

Dynamic Causal Modelling for fMRI

SPM for fMRI Course

Professor Peter Zeidman

Group Leader, Neurovascular Modelling Group Chair, Methods Group Functional Imaging Laboratory (FIL) UCL Department of Imaging Neuroscience

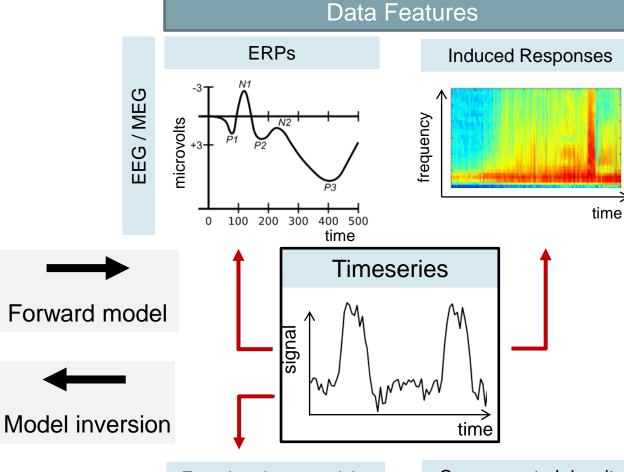


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- 1. Types of connectivity
- 2. Motivating example: stroke
- 3. DCM framework & Bayesian model comparison
- 4. Specific models for fMRI
- 5. Stroke example results
- 6. Group analysis using PEB

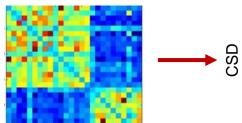
Neuronal causes

Neural circuitry (effective connectivity)

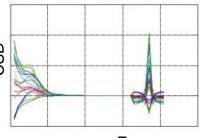


Functional connectivity

fMRI



Cross-spectral density



Frequency

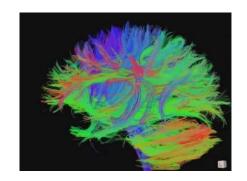


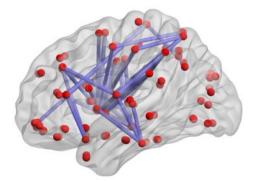
Connectivity

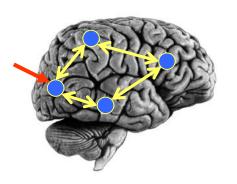
Structural Connectivity
 Physical connections of the brain



Effective Connectivity
 Causal relationships between brain regions









Dynamic Causal Modelling

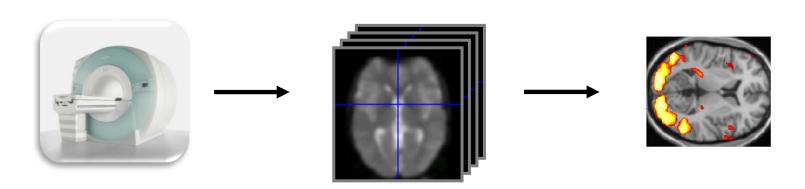
is a framework

for inferring the causes of

neuroimaging data



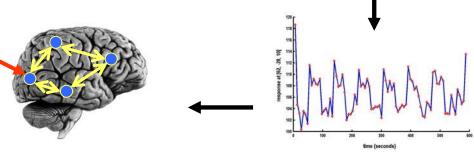
Where DCM sits in the pipeline



Functional MRI acquisition and image reconstruction

Image preprocessing (realignment, coregistration, normalisation, smoothing)

Statistical Parameter Mapping (SPM) / General Linear Model



Dynamic Causal Modelling (DCM)

Timeseries extraction from Regions of Interest (ROIs)



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Neuropsychologia 50 (2012) 3621-3635



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Research Report

Reading without the left ventral occipito-temporal cortex

Mohamed L. Seghier ^{a,*}, Nicholas H. Neufeld ^{a,b}, Peter Zeidman ^a, Alex P. Leff ^a, Andrea Mechelli ^c, Arjuna Nagendran ^a, Jane M. Riddoch ^d, Glyn W. Humphreys ^{d,e}, Cathy J. Price ^a

^a Wellcome Trust Centre for Neuroimaging, Institute of Neurology, UCL, London WC1N 3BG, UK

