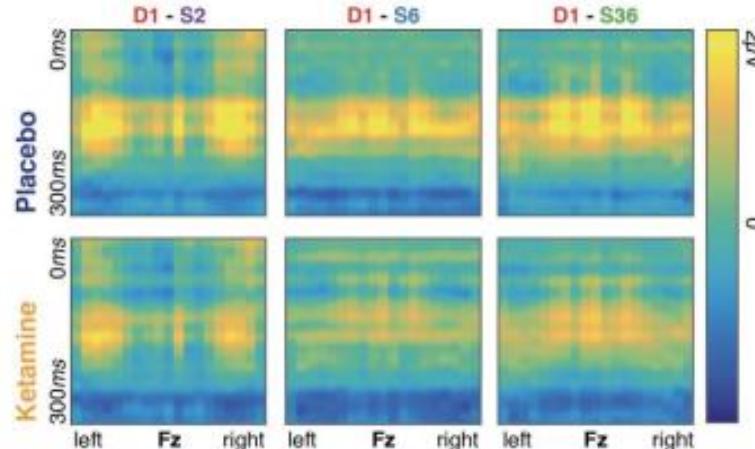
**A** Evoked response potentials at  $Fz$



**B Mismatch negativity waveform**

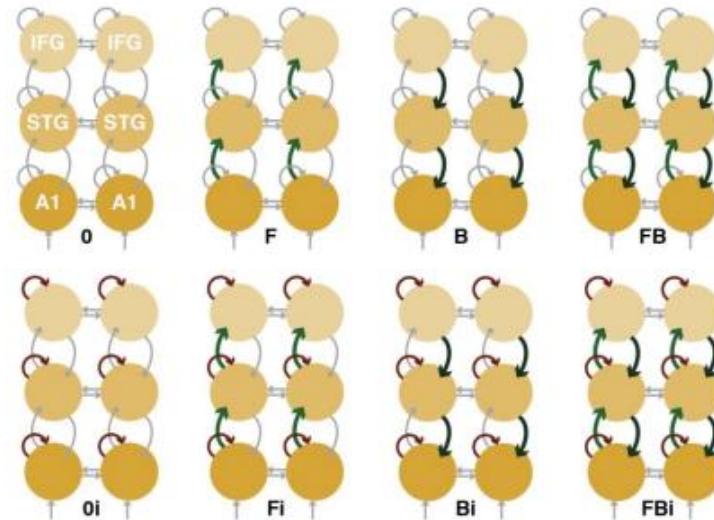


**C Scalp topography of mismatch responses**

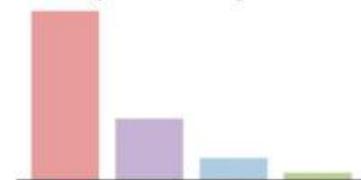


# Example #6: Hierarchical modelling

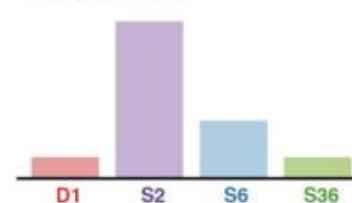
**A First level model space: Effects of repetition**



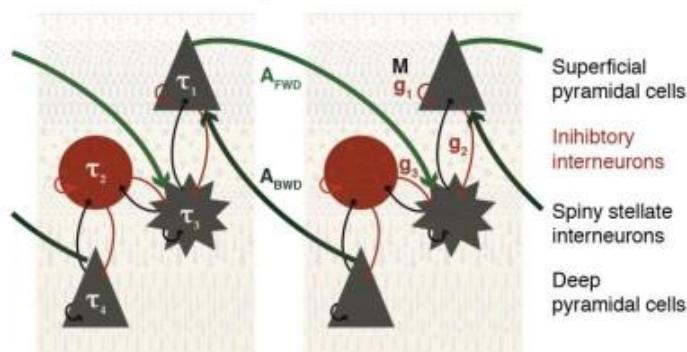
**Parametric effects of repetition**  
Monophasic Decay



