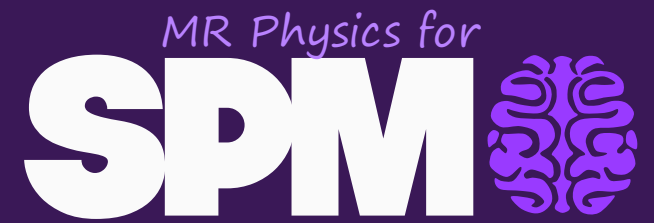


BOLD fMRI: Mechanisms & Sensitivity (How Acquisition Choices Matter)

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MR Physics for SPM – May 2026

Functional Imaging Laboratory
Department of Imaging Neuroscience



Learning Objectives

- ☐ Explain the principle of BOLD contrast in fMRI
- ☐ Understand physiological and MR-related factors influencing the BOLD signal
- ☐ Identify key acquisition parameters
- ☐ Make informed decisions to optimise BOLD sensitivity



BOLD Mechanisms

Functional MRI

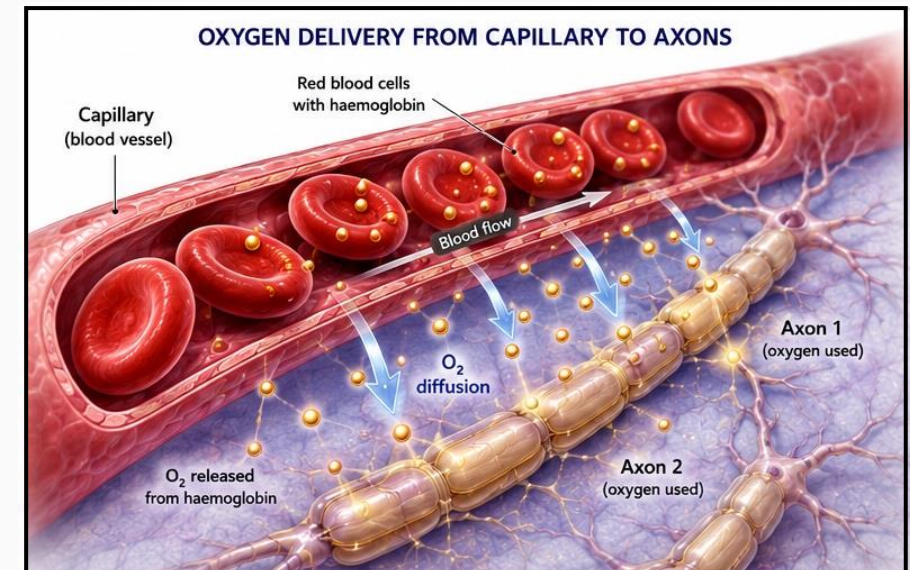
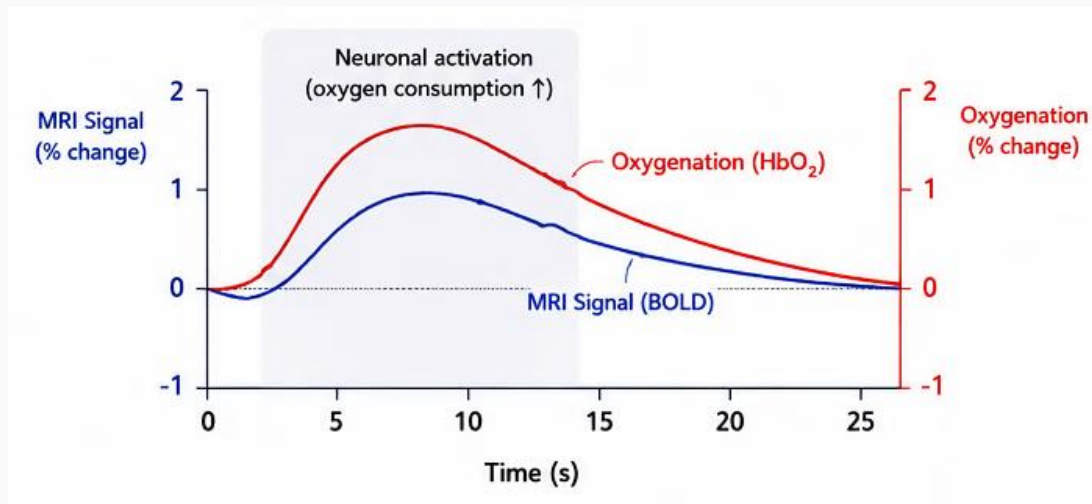
- ❑ A non-invasive imaging technique measuring brain activity **indirectly via haemodynamic changes**
- ❑ Introduced in the early 1990s
- ❑ Widely used in:
 - Cognitive neuroscience
 - Clinical research
 - Brain mapping



Ken Kwong et al. at early days of fMRI (MGH-Harvard)

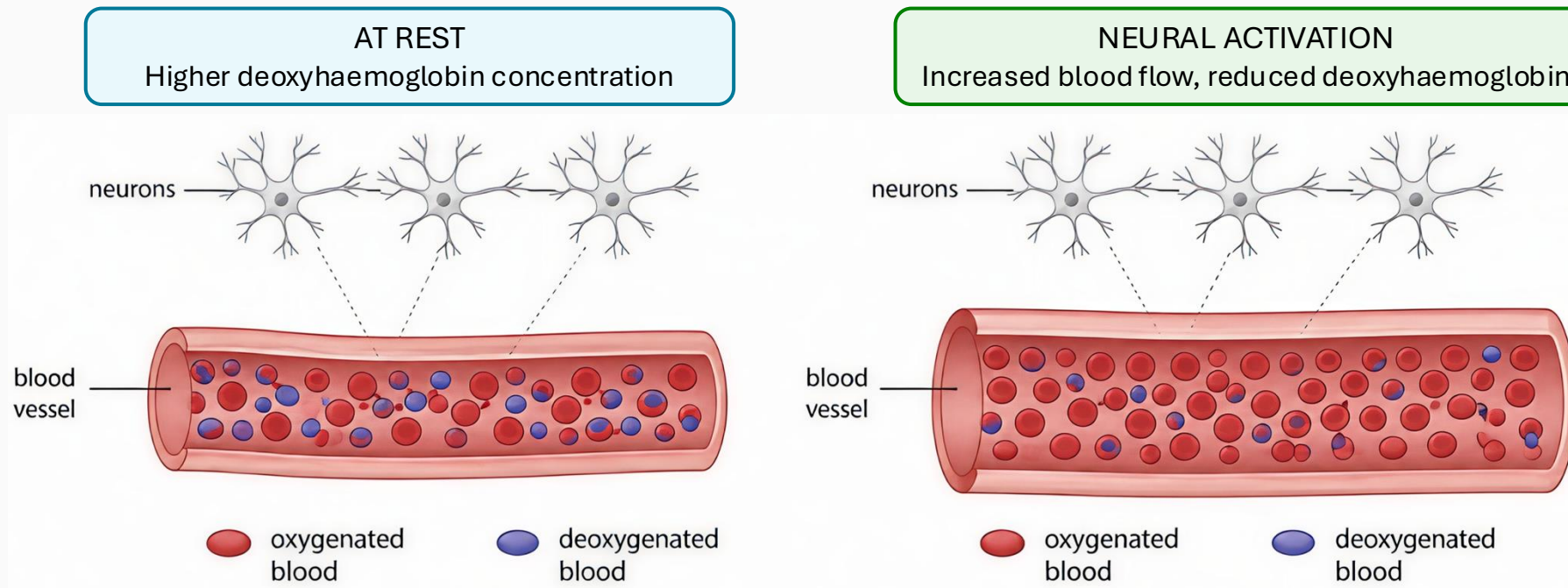
What is BOLD?

- ❑ Blood Oxygenation Level Dependent signal
- ❑ Uses [de]oxy-haemoglobin as an endogenous contrast agent
- ❑ Relies on magnetic susceptibility differences → MRI is sensitive to
- ❑ Reflects changes in blood oxygenation



Neural Activation → BOLD

- Physiological effects leading to a change of blood oxygenation, and thus a BOLD signal change:

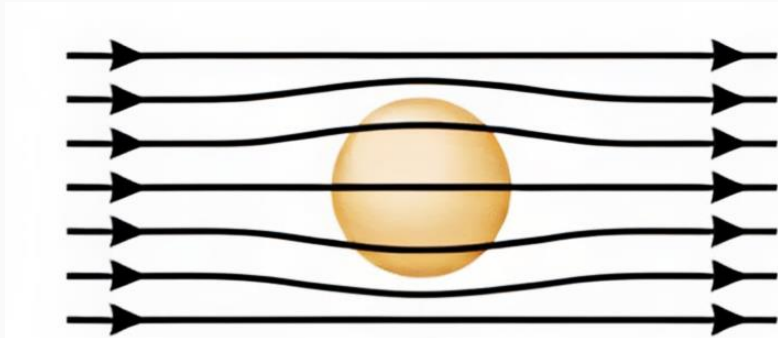


High *deoxy:oxygated* blood ratio → Higher T_2^*

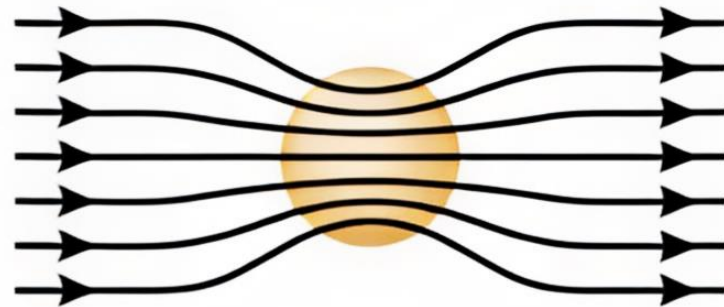
Low *deoxy:oxygated* blood ratio → Lower T_2^*

Magnetic susceptibility

- A measure of how easily a material becomes magnetized when placed in an external magnetic field
 - Diamagnetic ($\chi < 0$): weakly repelled by the external magnetic field
 - Paramagnetic ($\chi > 0$): attracted to the external magnetic field