^b University of Toronto, Toronto, ON, Canada M5S 1A8

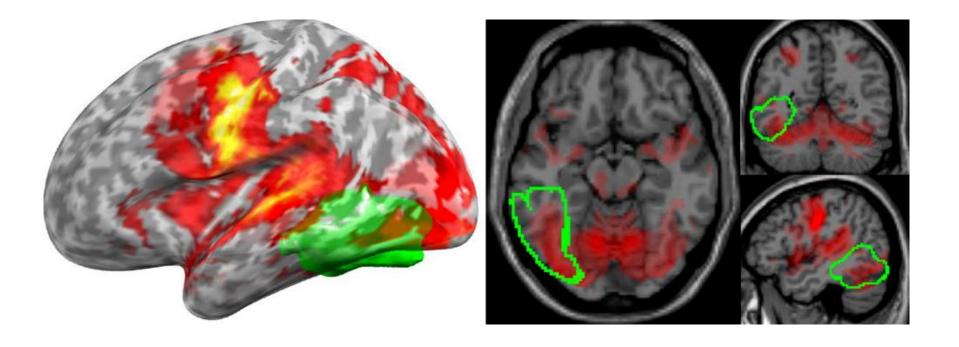
^c Institute of Psychiatry, King's College London, London SE5 8AF, UK

^d School of Psychology, University of Birmingham, Edgbaston, Birmingham B15 2TT, UK

e Department of Experimental Psychology, Oxford University, Oxford OX3 9DU, UK



Question: how is Patient AH able to read?



- Reading > fixation (29 controls)
- Lesion (Patient AH)



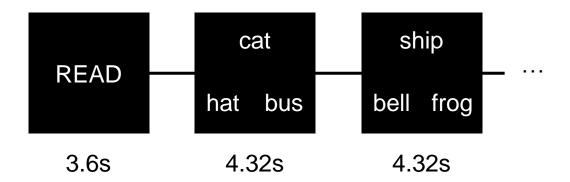
Question: how is Patient AH able to read?

Experimental design

[2 x 3] factorial(-ish) design:

- Stimulus type (words or pictures)
- Naming or reading
- + control conditions

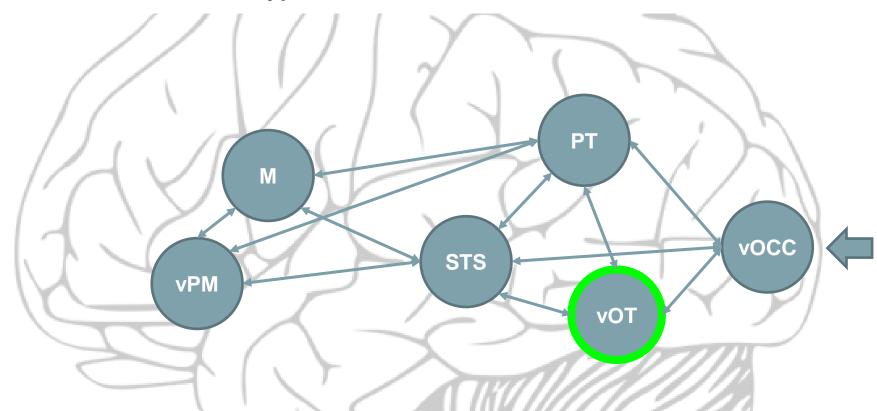
Example block



Results







M	motor cortex
vPM	ventral pre-motor cortex
STS	superior temporal sulcus
PT	planum temporale
vOT	ventral occipito-temporal cortex
vOCC	ventral occipital cortex