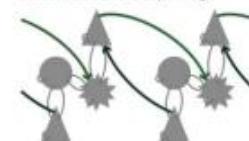
**Phasic Effect**



**B Second level model space: Effects of ketamine**



**Extrinsic coupling**



$A_{FWD}$   
 $A_{BWD}$   
 $B_{FWD}$   
 $B_{BWD}$

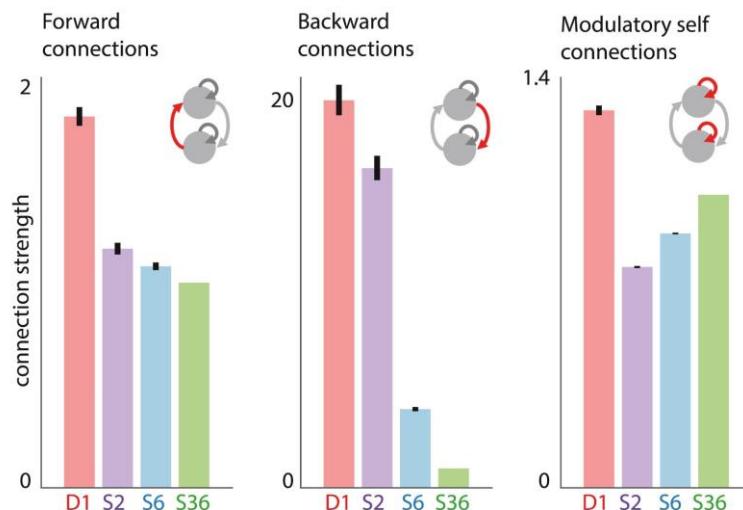
**Intrinsic coupling**



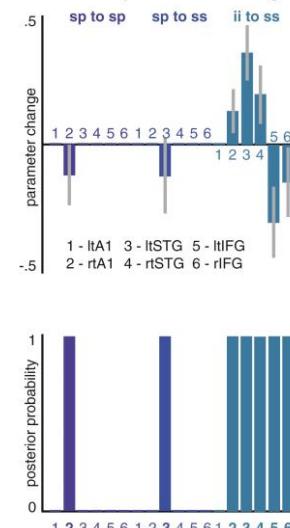
$\tau$   
 $g$   
 $M$   
 $N$

# Example #6: Hierarchical modelling

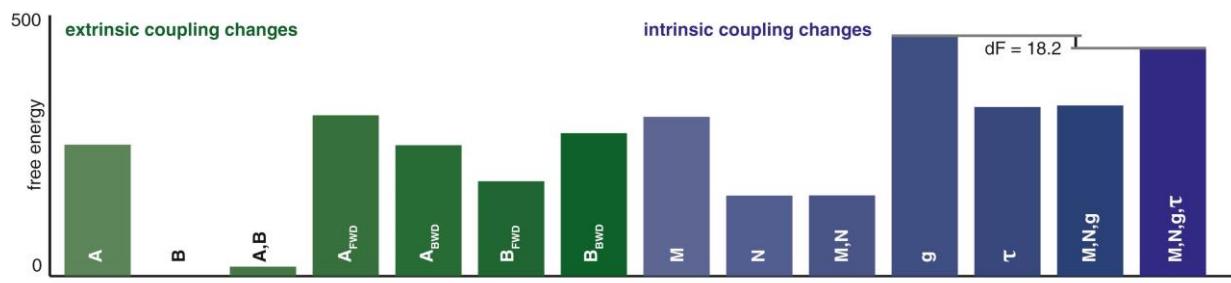
Parameter changes during repeated exposure



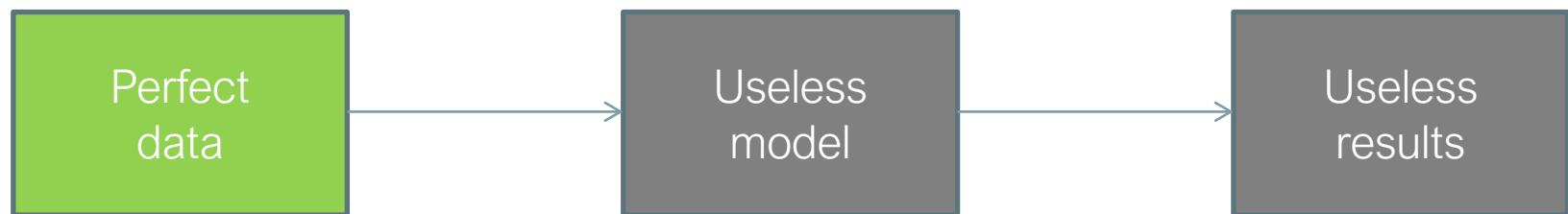
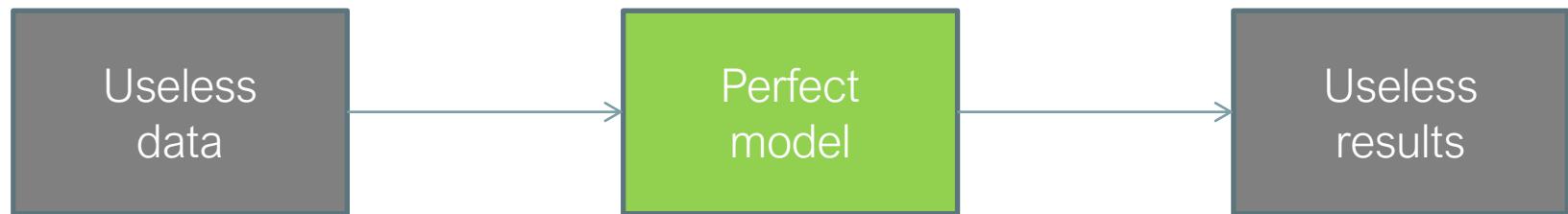
Induced parameter changes



Bayesian model comparison on reduced models explaining ketamine effects



# Motivate your assumptions!



# References

## Overview

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## Model specifics

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## Group inference

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## Examples

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Biol Psychiatry Cogn Neurosci Neuroimaging. 2019 Feb;4(2):140-150. doi: 10.1016/j.bpsc.2018.07.003.

# Thank you!

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