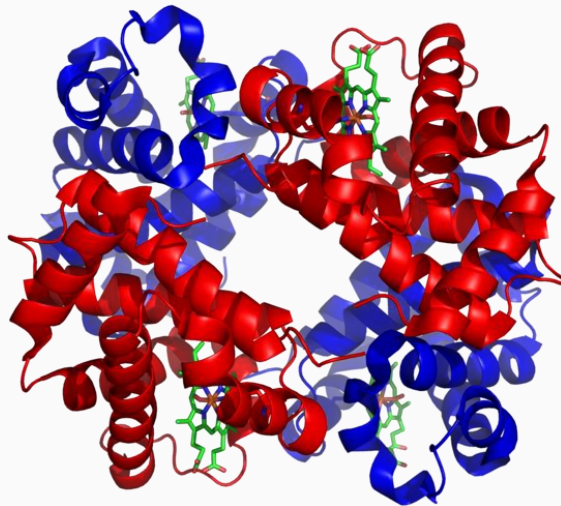
Field bends slightly away from the material



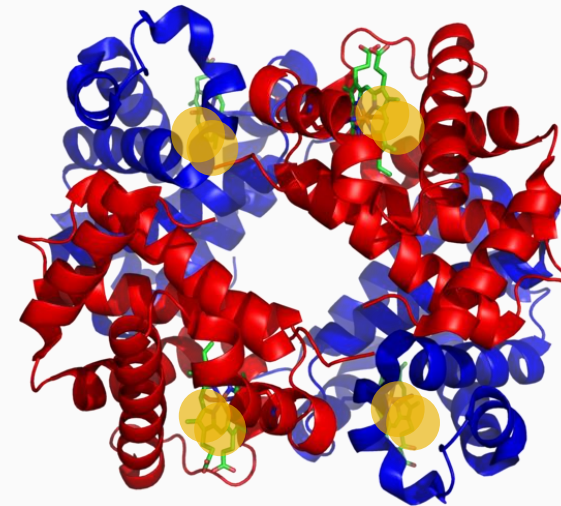
Field bends toward the material

Susceptibility → Signal Change

- ❑ Deoxyhaemoglobin creates local field gradients
- ❑ Act like microscopic dipoles affecting background magnetic field



Heme groups containing **Iron**
→ making Hb **paramagnetic**

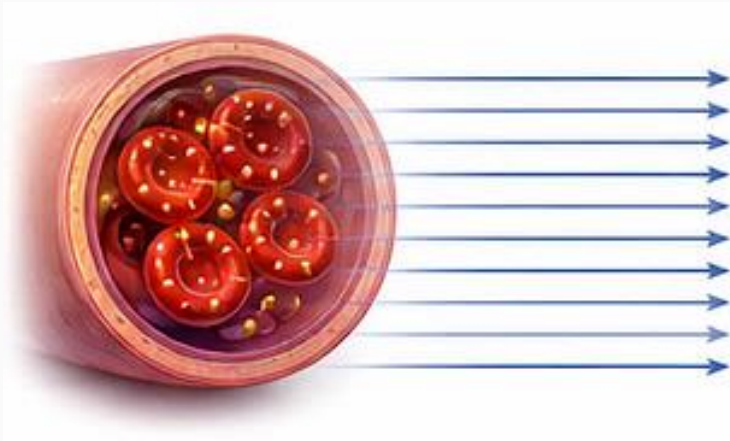


Bound **oxygen** shields Heme groups
→ making HBO₂ **diamagnetic**

Susceptibility → Signal Change

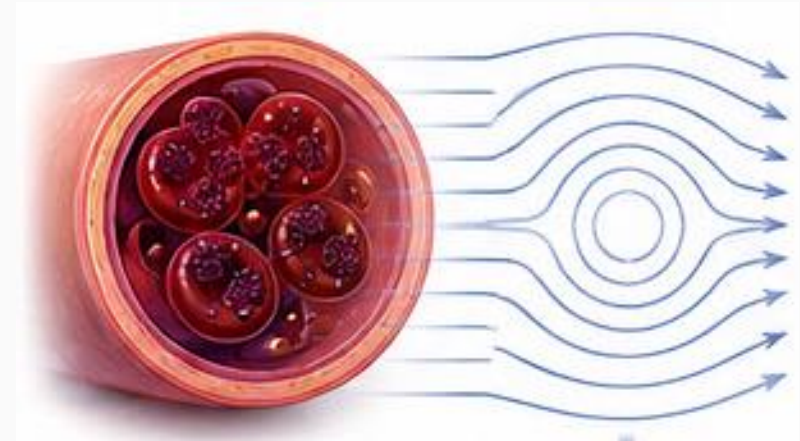
- ❑ Deoxyhaemoglobin creates local field gradients
- ❑ Act like microscopic dipoles affecting background magnetic field

Acting like the tissue



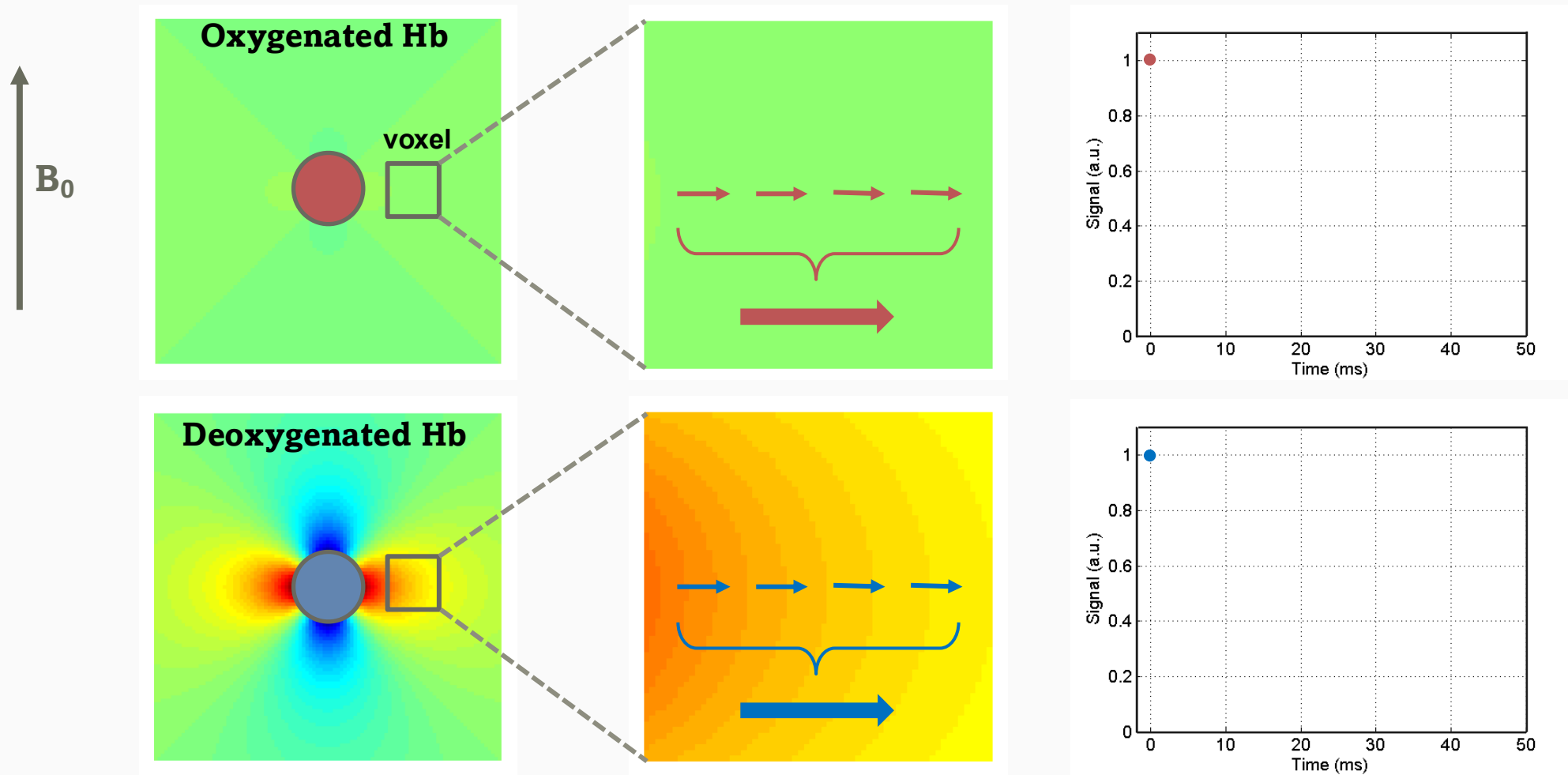
Heme groups containing **Iron**
→ making Hb **paramagnetic**