Seghier et al., Neuropsychologia, 2012

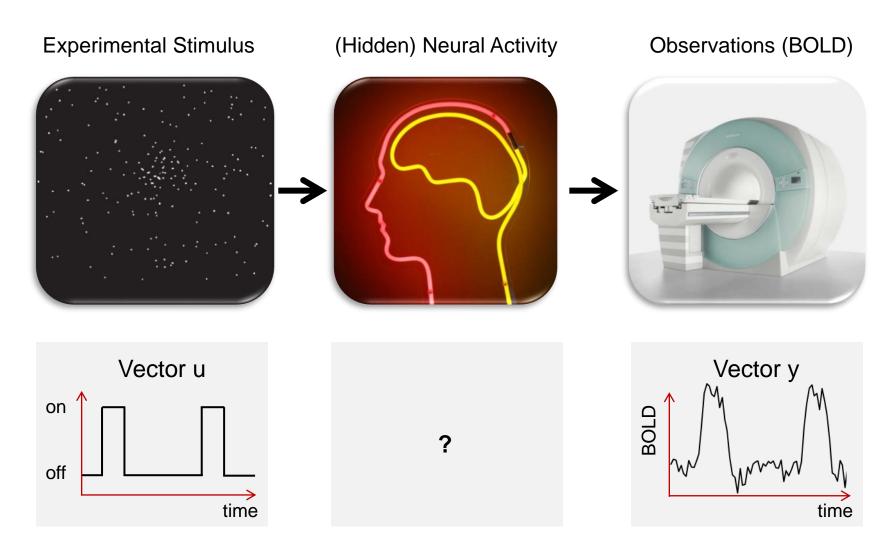


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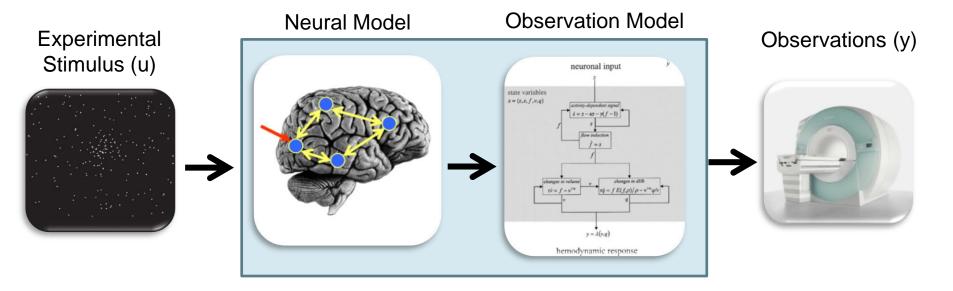
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The system of interest







How brain activity **z** changes over time

$$\dot{z} = f(z,u,\theta^n)$$

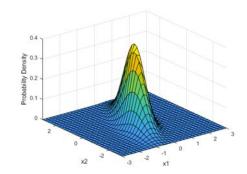
What we would see in the scanner, y, given the neural model?

$$y = g(z, \theta^h)$$

Stimulus from Buchel and Friston, 1997 Figure 3 from Friston et al., Neuroimage, 2003 Brain by Dierk Schaefer, Flickr, CC 2.0

Model Inversion (estimation) uses an algorithm called Variational Laplace, which produces two outputs:

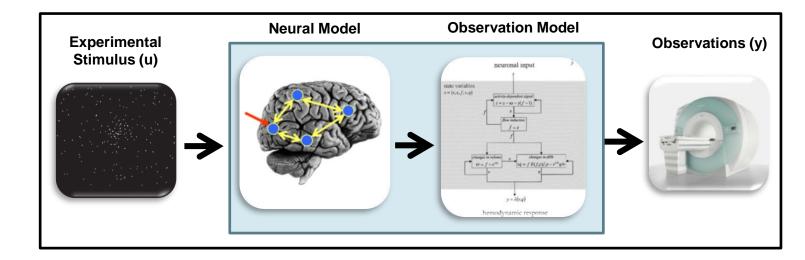
• Posterior probability distribution over the parameters $p(\theta|y,m)$



• Approximation of the model evidence p(y|m) called the free energy F

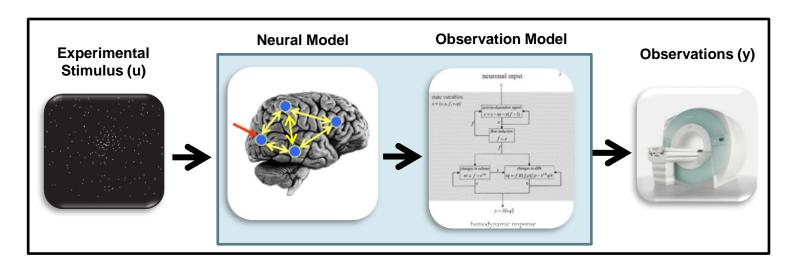
$$F \cong \log p(y|m) = \operatorname{accuracy} - \operatorname{complexity}$$





Model 1:

Model comparison: Which model best explains my observed data?



Model 2:



1. We embody each of our hypotheses in a generative model.

The generative model separates neural activity from haemodynamics

2. We perform model estimation (inversion)

This identifies parameters $\theta = \{\theta^n, \theta^h\}$ which make the model best fit the data and the free energy F which is a score for the quality of the model

3. We inspect the estimated parameters and / or we compare models to see which best explains the data.



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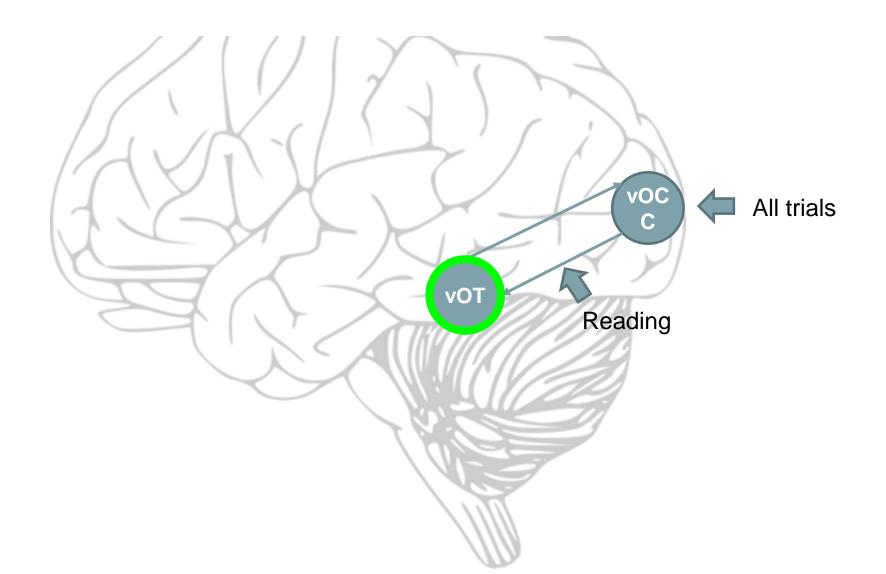


"How does brain activity, z, change over time?"

$$\dot{z} = (A + \sum_{j=1}^{m} u_j B^j)z + Cu$$

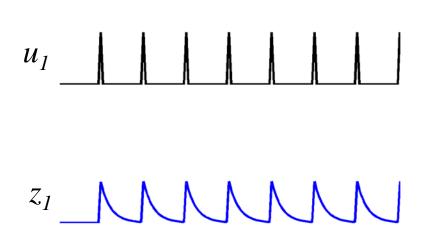
Friston et al. 2003







"How does brain activity, z, change over time?"



$$z_1$$
 vocc a

C

Driving input u_1

$$\dot{z}_1 = az + cu_1$$

Inhibitory self-connection (Hz). Rate constant: controls rate of decay in region 1. More negative = faster decay.



"How does brain activity, z, change over time?"

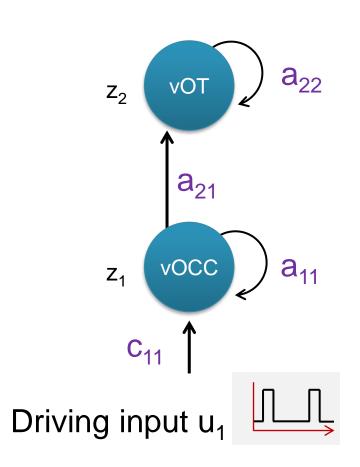
Change of activity in vOCC:

$$\dot{z}_1 = a_{11}z_1 + c_{11}u_1$$

Change of activity in vOT:

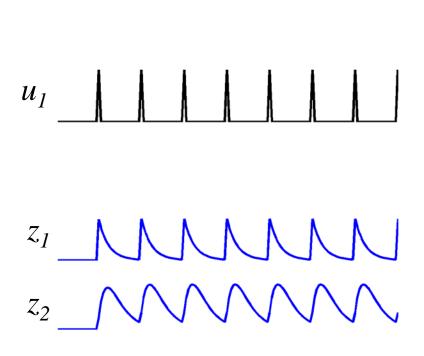
$$\dot{z}_2 = a_{22}z_2 + a_{21}z_1$$
 \uparrow