Acting different from the tissue

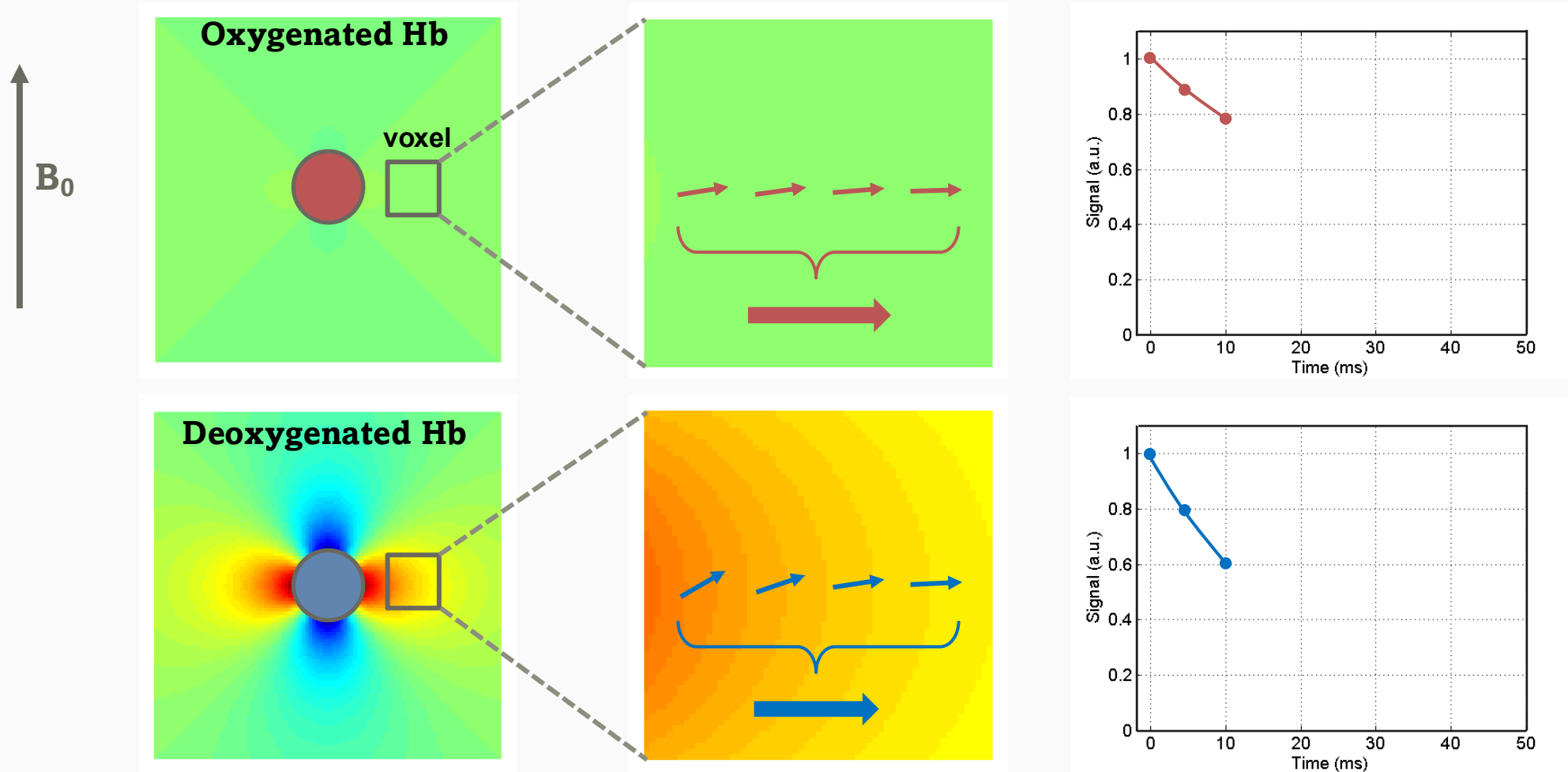


Bound **oxygen** shields Heme groups
→ making HBO₂ **diamagnetic**

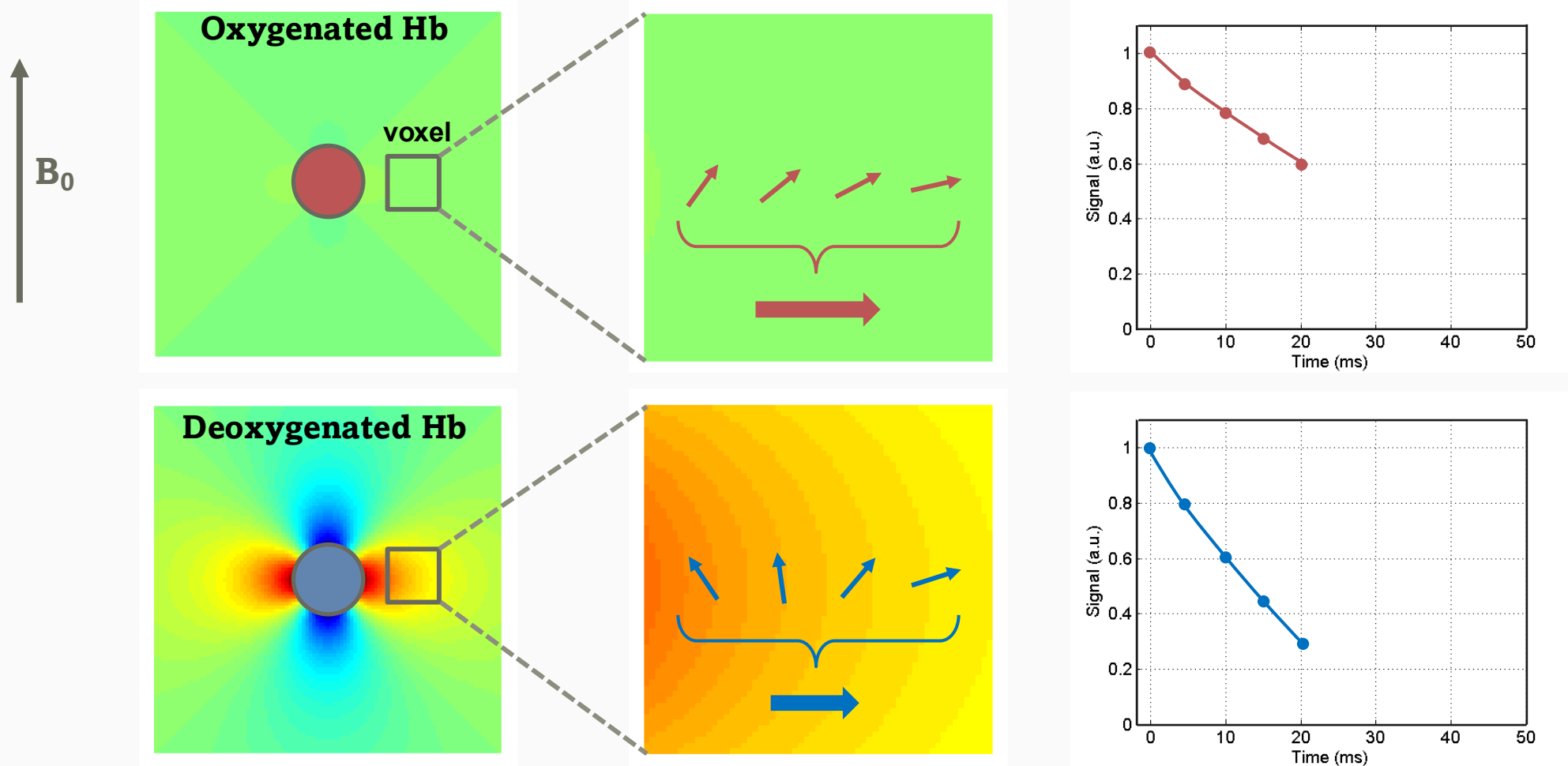
Susceptibility → Signal Change



Susceptibility → Signal Change



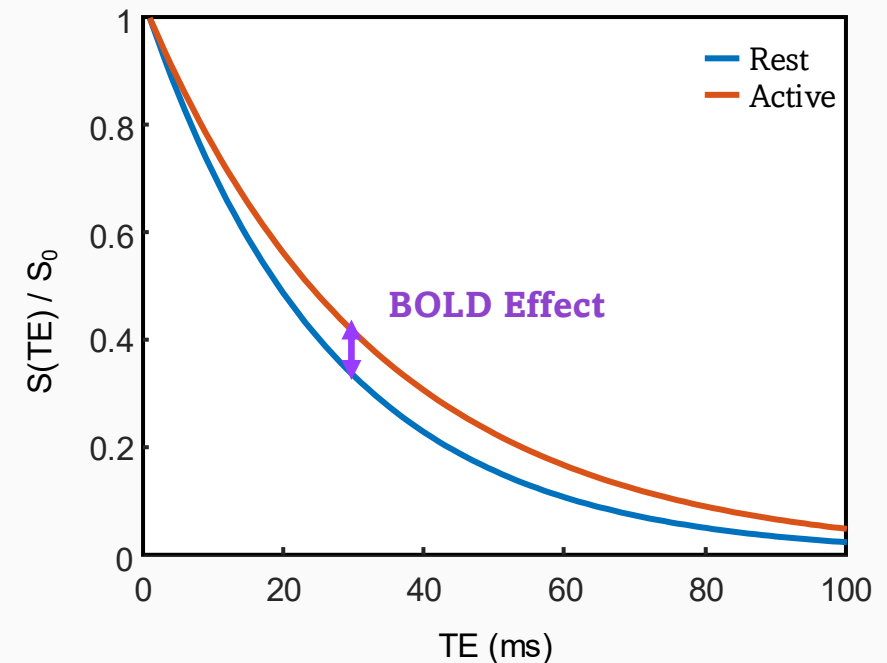
Susceptibility → Signal Change



BOLD Signal

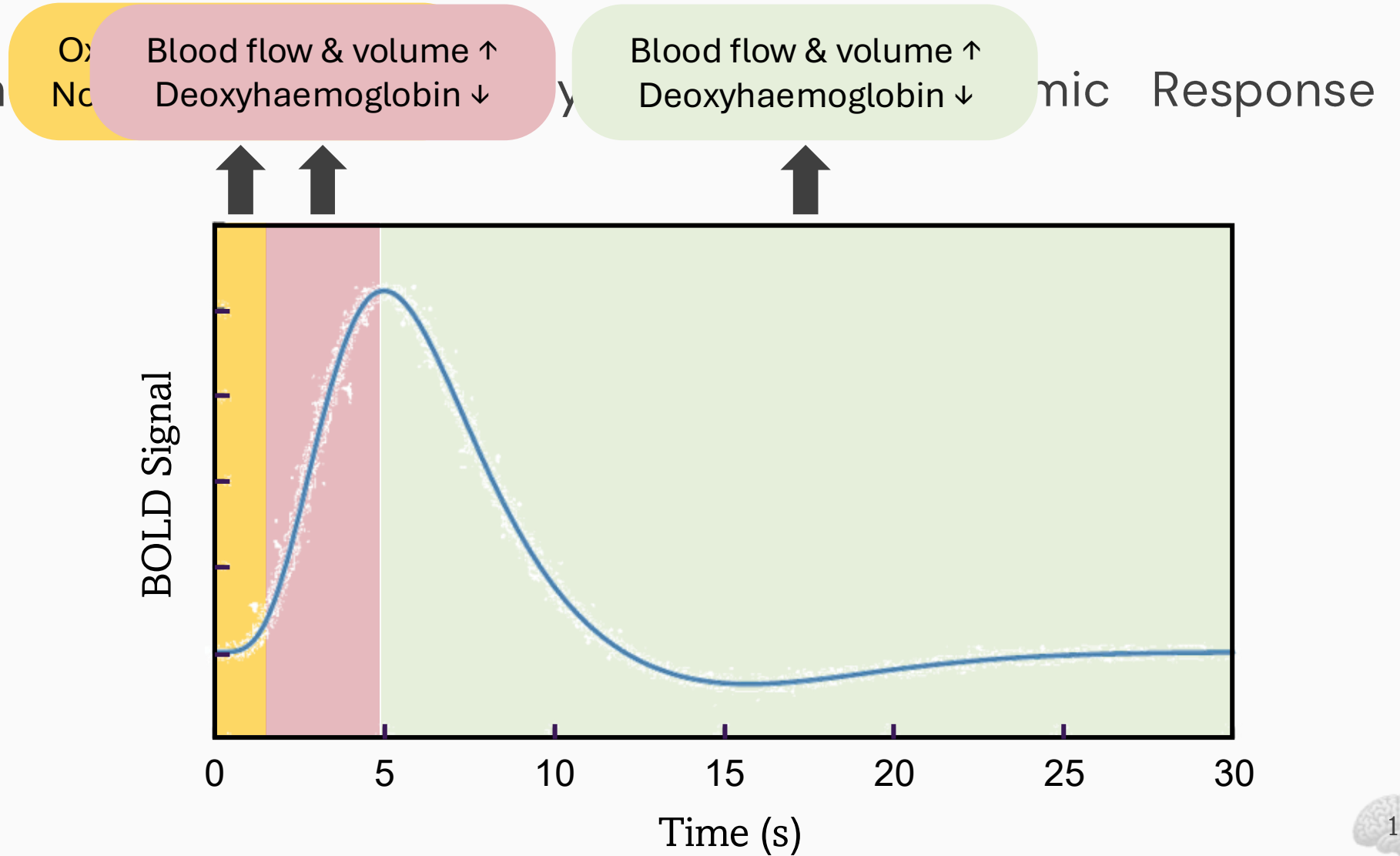
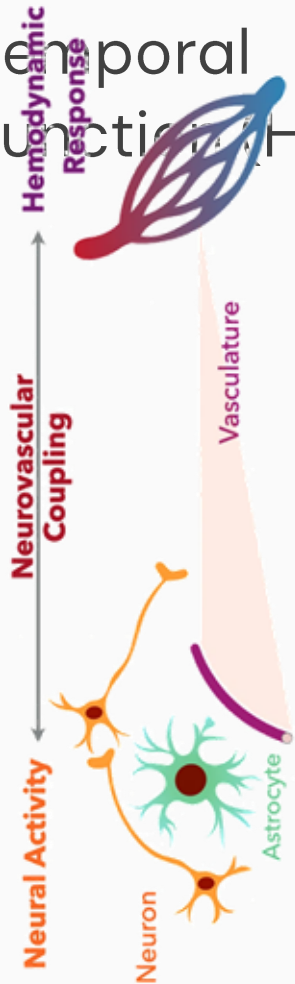
- ❑ Small effect (1–5%)