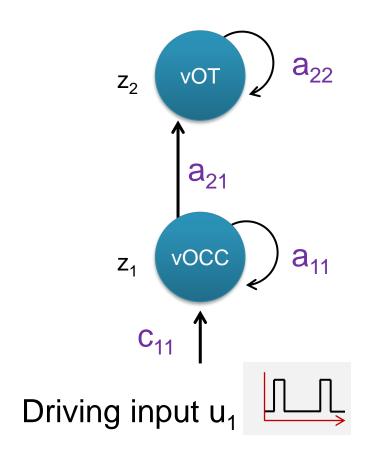
Self decay V1 input





"How does brain activity, z, change over time?"







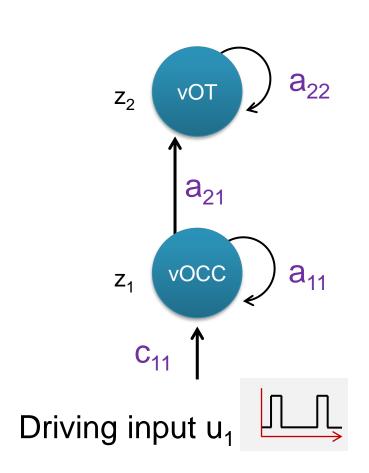
"How does brain activity, z, change over time?"

$$\begin{bmatrix} \dot{z_1} \\ \dot{z_2} \end{bmatrix} = \begin{bmatrix} a_{11} & 0 \\ a_{21} & a_{22} \end{bmatrix} \begin{bmatrix} z_1 \\ z_2 \end{bmatrix} + \begin{bmatrix} c_{11} \\ 0 \end{bmatrix} u_1$$



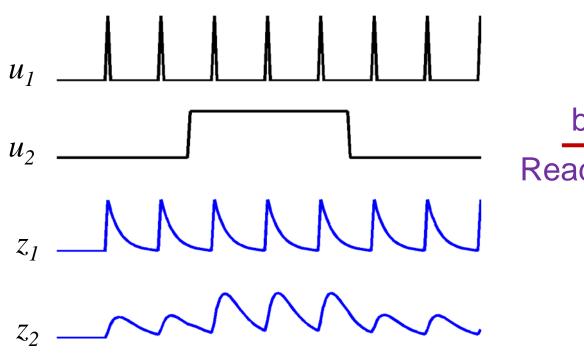
Columns are outgoing connections
Rows are incoming connections

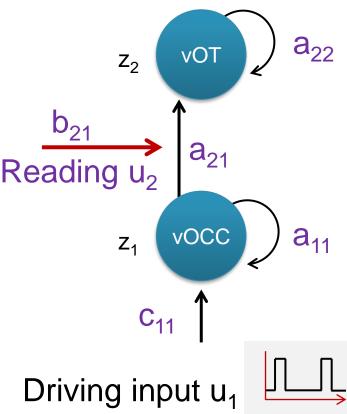
$$\dot{z} = Az + Cu_1$$





"How does brain activity, z, change over time?"







"How does brain activity, z, change over time?"

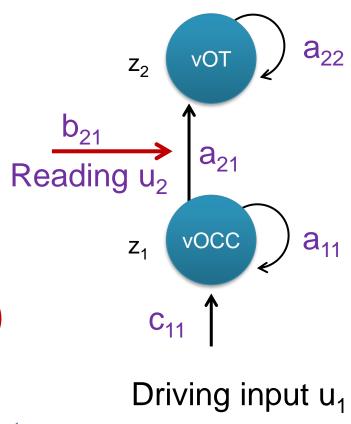


$$\dot{z_1} = a_{11}z_1 + c_{11}u_1$$

Change of activity in vOT:

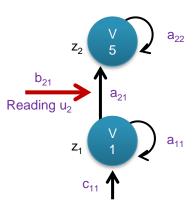
$$\dot{z_2} = a_{22}z_2 + a_{21}z_1 + (b_{21}u_2)z_1$$

$$\uparrow \qquad \uparrow \qquad \uparrow$$
Self decay V1 input Modulatory input





"How does brain activity, z, change over time?"

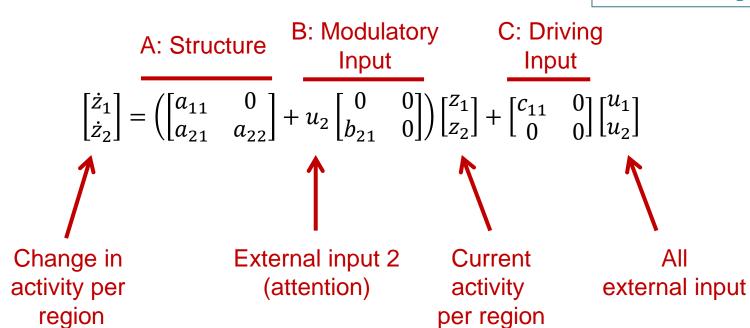


Driving input u₁

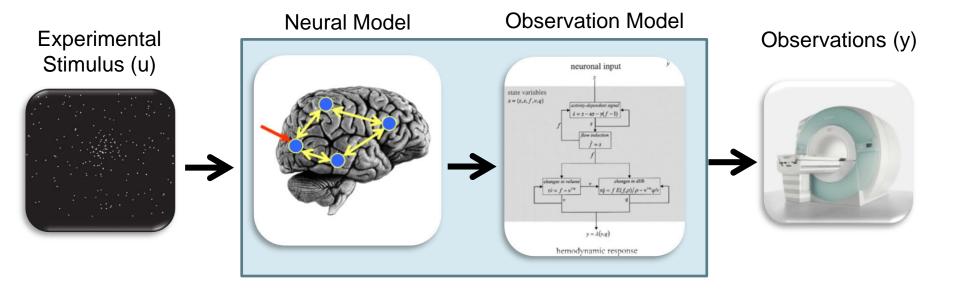
For m inputs:

$$\dot{z} = (A + \sum_{j=1}^{m} u_j B^j)z + Cu$$

Columns: outgoing connections Rows: incoming connections







How brain activity **z** changes over time

$$\dot{z} = f(z,u,\theta^n)$$

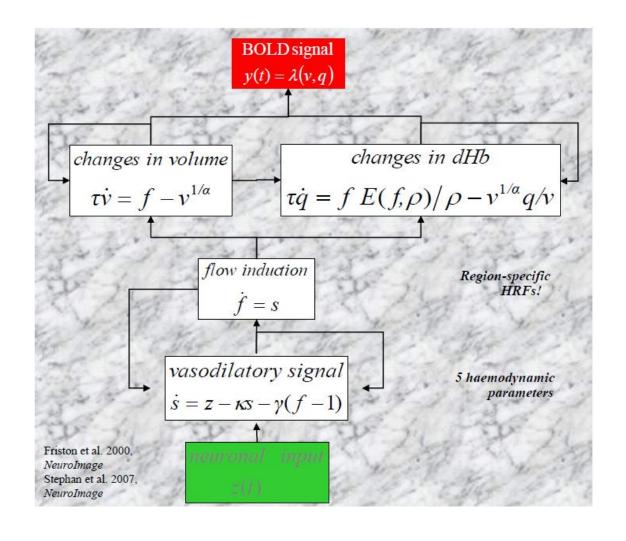
What we would see in the scanner, y, given the neural model?

$$y = g(z, \theta^h)$$

Stimulus from Buchel and Friston, 1997 Figure 3 from Friston et al., Neuroimage, 2003 Brain by Dierk Schaefer, Flickr, CC 2.0



The Haemodynamic Model





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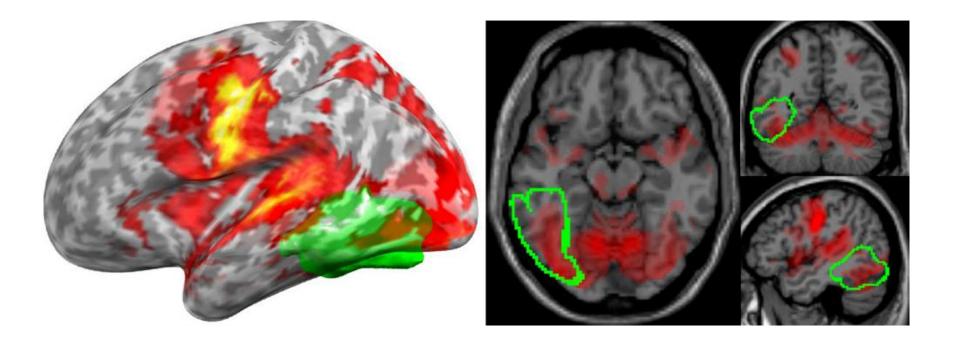
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^b University of Toronto, Toronto, ON, Canada M5S 1A8