- ❑ Spatially variable
- ❑ Competes with:
 - Thermal noise
 - Physiological noise

$$S(TE) = S_0 e^{-TE/T_2^*}$$



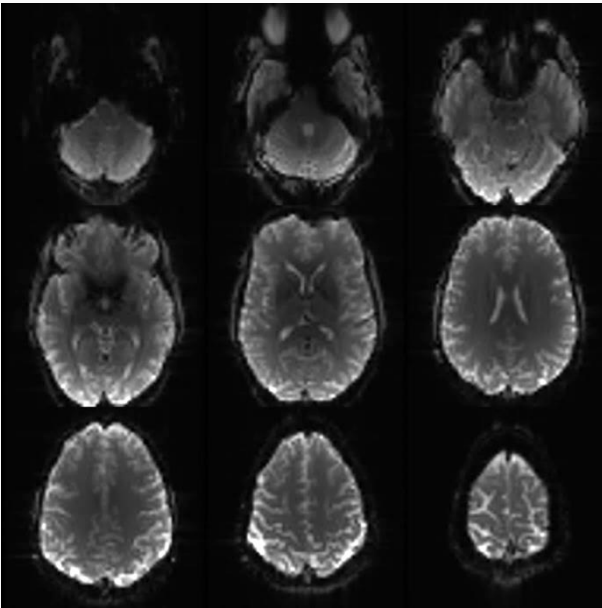
BOLD Signal Time Course

- Temporal behaviour of the BOLD signal (HRF)

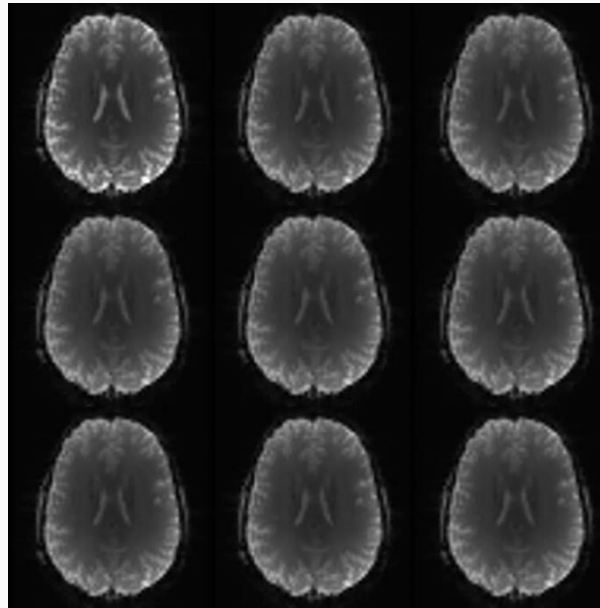


Sampling Requirements

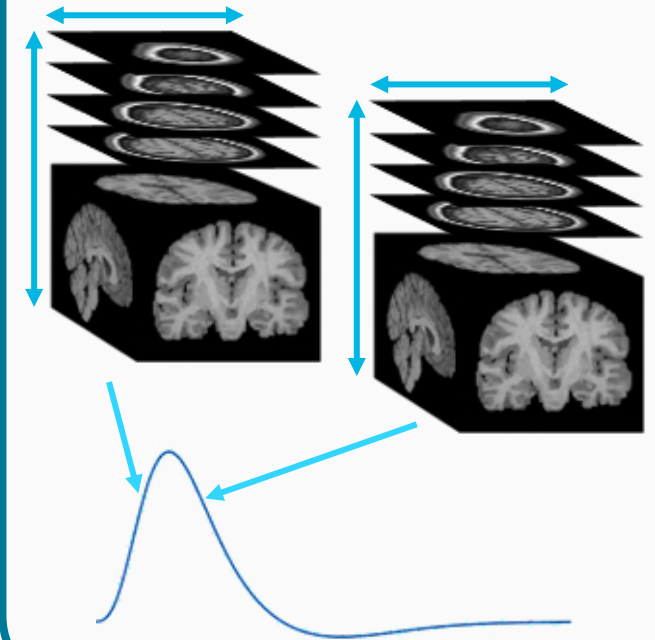
Cover spatial extent



Capture dynamics



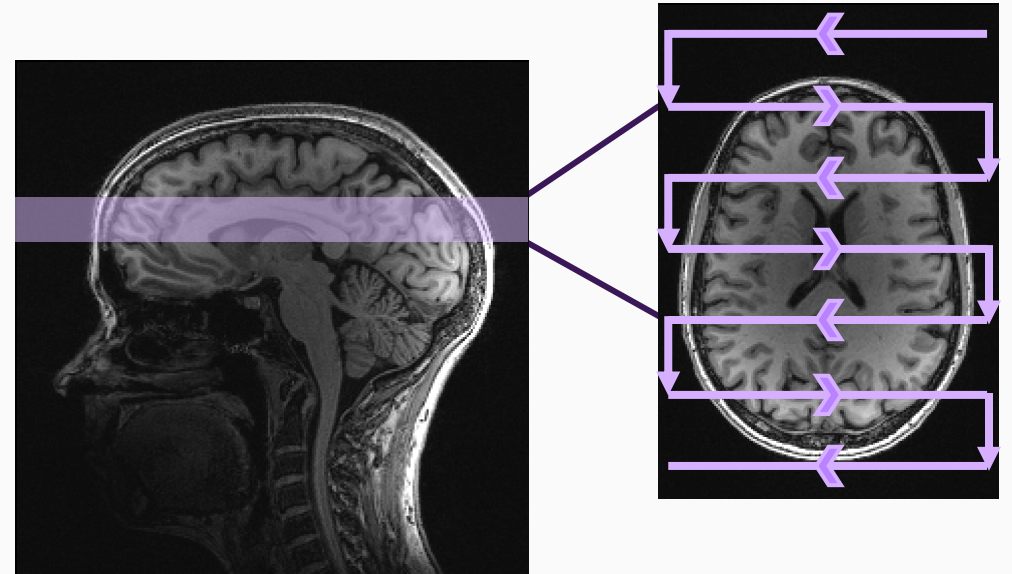
Be sufficiently fast



How To Measure BOLD?

- ❑ Gradient-Echo Echo Planar Imaging (GRE-EPI)
 - ✓ Provides T_2^* contrast
 - ✓ Acquires whole slice in one shot
 - ✓ Very fast $\rightarrow$ captures dynamics

👉 Key benefit:
Enables whole-brain imaging every $\sim 2-3$ seconds



BOLD Sensitivity

BOLD Sensitivity

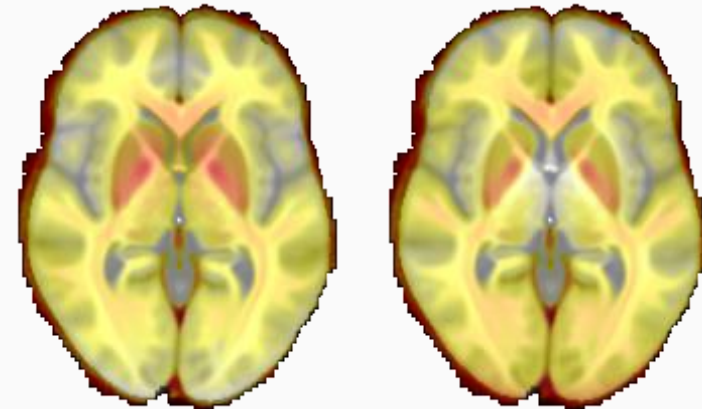
- ❑ Ability to detect small neural changes reliably

- ❑ Simplified Model:

$$\text{Sensitivity} \approx \text{TE} \times \text{Signal}$$

- ❑ Depends on:

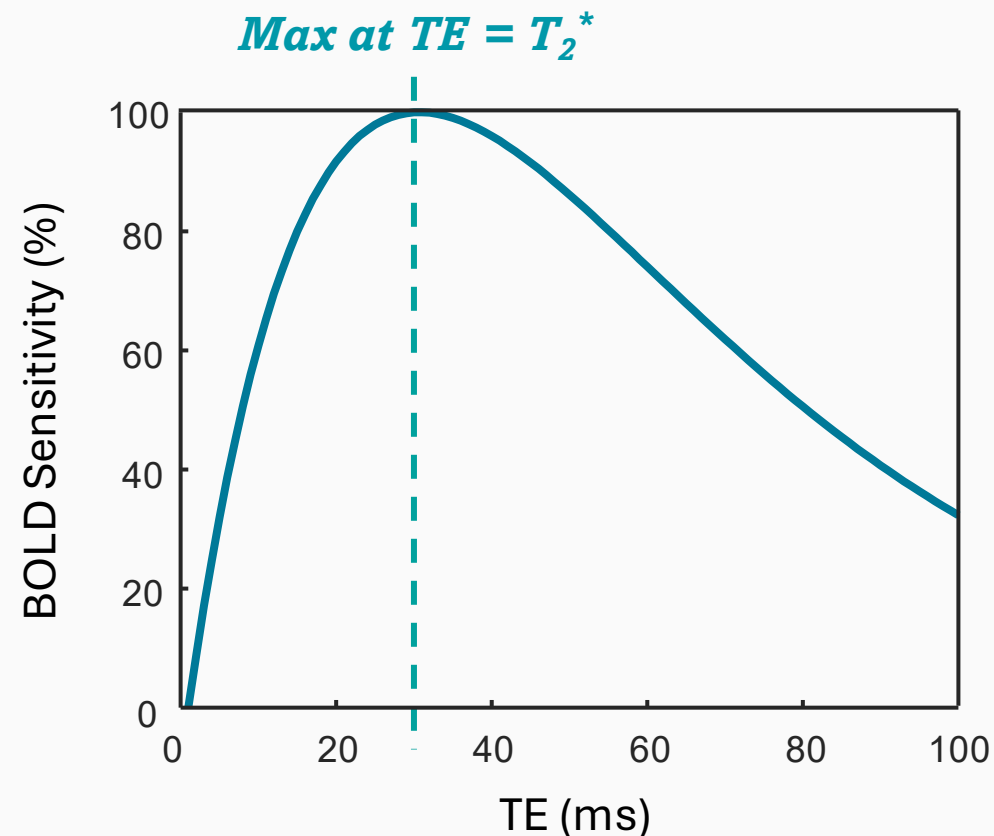
- ✓ TE (Contrast)
- ✓ Signal strength
- ✓ Sampling (acquisition strategy)



BOLD Sensitivity – Echo Time (TE)

□ TE must be sufficiently long for the BOLD signal to evolve

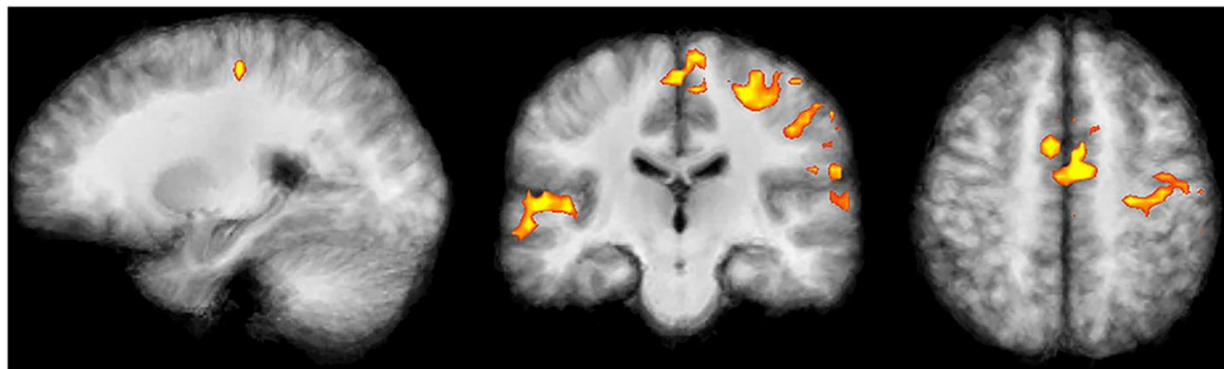
- Short TE → weak BOLD contrast
- Long TE → signal already gone
- Optimal TE $\approx T_2^*$



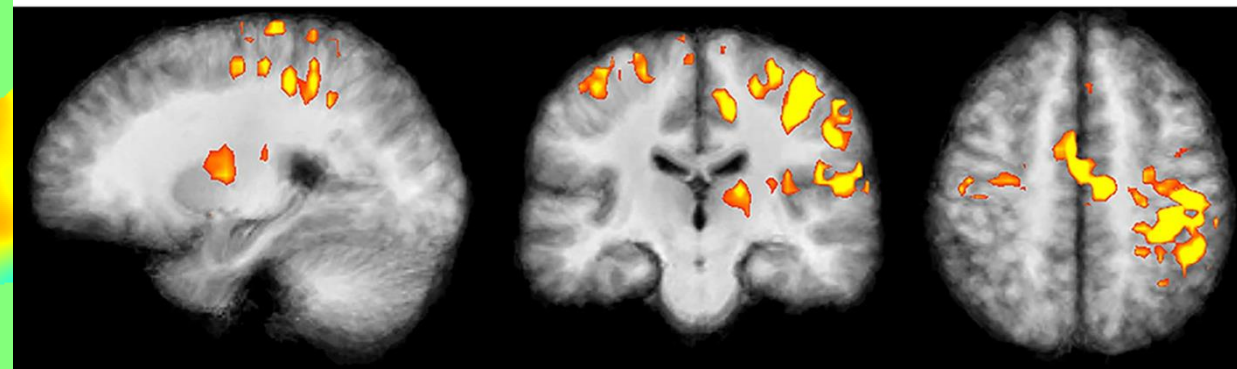
→ *matching tissue property*

BOLD Sensitivity – Signal

- ❑ Field strength
- ❑ Field inhomogeneities



3T



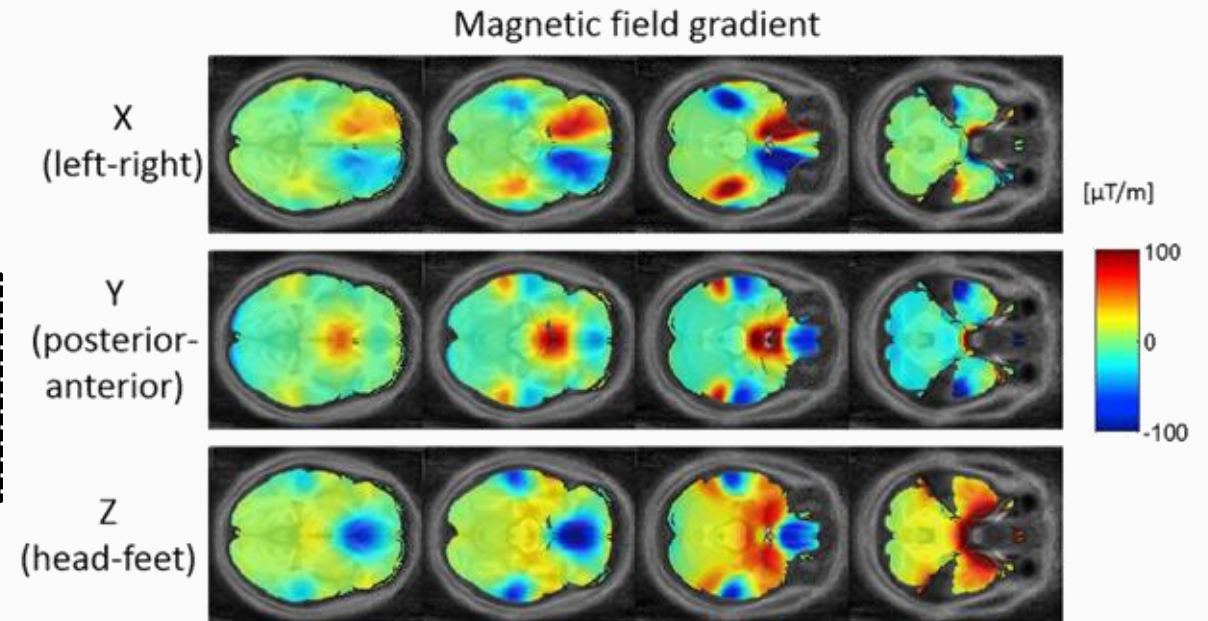
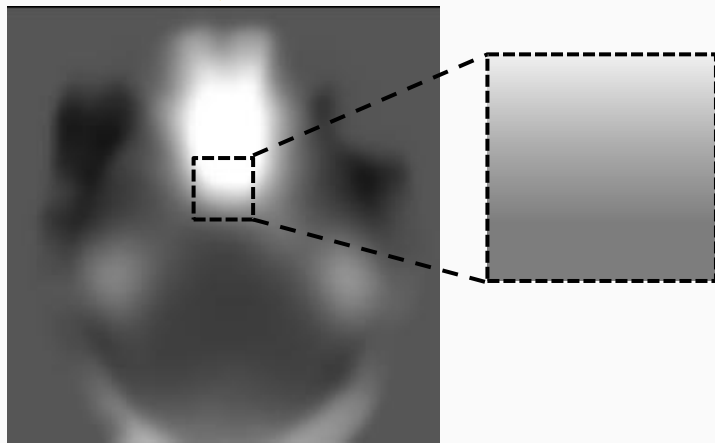
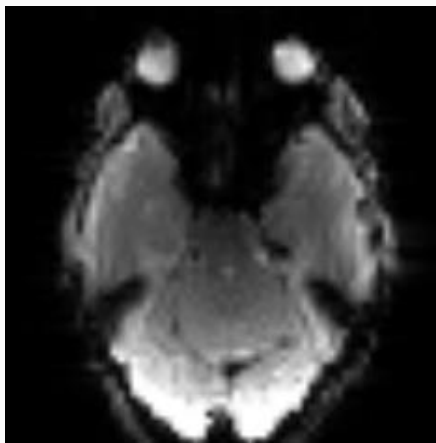
7T