^c Institute of Psychiatry, King's College London, London SE5 8AF, UK

^d School of Psychology, University of Birmingham, Edgbaston, Birmingham B15 2TT, UK

e Department of Experimental Psychology, Oxford University, Oxford OX3 9DU, UK



Reading > fixation (29 controls)
Lesion (Patient AH)

Pipeline



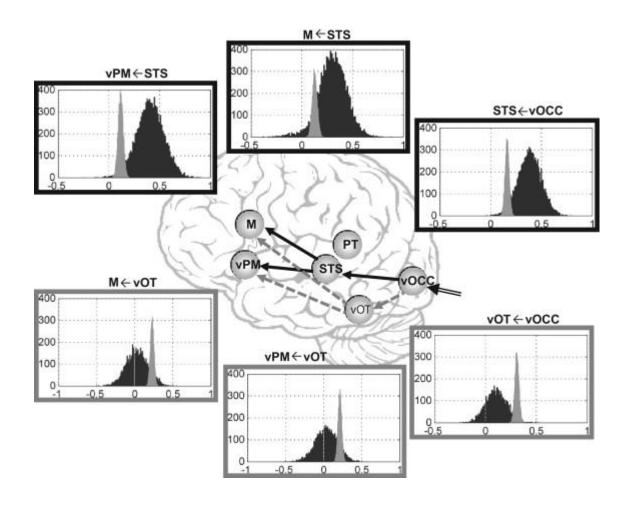
- We specified DCMs for every subject (patient and controls)
- 2. We fitted these models to the subjects' data (model estimation or inversion) to give:
 - Posterior probability distribution for each parameter $p(\theta|y,m)$
 - Estimate of the model evidence p(y|m)

$$F \cong \log p(y|m) = \operatorname{accuracy} - \operatorname{complexity}$$

Free energy

3. We chose the models with the highest evidence and then inspected their parameters.





Key: Controls Patient



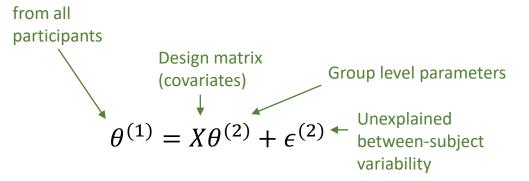
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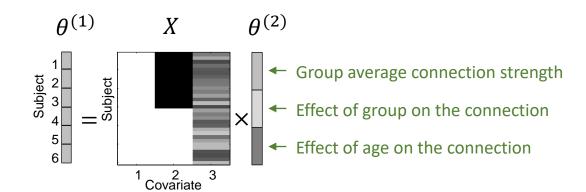


Parametric Empirical Bayes (PEB)

The connectivity parameters are taken to the group level and modelled using a (Bayesian) General Linear Model



Estimated connections



Outputs:

- One free energy for the entire group-level model (DCMs and GLM).
- Group-level
 parameters (effect of
 each covariate on
 each connection)



Summary

- DCM is a framework which enables us to make inferences about the effective connectivity of brain regions, which we can't directly observe
- We create one or more generative models, each expressing a hypothesis
- We invert the model(s), using Bayesian inference to estimate coupling parameters and the model evidence
- We compare models using Bayesian Model Comparison



Further reading and training

Tutorial papers:

Part 1 - DCM for fMRI	Zeidman, P., Jafarian, A., Corbin, N., Seghier, M.L., Razi, A., Price, C.J., Friston, K.J. A guide to group effective connectivity analysis, part 1: First level analysis with DCM for fMRI. <i>Neurolmage</i> , 200, pp. 174-190. 2019.
Part 2 - Group analysis with PEB	Zeidman, P., Jafarian, A., Seghier, M.L., Litvak, V., Cagnan, H., Price, C.J., Friston, K.J. A guide to group effective connectivity analysis, part 2: Second level analysis with PEB. <i>Neurolmage</i> , 200, pp. 12-25. 2019.