Frequency offset: $\Delta\omega_0 = \gamma\Delta B_0$

BOLD Sensitivity – Field Inhomogeneities

- ❑ Occur at interfaces with large susceptibility differences
 - ✓ air-tissue interfaces (e.g., sinuses, ear canals in the head)

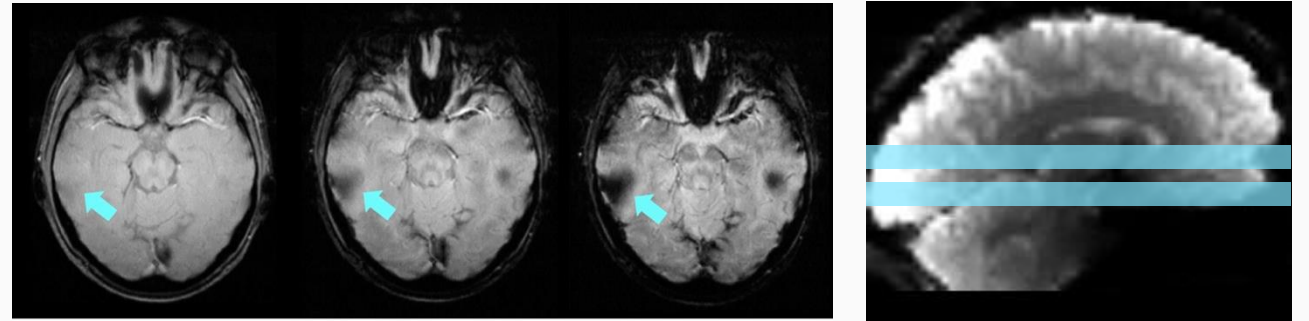
Air/Tissue interfaces lead to susceptibility mismatch



BOLD Sensitivity – Field Inhomogeneities

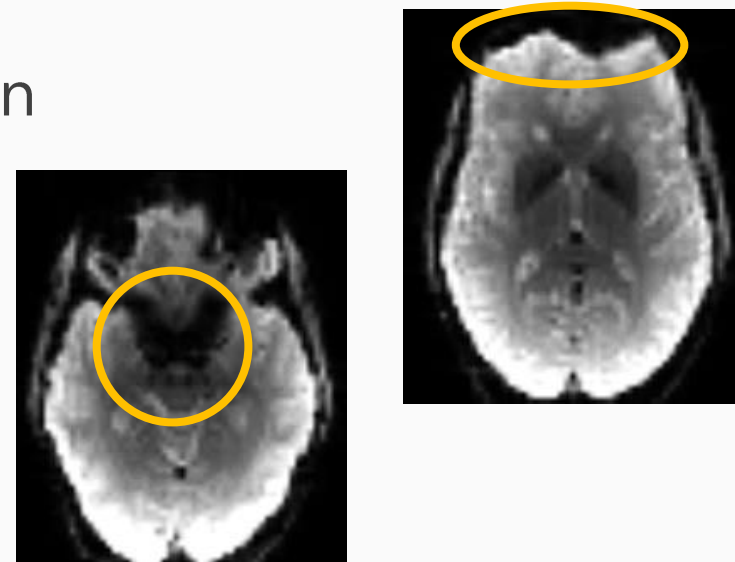
❑ Through-slice dephasing:

- Signal loss (dropouts)



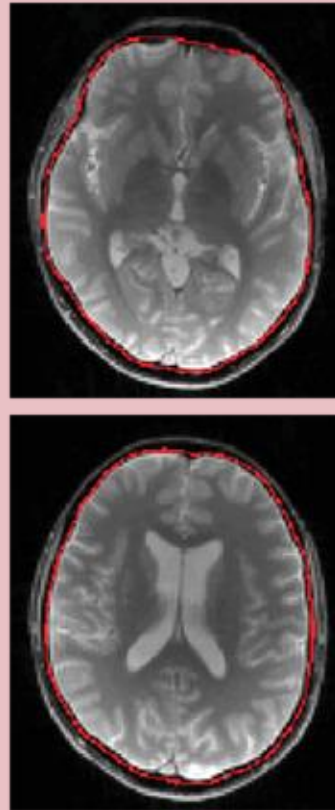
❑ In-plane dephasing:

- Signal stretch/compress in PE direction
- Signal loss (dropouts or void)

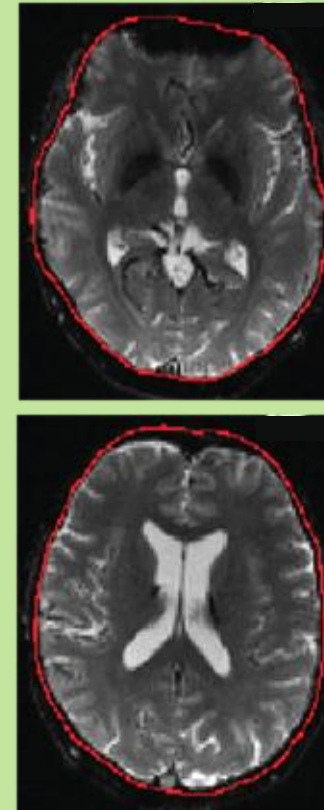


BOLD Sensitivity – Field Inhomogeneities

Conventional GRE



GRE EPI



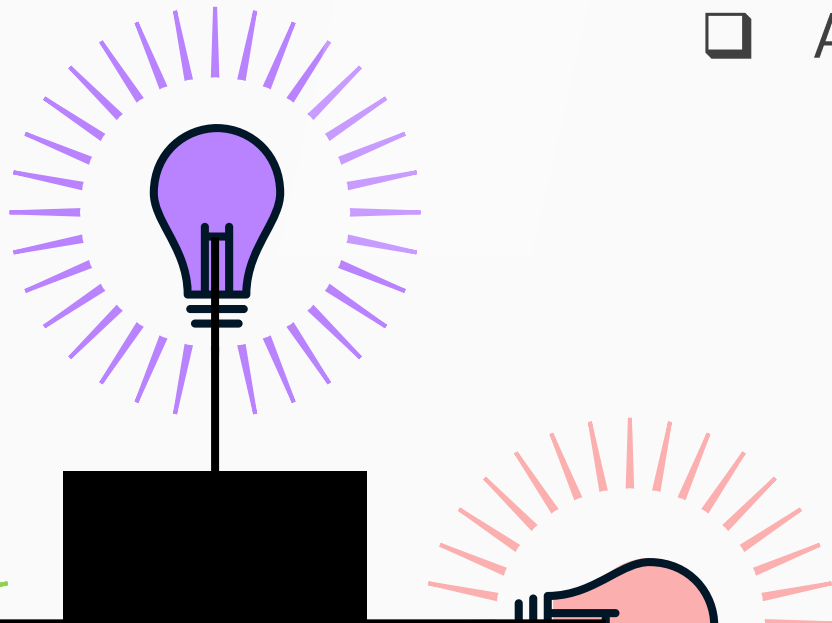
How to Improve BOLD Sensitivity?

Improving Sensitivity

1

Slice Angulation

- ❑ Susceptibility gradients depend on orientation
- ❑ Adjust slice orientation to:
 - Redistribute gradients

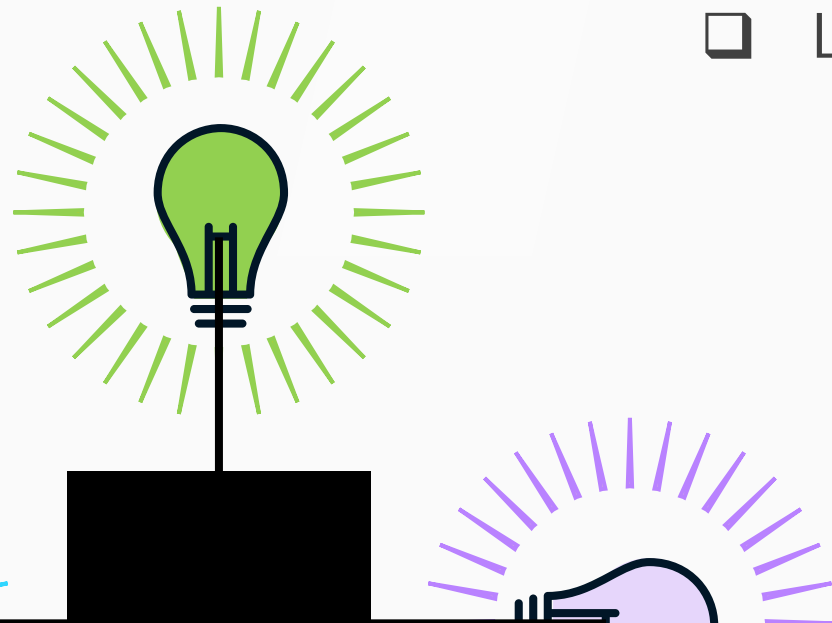


Improving Sensitivity

2

Compensation Gradients

- ❑ Refocus signal → reduce through-slice signal loss
- ❑ Limitations:
 - Not always available (e.g. in multiband)
 - Dephasing other regions



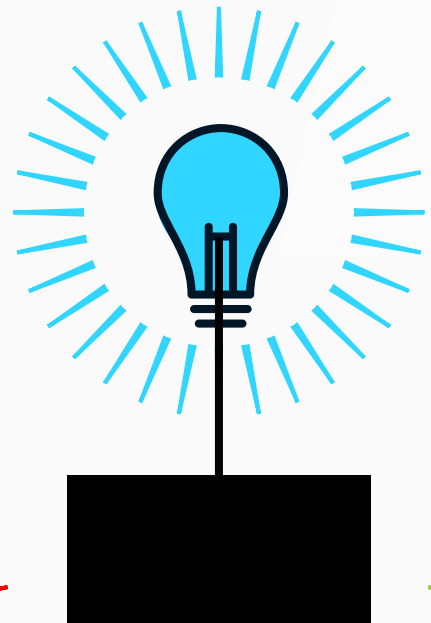
Improving Sensitivity

3

Phase Encoding Direction

- ❑ Determines the direction of distortion
- ❑ AP vs PA encoding:
 - Not changing *whether* distortion happens
 - But changing *where* signal is misplaced

Want to know more?
Heads up for the next
lecture 😊

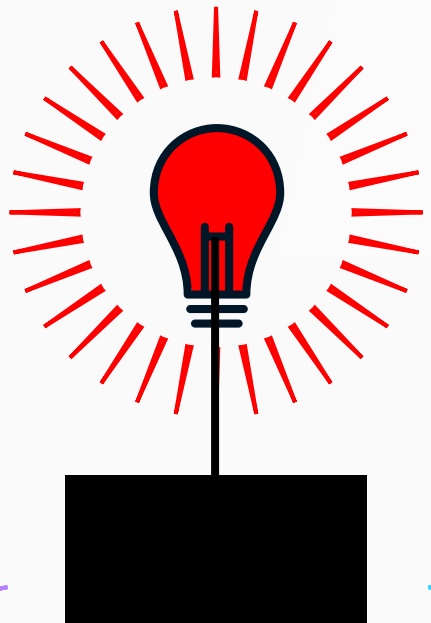


Improving Sensitivity

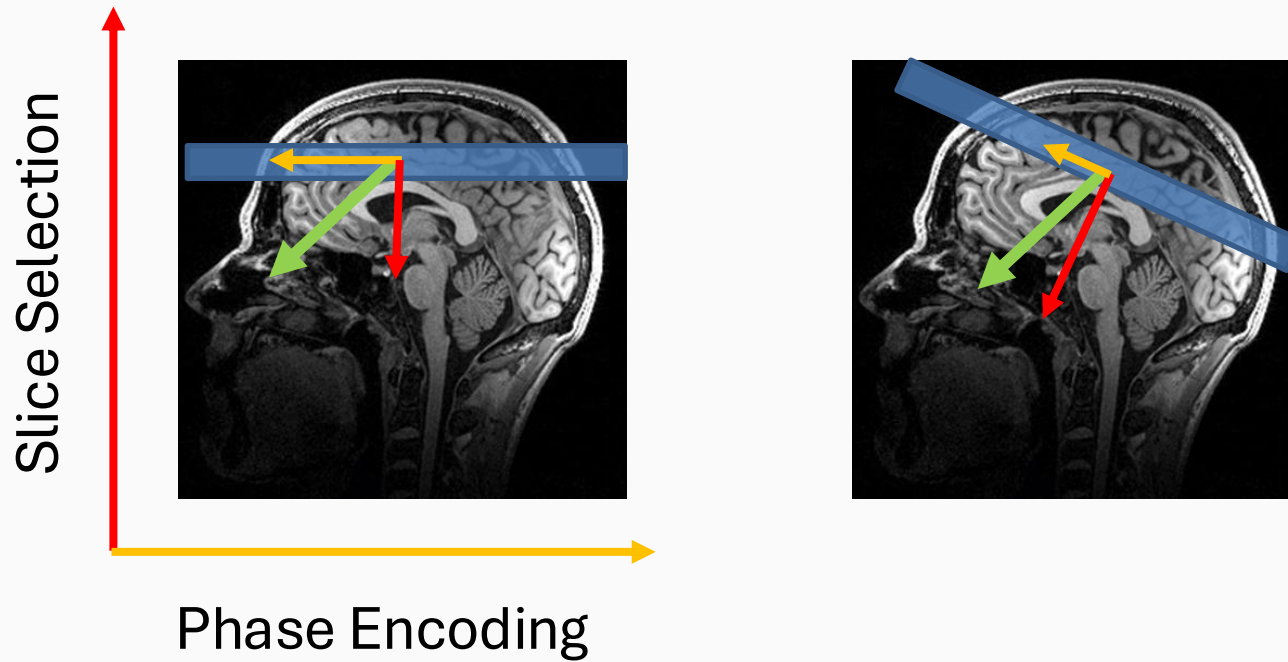
4

Match TE

- ❑ TE should reflect regional T_2^*
 - Not always feasible from signal perspective
- ❑ Effective local TE is influenced by the susceptibility gradients in the PE direction



Improving Sensitivity



Combined angulation, z-shimming and optimal PE direction

→ moves the sources of trouble away from the region of interest...

**How to make Informed decision to
improve BOLD Sensitivity?**

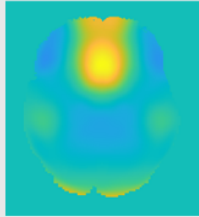
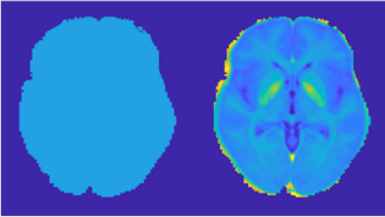
Optimisation Toolbox

- ☐ Available in SPM
- ☐ Predicts signal loss & Sensitivity across brain
- ☐ Enables data-driven protocol design
- ☐ Supports ROI-based optimisation
- ☐ Upcoming → Global optimisation across multiple ROIs

Inputs

Field map

Global R_2^* value or a spatial map

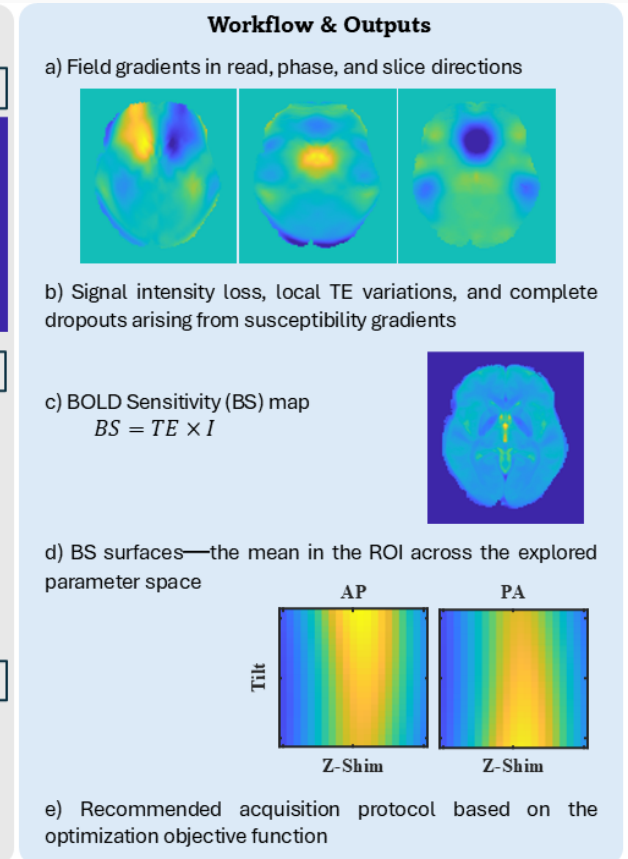



Parameters of the reference EPI sequence

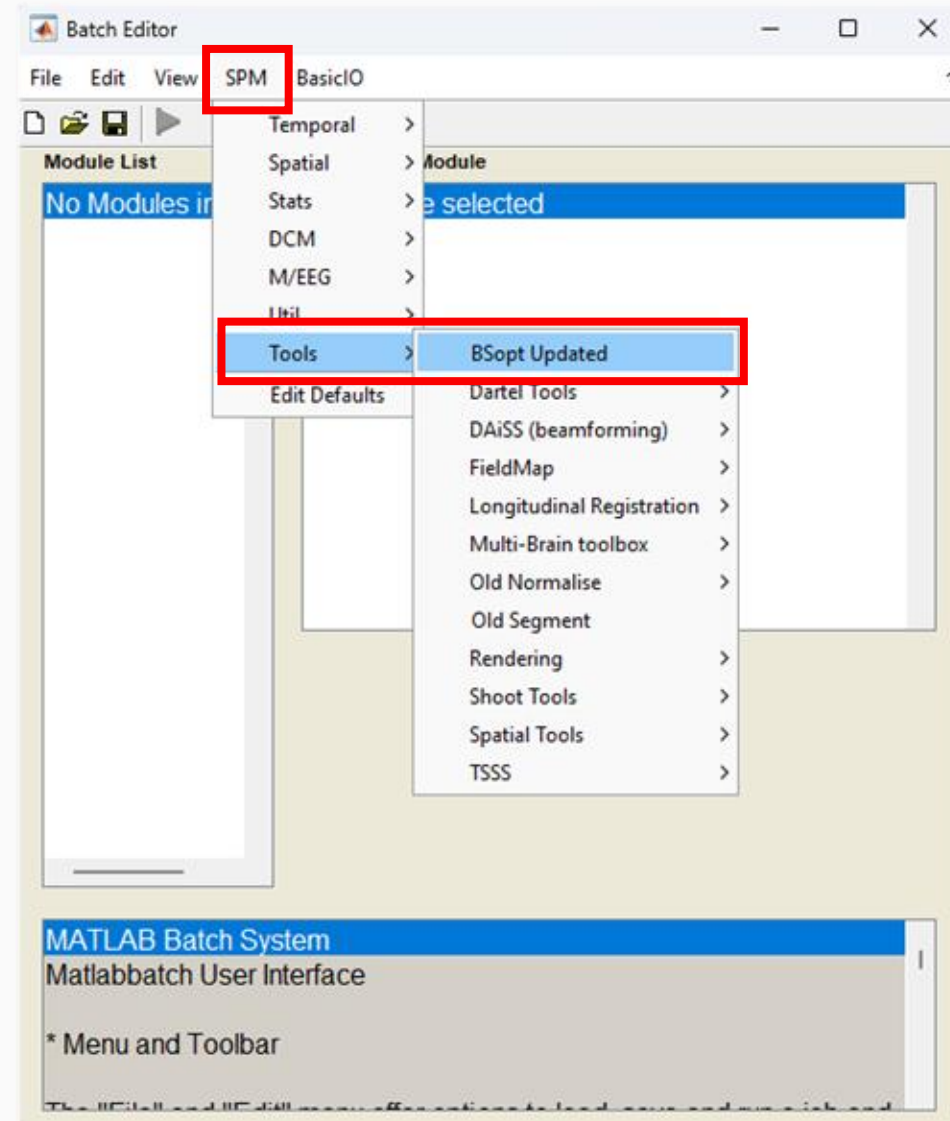
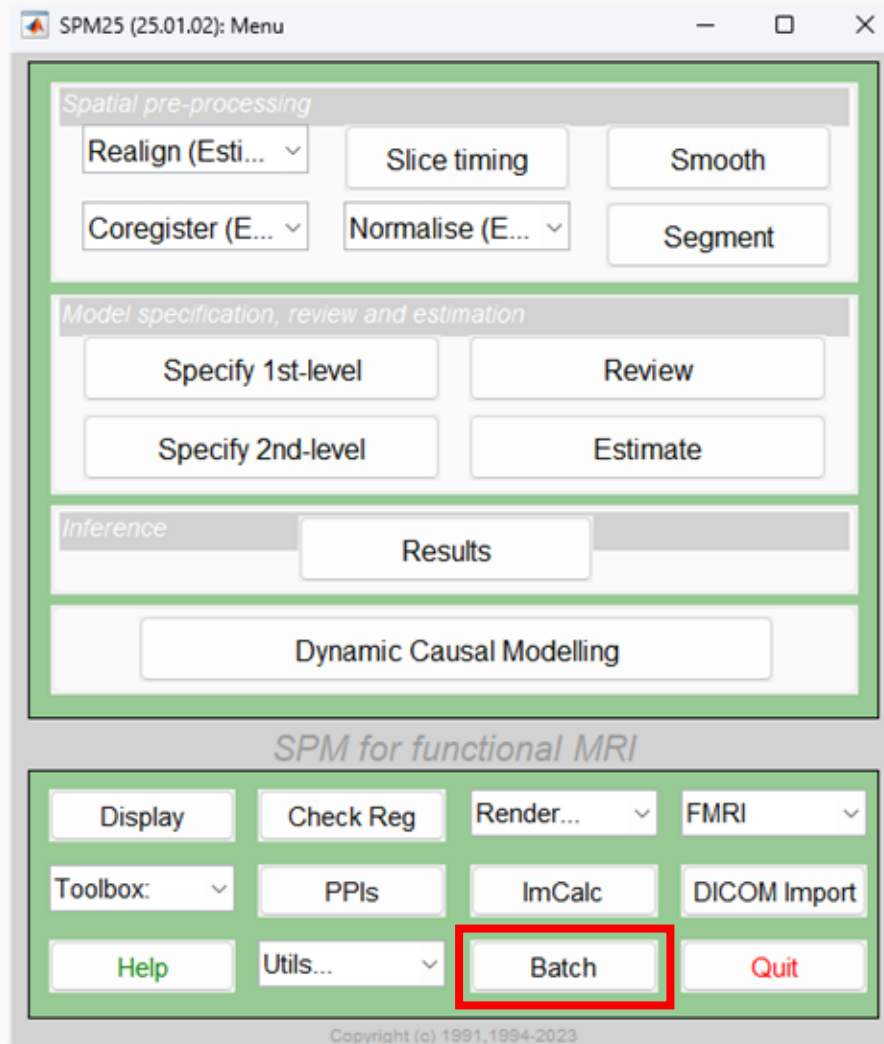
- Choose the main orientation	TRA
- Field of view	192
- Base resolution	64
- Phase oversampling	12
- Slice thickness	3
- Echo spacing	0.5
- Echo time	30
- Voxel size	[3 3 3]
- Acceleration factor	1
- Partial Fourier factor	1

Search space

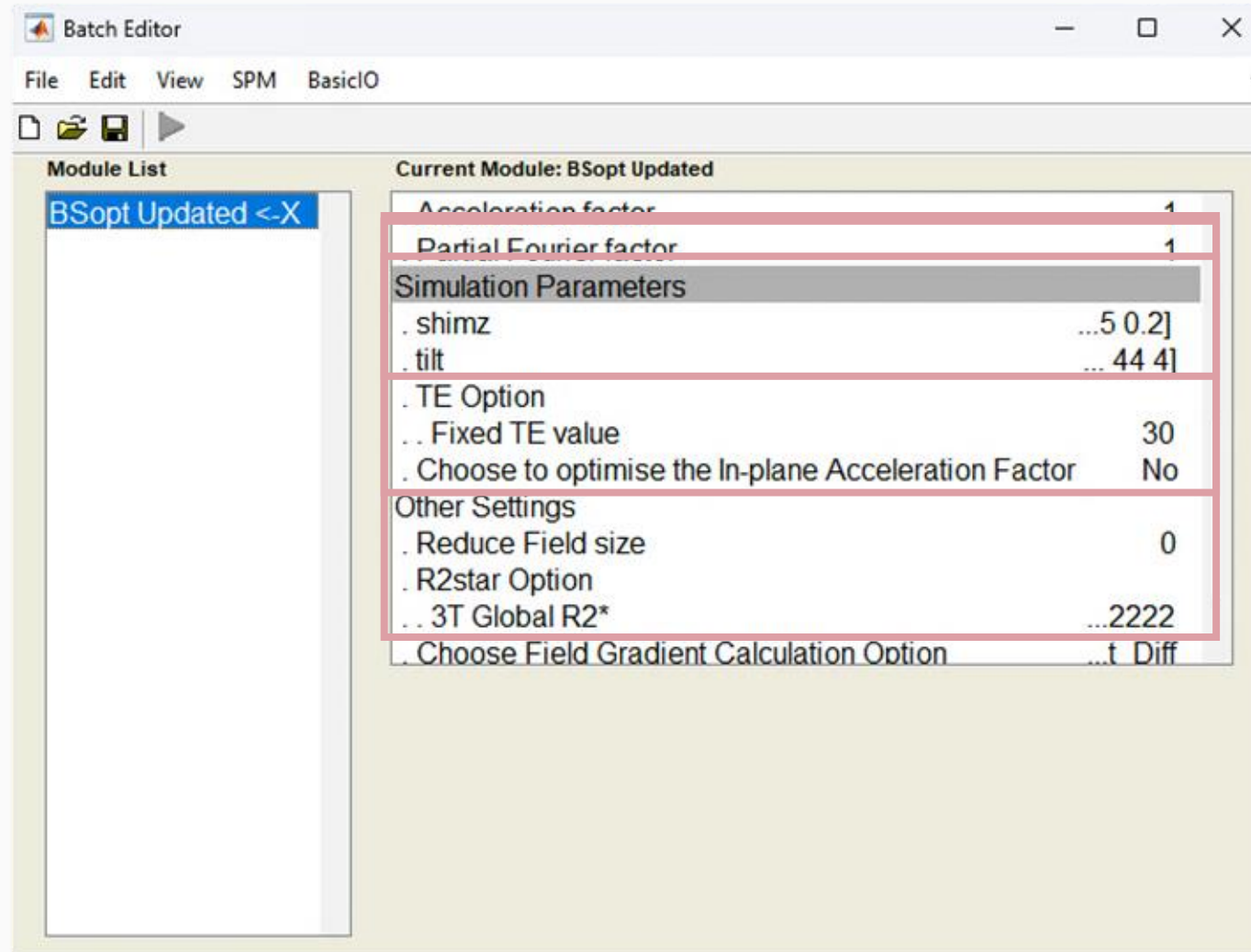
- PE direction	AP, PA
- Z-shim	[-5:0.5:5]
- Tilt	[-44:4:44]
- TE Option	
- Fixed/Variable TE	



Optimisation Toolbox

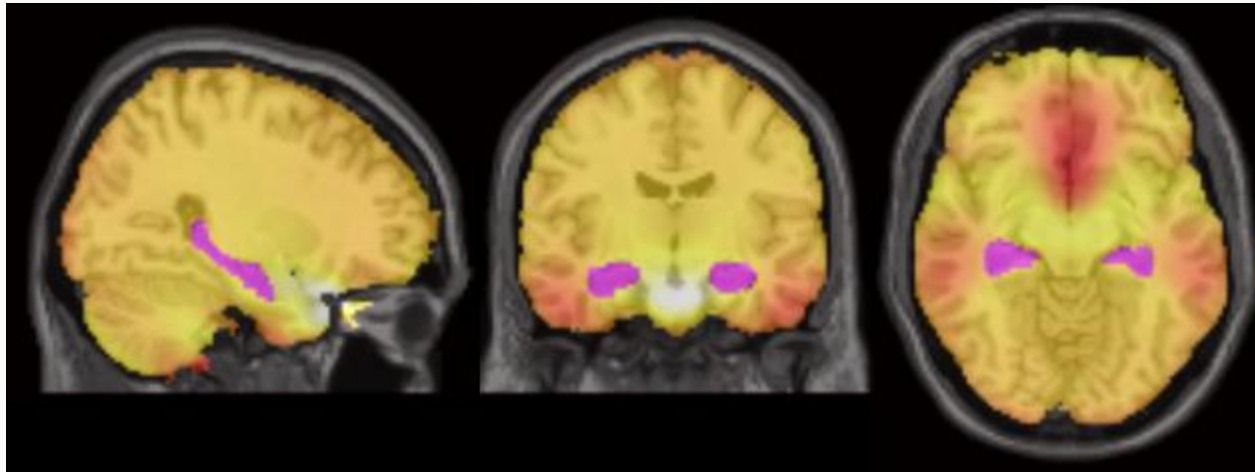


Optimisation Toolbox



Optimisation Toolbox

BOLD Sensitivity map of the optimised protocol



Optimal Protocol



Optimization summary for echotime = 30.00 and in-plane acceleration factor = 1

ROI_Nr	ROI	BS_gain (%)	z-shim	tilt	PE
1	{ 'Hippocampus' }	15.08	0.4	-44	"AP"

Summary & Take-Home Messages

1

BOLD signal is small, indirect, and physically constrained

2

Sensitivity depends on: TE, geometry, and acquisition strategy

3

Trade-offs are unavoidable → design must match research question

4

Optimisation = managing trade-offs, not eliminating them

Good fMRI  informed compromise

Acknowledgement & Questions

- ❑ SPM Course Organisation Team & FIL Physics Team
- ❑ Some images generated using *OpenAI* tools.



Thank
You

